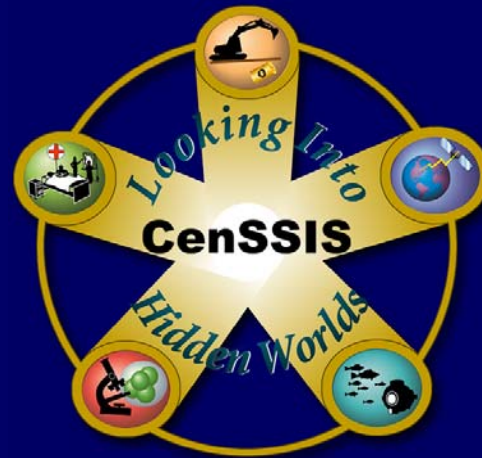


NSF Engineering Research Center for Subsurface Sensing & Imaging Systems

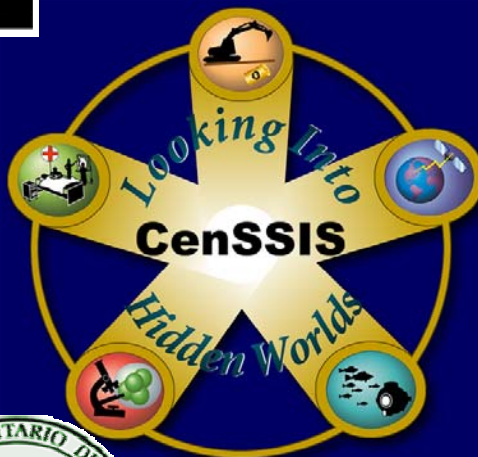


Badri Roysam, D. Sc.,

Associate Director of CenSSIS ERC

Professor, Rensselaer Polytechnic Institute, Troy, NY.

About the CenSSIS ERC



Established: 2000



Air Force Office of Scientific Research (AFOSR)
The Basic Research Manager of the Air Force Research Laboratory



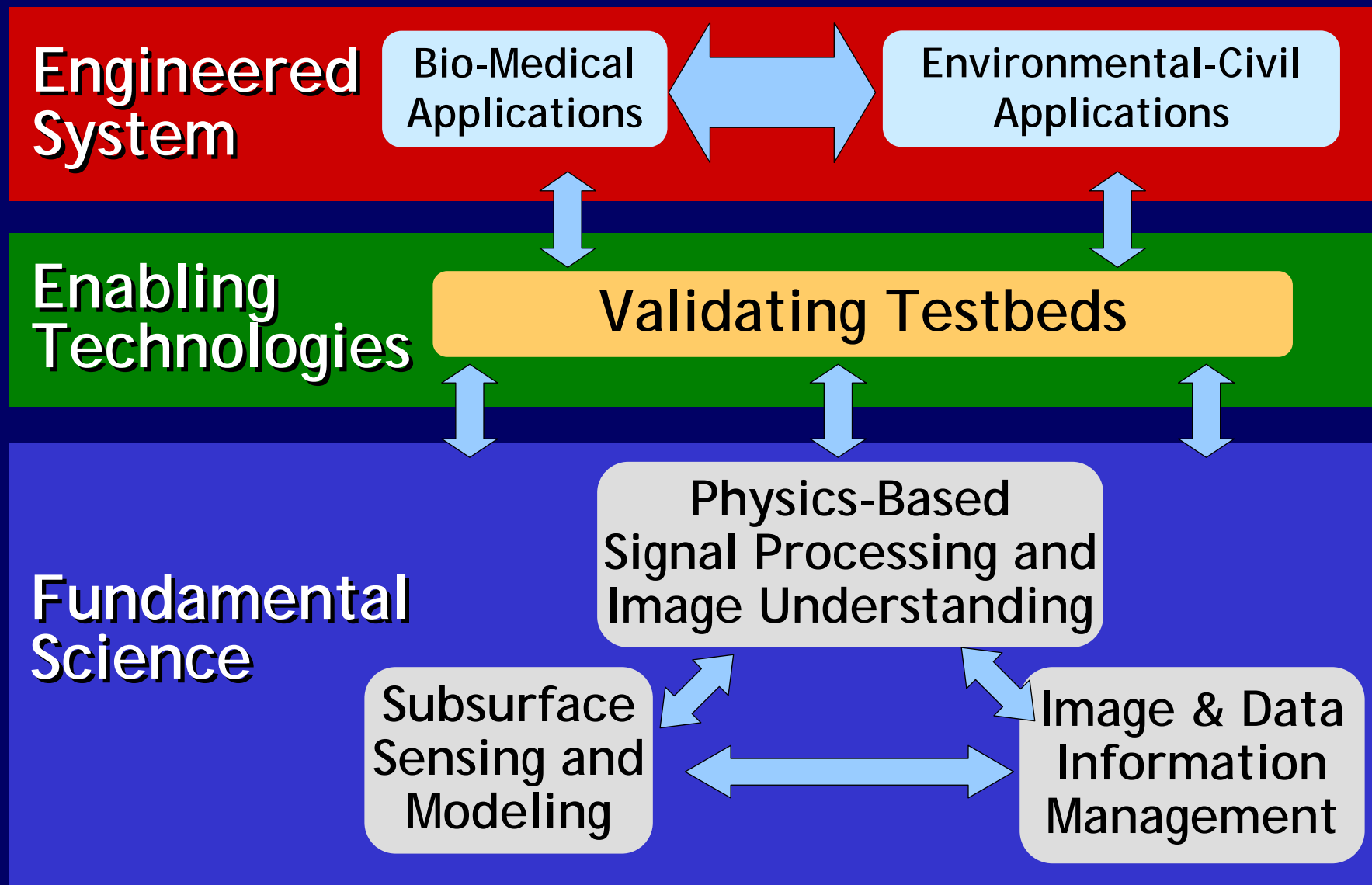


Colleagues

- **Rensselaer Polytechnic Institute**
 - Richard Radke (PhD), Daniel Freedman (PhD), Charles Stewart (PhD), Gang Lin (PhD), Howard Tanenbaum (MD), Anna Majerovics (MD)
- **Mass General Hospital**
 - George T. Y. Chen (PhD), Evangelos Gragoudas (PhD), Noah Choi (MD), Eike Rietzel (PhD)
- **Memorial Sloan Kettering**
 - D. Michael Lovelock (PhD), Andrew Jackson (PhD)
- **Woods Hole**
 - Ali Can (PhD), Hanu Singh (PhD)
- **Boston U.**
 - Bahaa Saleh (PhD)



Overview of the CenSSIS Research Program





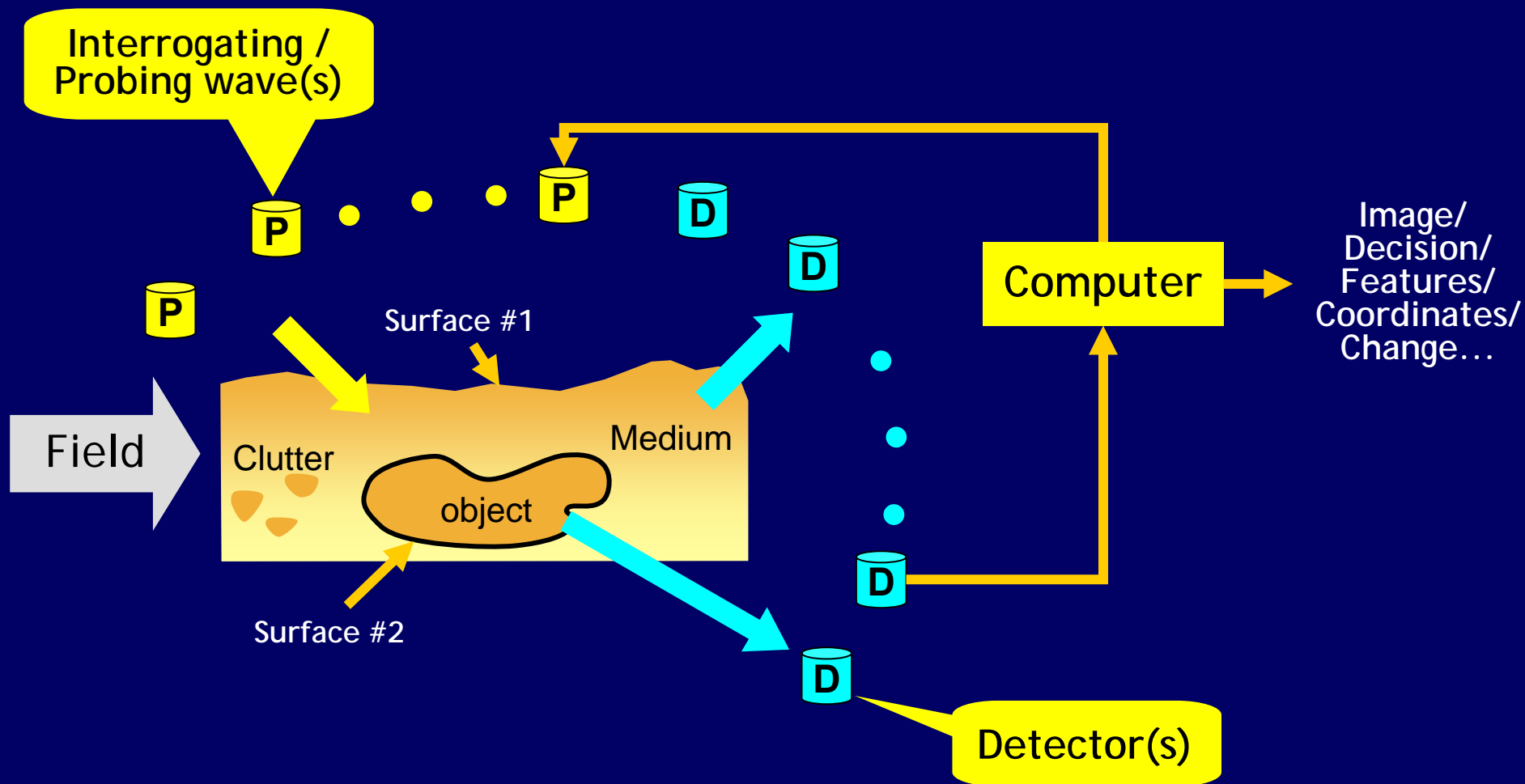
CenSSIS Themes

“Diverse Problems – Similar Solutions”

- A **unified view** of Subsurface Sensing & Imaging,
 - Optical, Electromagnetic and acoustic sensing modalities
 - Biomedical, biological, civil, industrial, and environmental applications
 - Emphasis on signal processing issues: Inverse problems, image reconstruction, image understanding, pattern recognition,...
- A **taxonomy and framework** for diverse SSI problems:
 - Physical, mathematical, and numerical models
 - Sensing and Imaging Architectures
 - Information Extraction Methods
 - LPM, MVT, MSD
 - Image & Change understanding
- Cross-application software **toolboxes** for rapid prototyping
- Hardware **testbeds** for **multi-sensor fusion** experiments



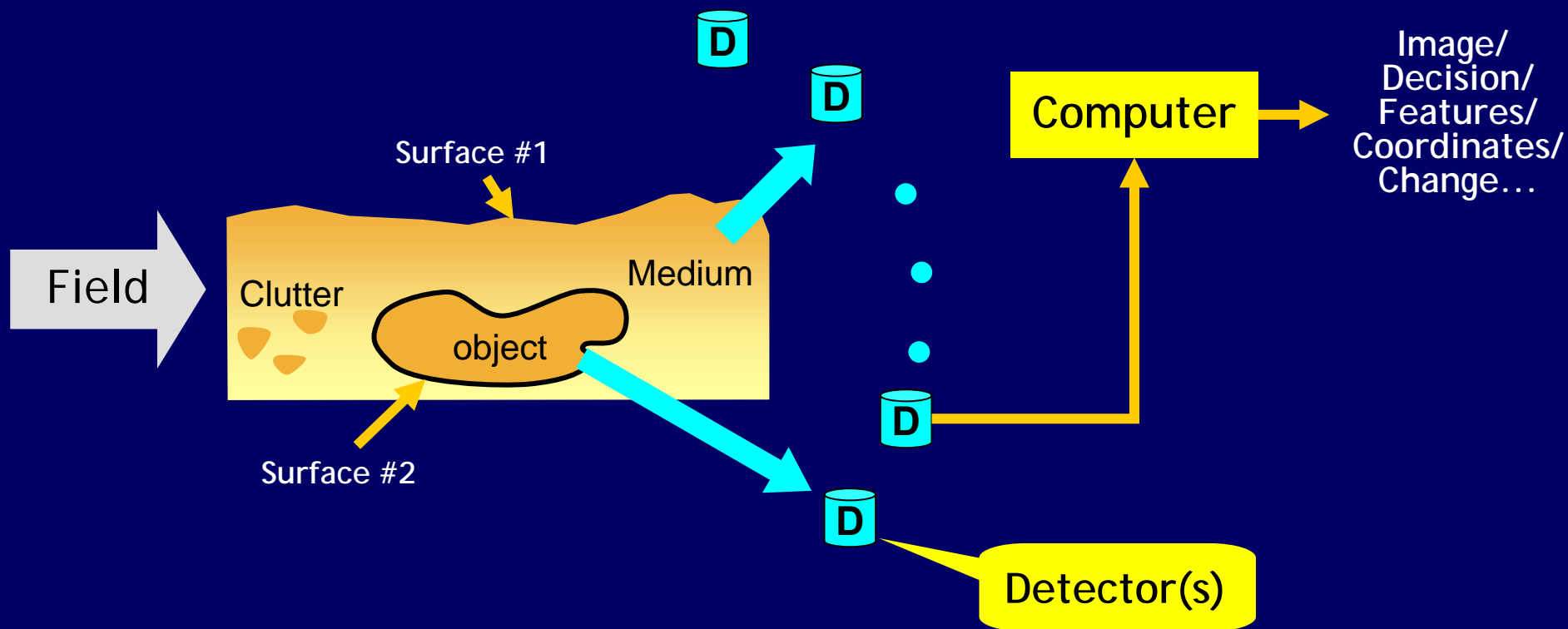
A Unifying View of Subsurface Sensing/Imaging Systems



The medium and object interact differently with the interrogating waves to generate detectable **contrast**.



Passive Subsurface Sensing/Imaging Systems



The medium and object emit differently to generate detectable **contrast**.



Many Choices for Imaging Systems

Excitation

Acoustic ↔ EM

Coherent ↔ Incoherent

Spatial Distribution

Spectral Distribution

(..RF ↔ THz ↔ IR-VIS-UV ↔ x-ray..)

Temporal Distribution

(CW ↔ Pulsed ↔ Modulated)

Polarized ↔ Unpolarized

Media/Target

- Emission
- Absorption
- Photoluminescence
 - Fluorescence,...
- Scattering
 - elastic ↔ inelastic
 - low ↔ high
 - linear ↔ non-linear
- Quantum effects:
 - entanglement
 - contrast agents
- Bulk Effects:
 - Reflection, refraction
 - Diffraction
 - Doppler
 - Polarization change
 - Dispersion
 - Phase change
 - Impedance

Detection

Coherent ↔ Incoherent

Near-field ↔ Far-field

Time-resolved ↔ Integrating

Spectral ↔ Narrowband

Spatial Distribution

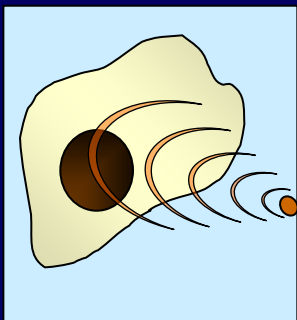
Spectral Distribution

Influence field



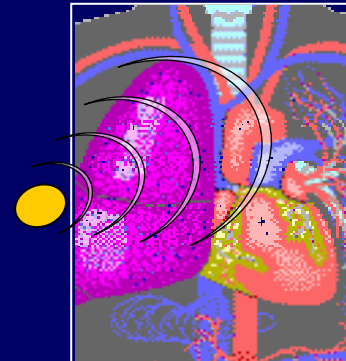
Scope of Center Activities

Sub-cellular Biology



100nm- 10 mm

Tissues & Organs

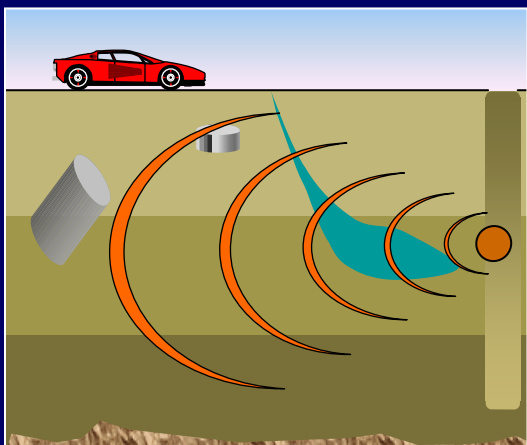


100 mm - 10 cm

Optics

Ultrasound

Underground Diagnosis

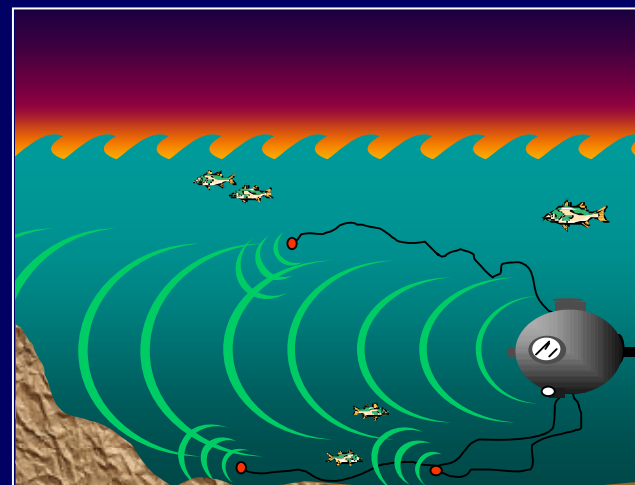


1 cm - 100 m

Radar

Sonar

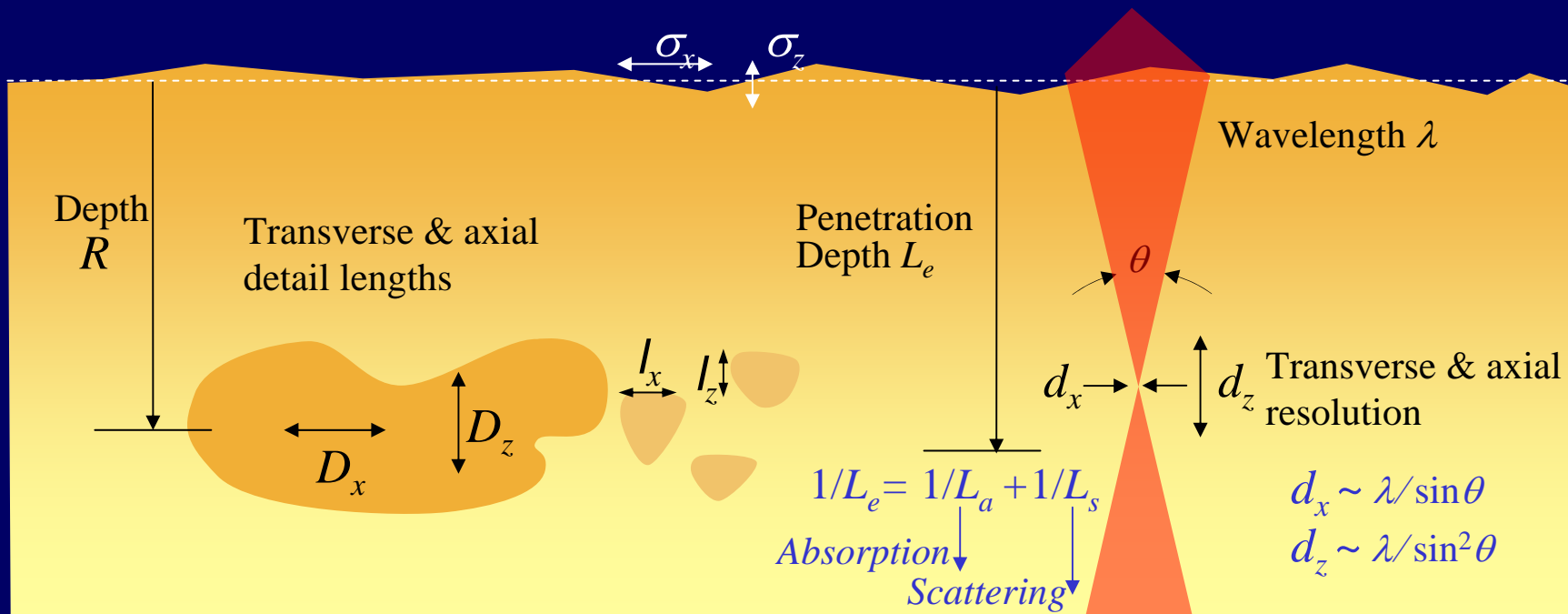
Underwater Exploration



10 cm - 1 km



Common General Considerations



Contrast Scales:

Object: $\Delta\alpha/\alpha_b$ or $\Delta k/k_b$

Surface: Impedance mismatch



Low contrast \rightarrow Weak Scattering

High contrast \rightarrow Strong Scattering

Spatial Scales:



$\lambda \ll D$

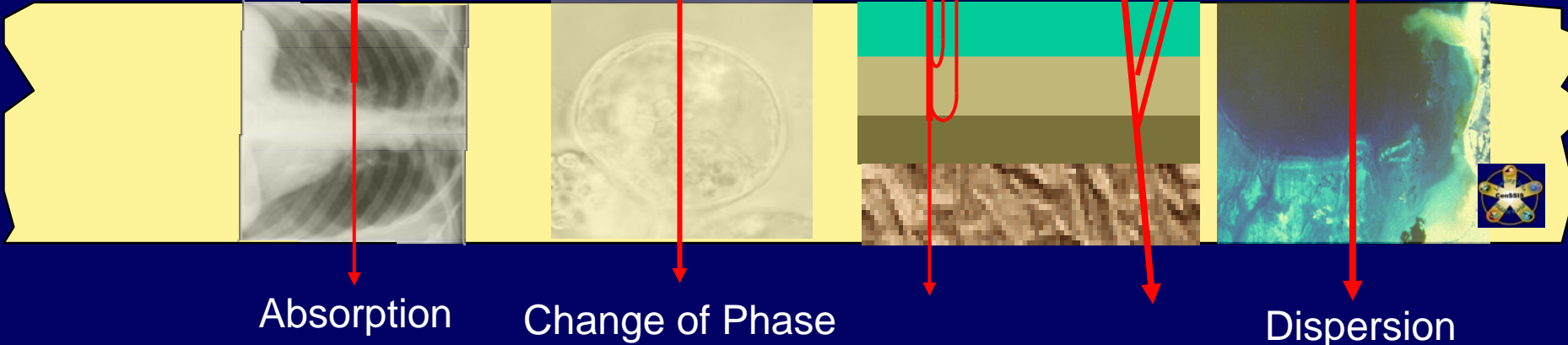
$\lambda \sim D$

$\lambda \gg D$

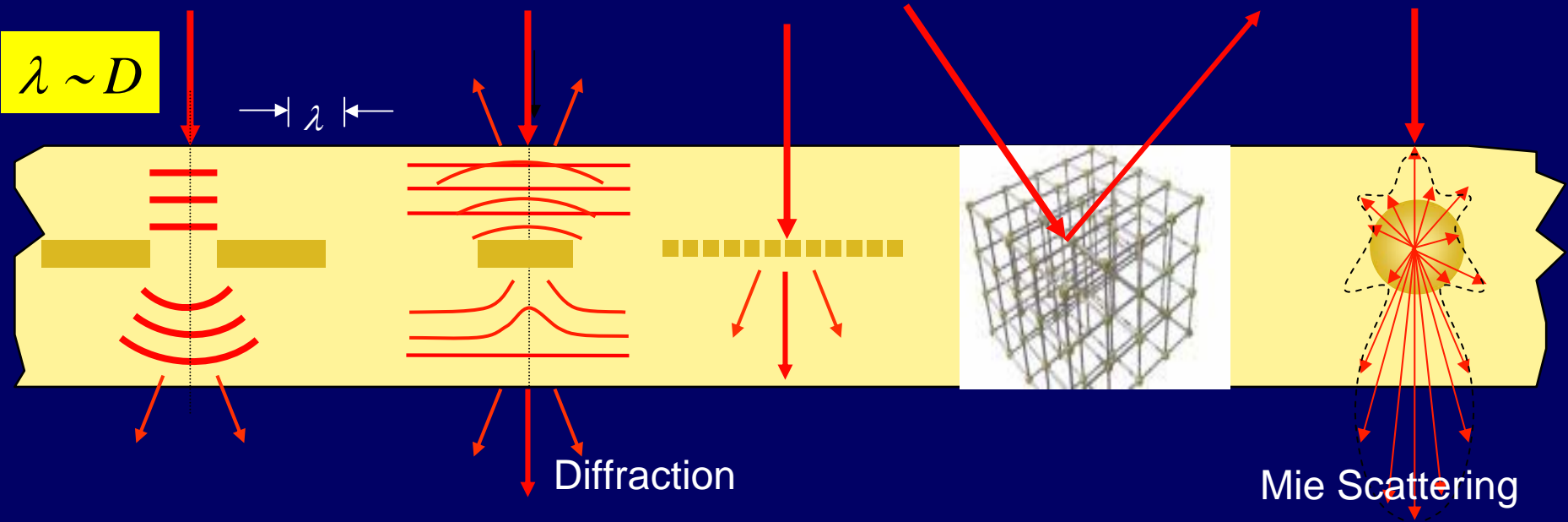


Common Wave-media Interactions

$\lambda \ll D$



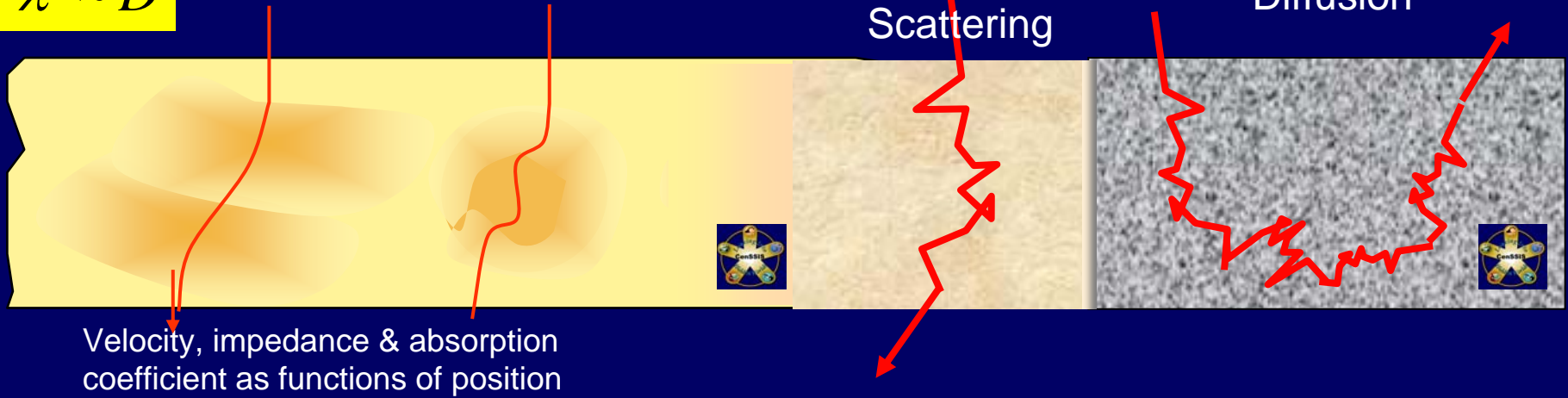
$\lambda \sim D$



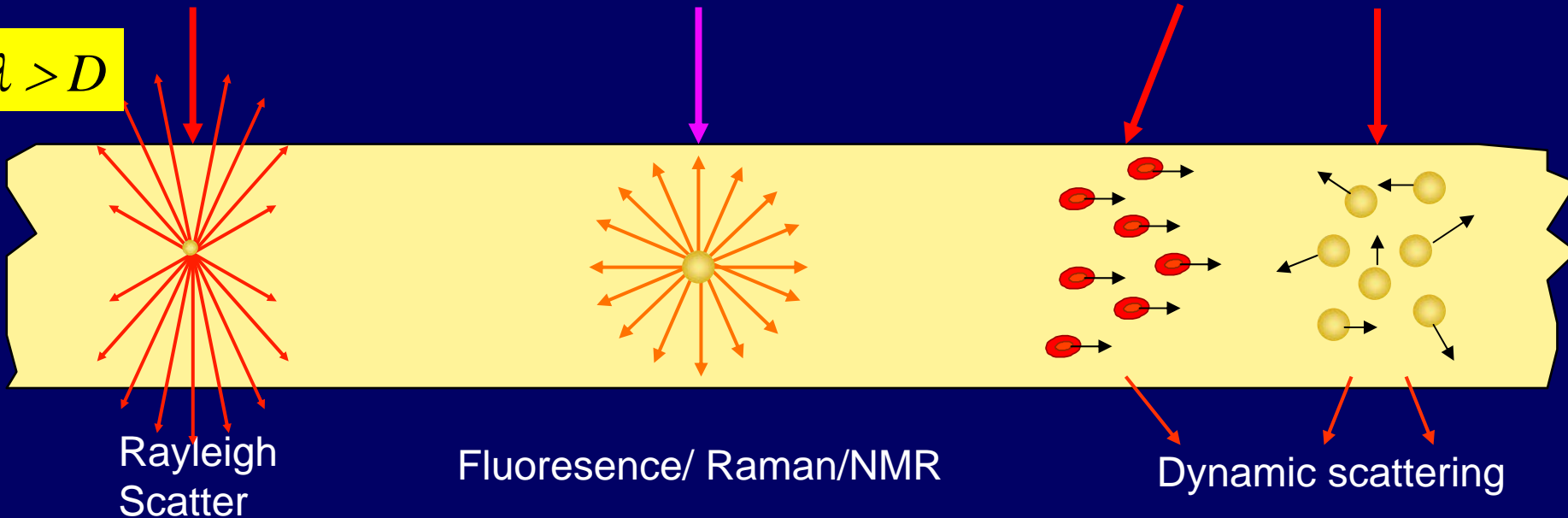


Common Wave-Media Interactions

$$\lambda \sim D$$

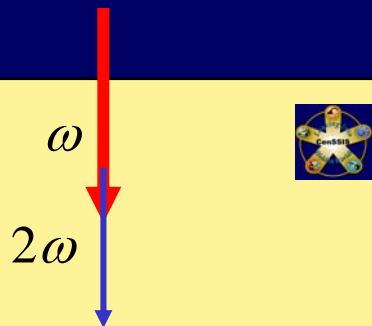


$$\lambda > D$$

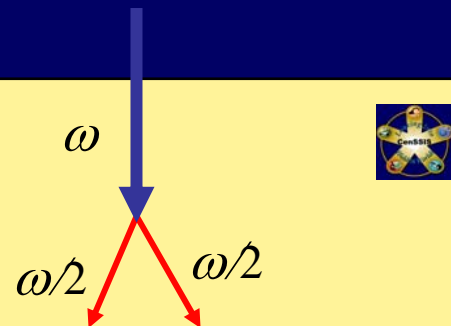




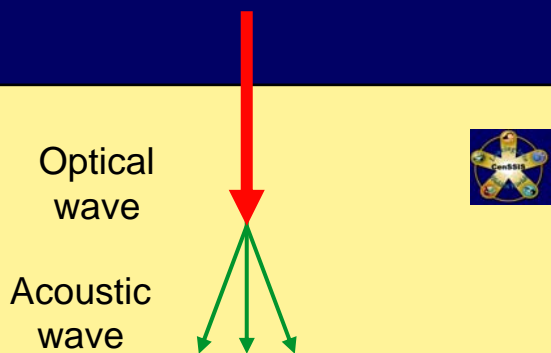
Nonlinear and Dual-Wave Interactions



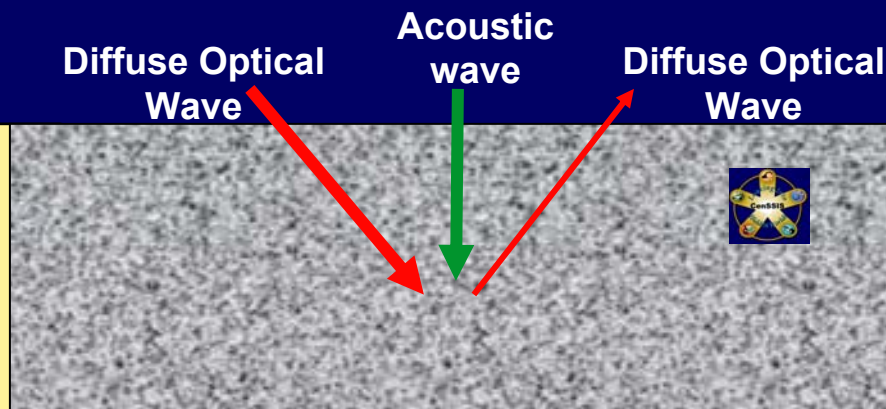
Up-conversion: Harmonic imaging



Down-conversion: Sub-Harmonic imaging



Opto-Acoustic Imaging (OAI)



Acousto-Optic Imaging (AOI)



What Are The Fundamental Science Barriers?

Barrier 1

Inadequate understanding of the physics of subsurface sensing and imaging

Barrier 2

Unreliable inversion methods for inhomogeneous and cluttered subsurface media

Barrier 3

Lack of robust, physics-based recognition and sensor fusion techniques



What Barriers Prevent the Development of an Integrated Engineered System?

Barrier 4

Lack of computationally efficient, realistic physical models

Barrier 5

Lack of optimal end to end sensor design methods

Barrier 6

Lack of rapid processing and management of large image databases

Barrier 7

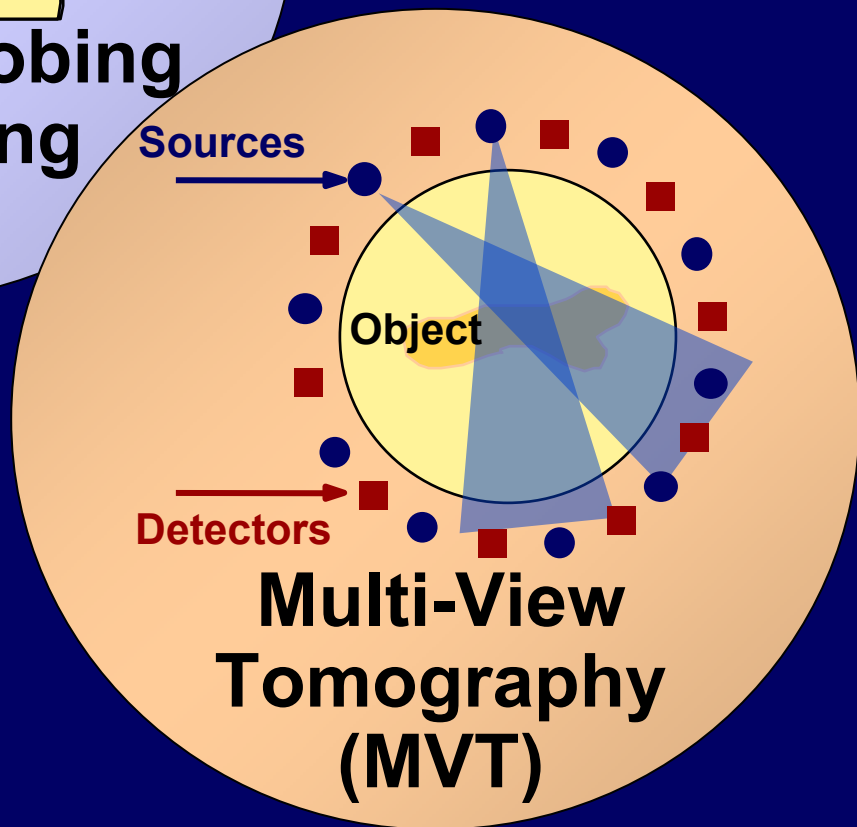
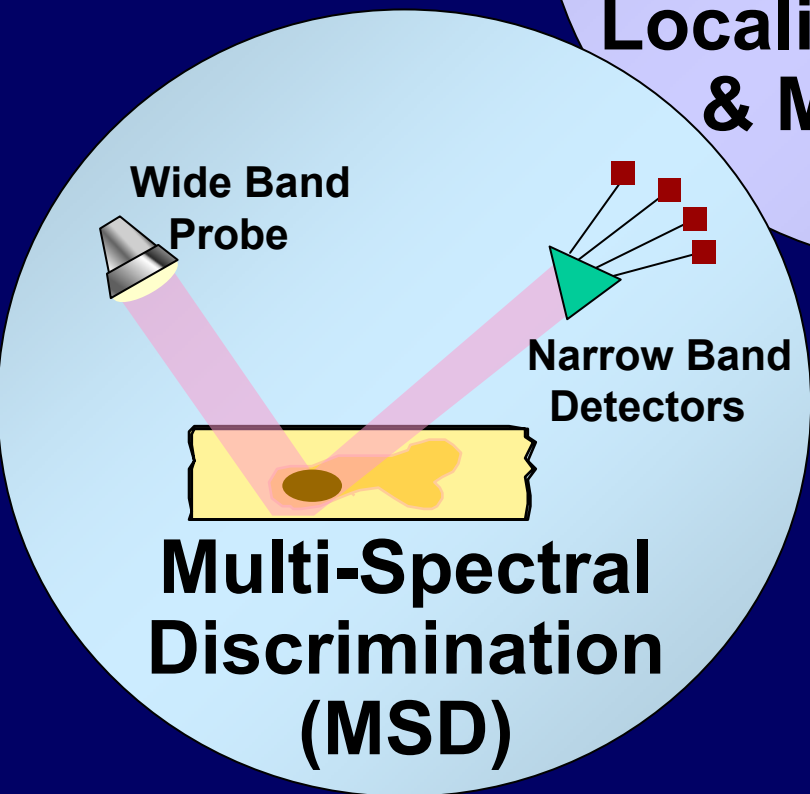
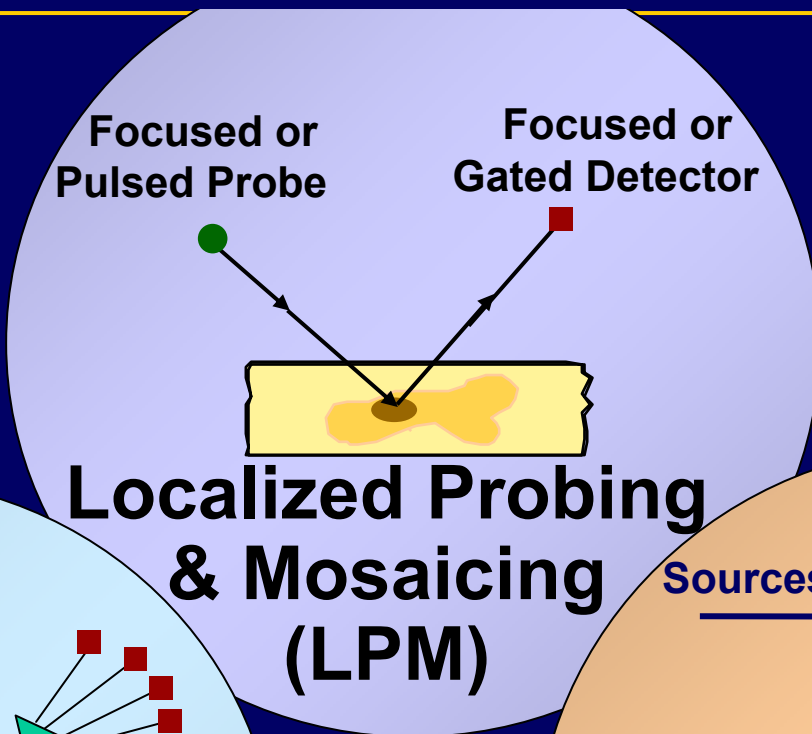
Lack of validated, integrated processing and computation tools

Barrier 8

Lack of a unified framework for diverse sensing and imaging modalities



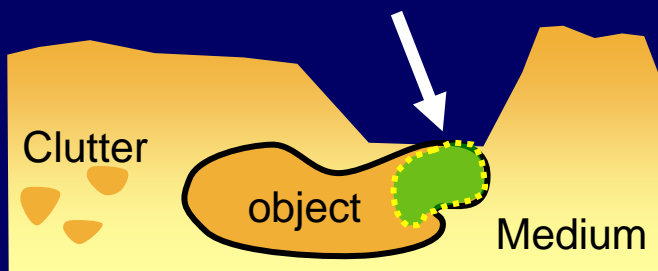
Principal Information Extraction Methods



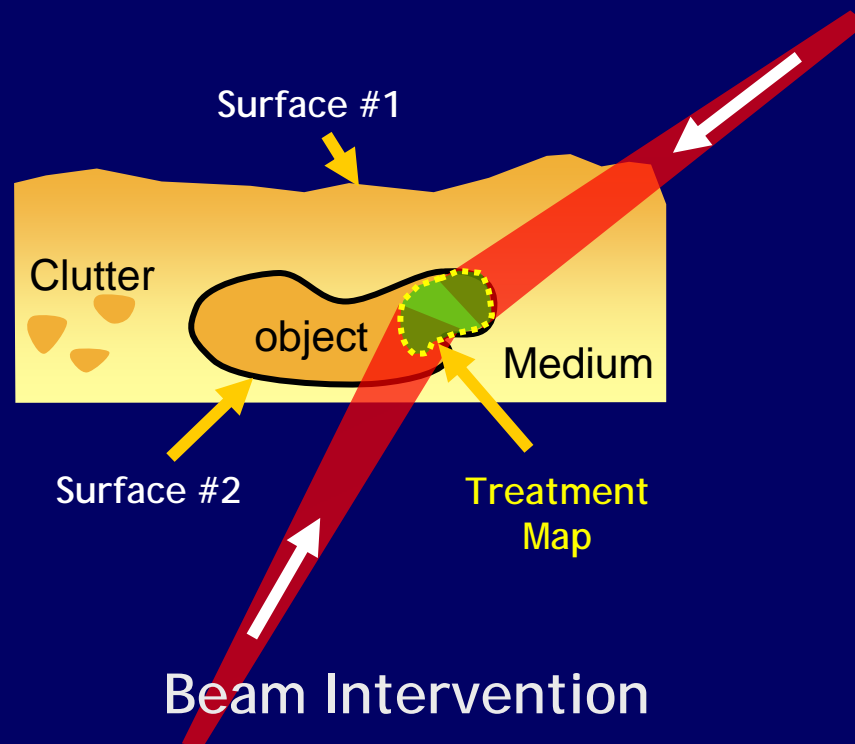
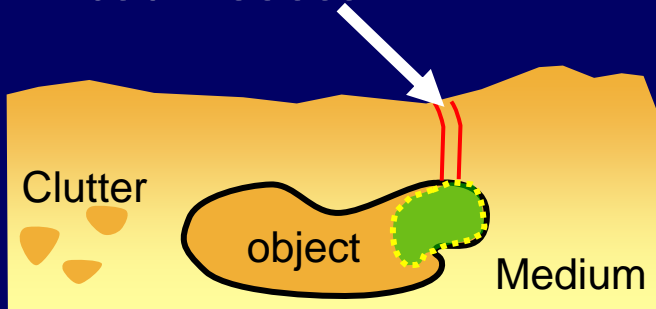


Subsurface Intervention Methods

Invasive Access



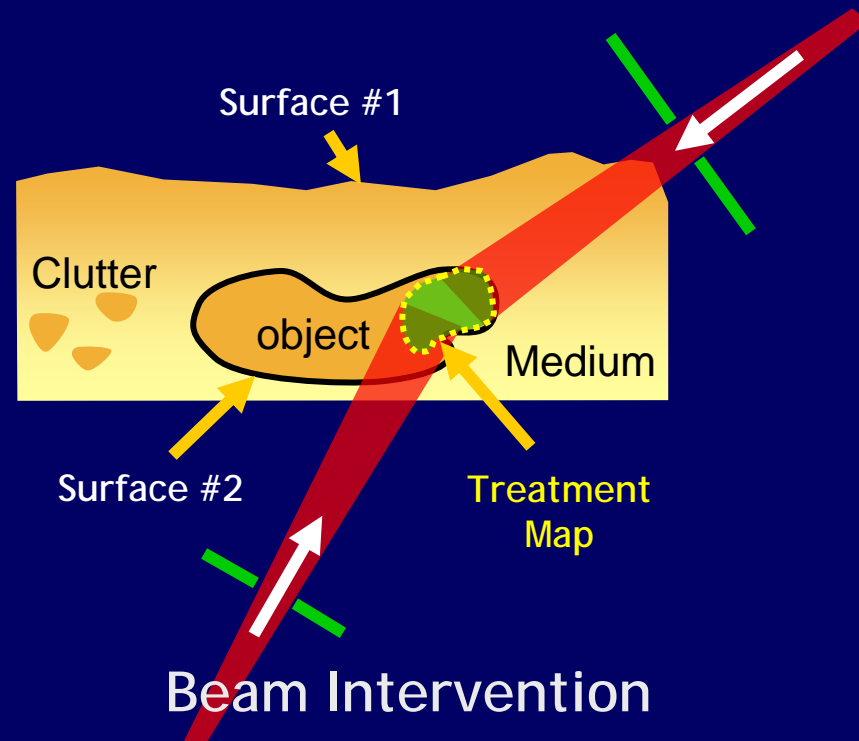
Limited Access





Beam Interventions

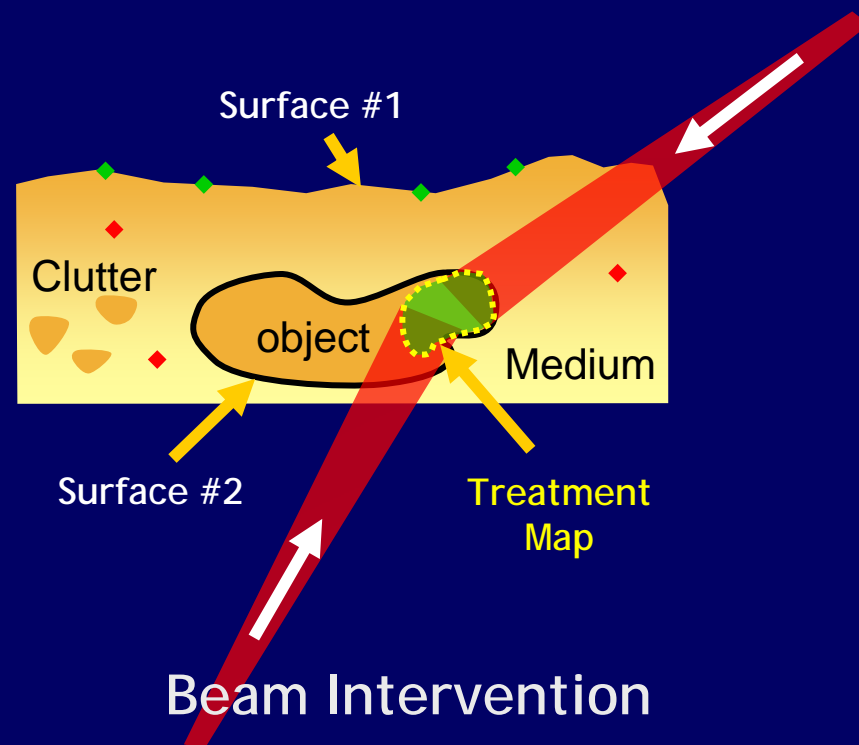
- **Common Beam Types:**
 - Optical (laser)
 - Acoustic (HIFU)
 - Radiation (x-ray, gamma ray, proton beam, ...)
- **Common Objectives:**
 - Achieve desired spatial dose distribution:
 - Full coverage of pathology
 - Minimize dose to background
 - Motion and deformation compensation
 - Conforming the beam to the treatment map
 - Integrated approaches to diagnosis, planning, execution, and follow up
- **Examples**
 - Laser retinal surgery
 - Radiation treatment of intra-ocular tumors
 - Radiation treatment of cancer of lung, prostate, ...





Beam Interventions (...contd)

- **Common issues:**
 - Availability/otherwise of implantable marker targets
 - Relating several coordinate systems:
 - Imagery & coordinates of the surface and the subsurface
 - Marker targets
 - Imaging and Beam coordinate systems
 - Identification of delicate neighboring structures to be avoided
 - Achieving adequate spatio-temporal sampling of moving 3-D structures
 - Minimizing damage from imaging probes





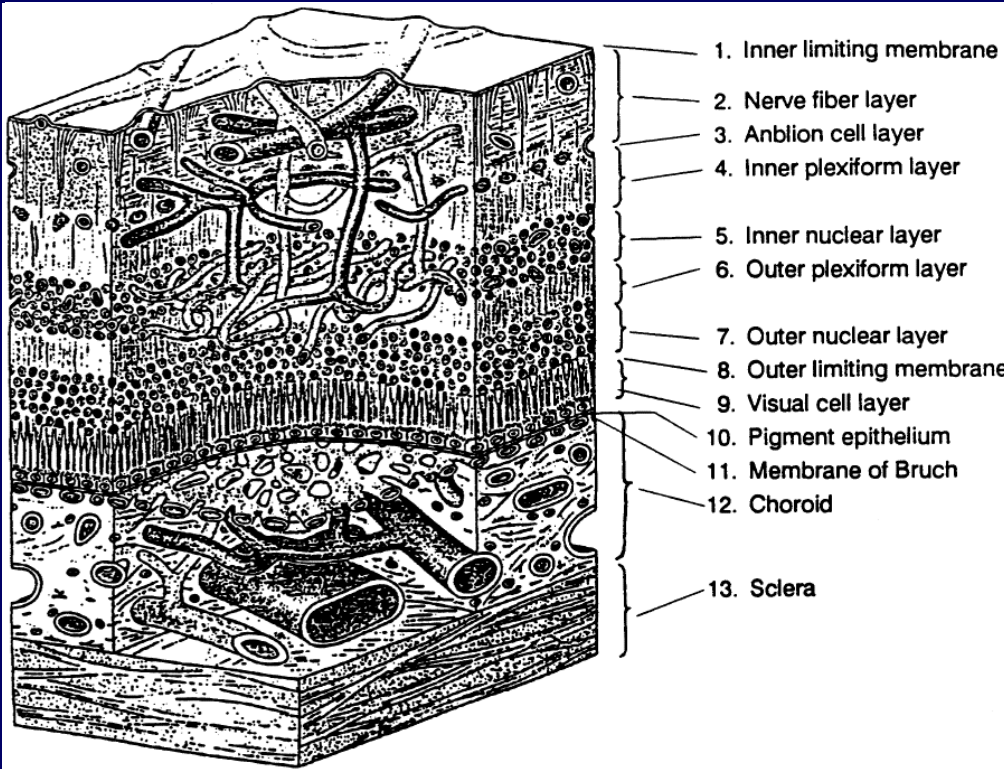
Before, During, and After Intervention

- **Before intervention**
 - Establishing a spatial reference map
 - Surface, subsurface, motions
 - Reliable detection of pathology
 - Accurate delineation of pathology & treatment map
 - Planning the intervention optimally
- **During intervention**
 - Precise knowledge and spatio-temporal control of dose
 - Maximize dose to pathology & minimize dose to other regions
 - Complete & stable visualization with context
 - Predictable real-time motion compensation & spatial referencing to map
 - Correction for patient pose and variable deformations
 - Responsibility and control
 - Spatial dosimetry
 - Alarms and safety cutoffs
 - Accounting for changes as they occur
- **After intervention**
 - Accurate assessment of changes inflicted by intervention
 - Updated planning for next intervention



Human Eye and Retina

webvision.med.utah.edu

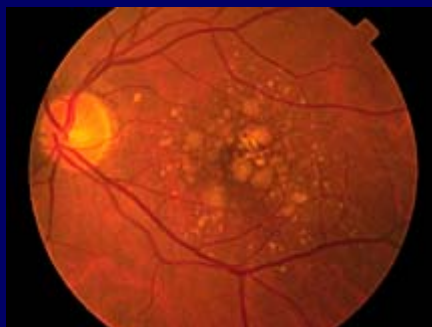


- **Leading Causes of Blindness**
 - **Age-Related Macular Degeneration**
 - **Diabetic Retinopathy**
 - **Glaucoma**
 - **Retinopathy of Prematurity**
- **Laser Retinal Surgery = Best-available Treatment**
- **Failure Rate \approx 50%**

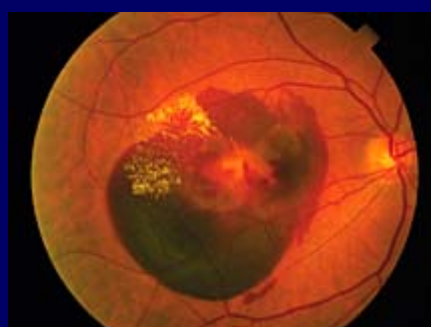
Macula.org



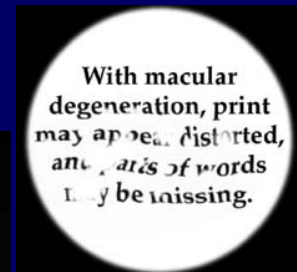
Early AMD



Dry AMD



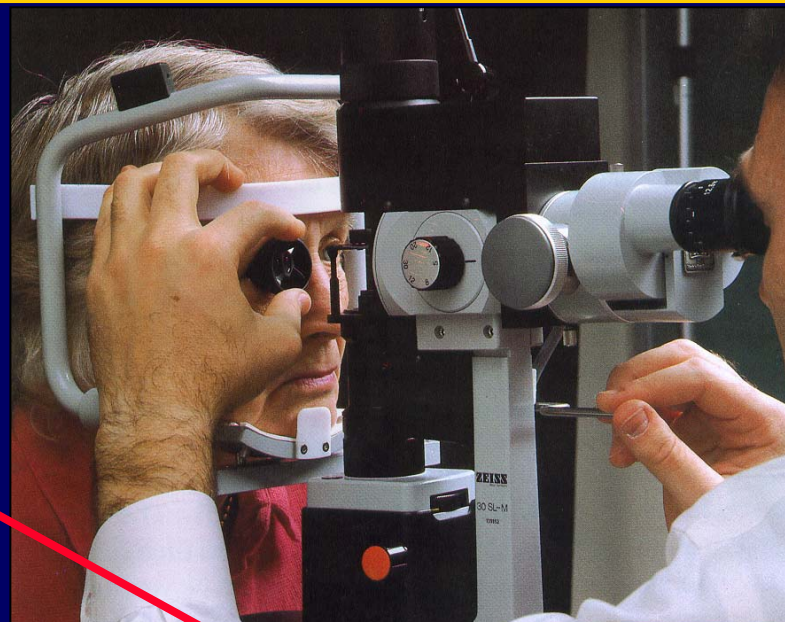
Wet AMD



Scotoma



Current State of the Art



6569
08-02-93



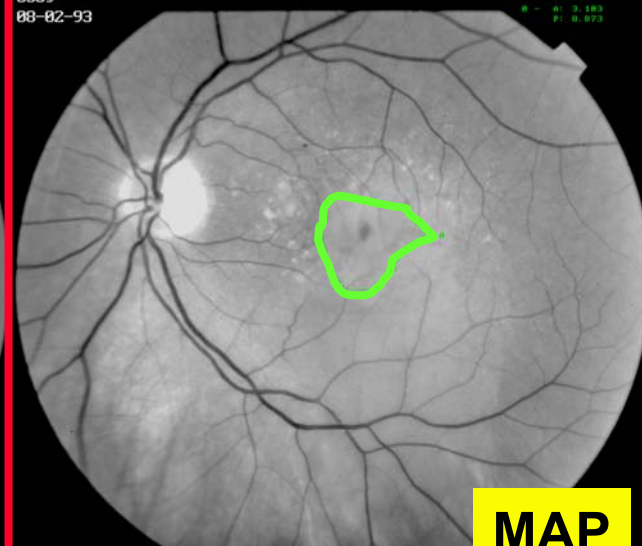
Green

6569
08-02-93



Infrared

6569
08-02-93



MAP

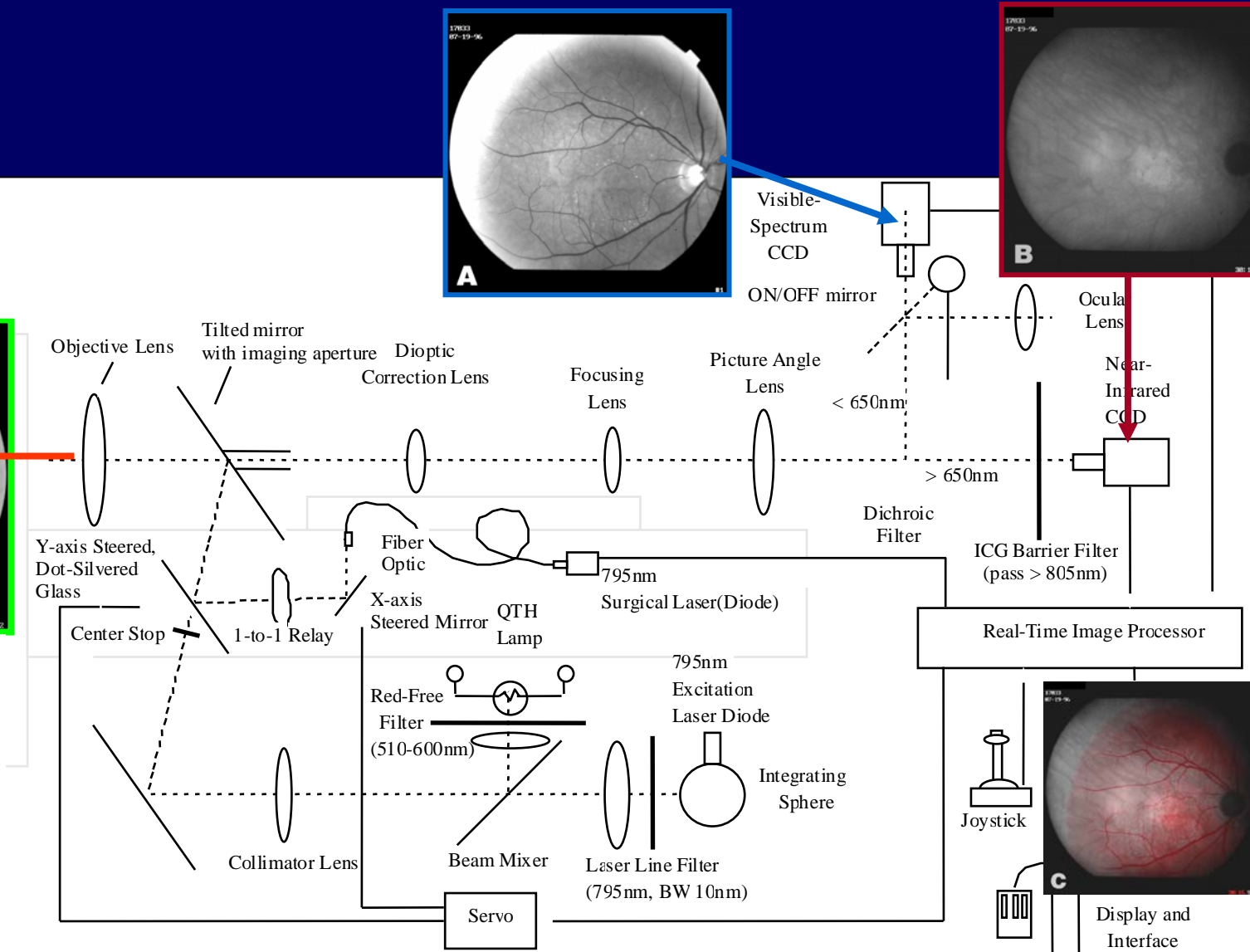
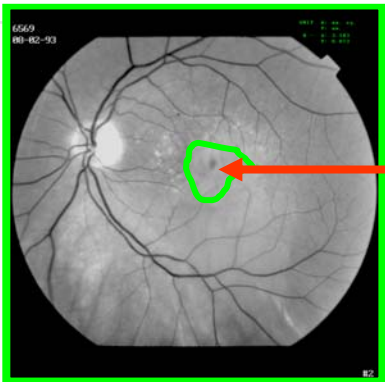
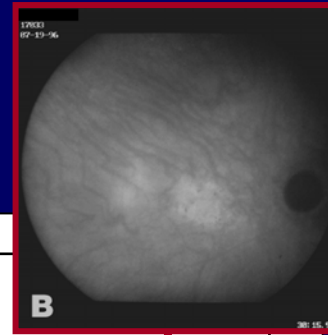
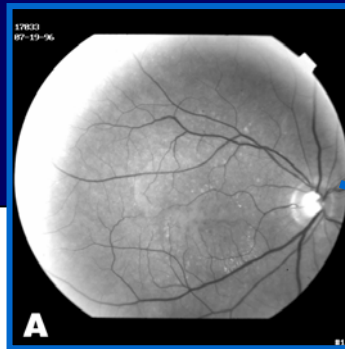


What can we engineers do to help?

- **Develop an integrated solution**
 - **Optical hardware:**
 - Multi-spectral imaging
 - Assisted laser guidance and safety shutoffs
 - **Computer Software:**
 - Establish a spatial map based on computer image analysis
 - Map-based spatial referencing and tracking for beam delivery
 - Tools to integrate with diagnosis, planning, and delivery
 - **Computer Hardware:**
 - Enable predictable real-time computing
 - Enable fast (parallel) computing



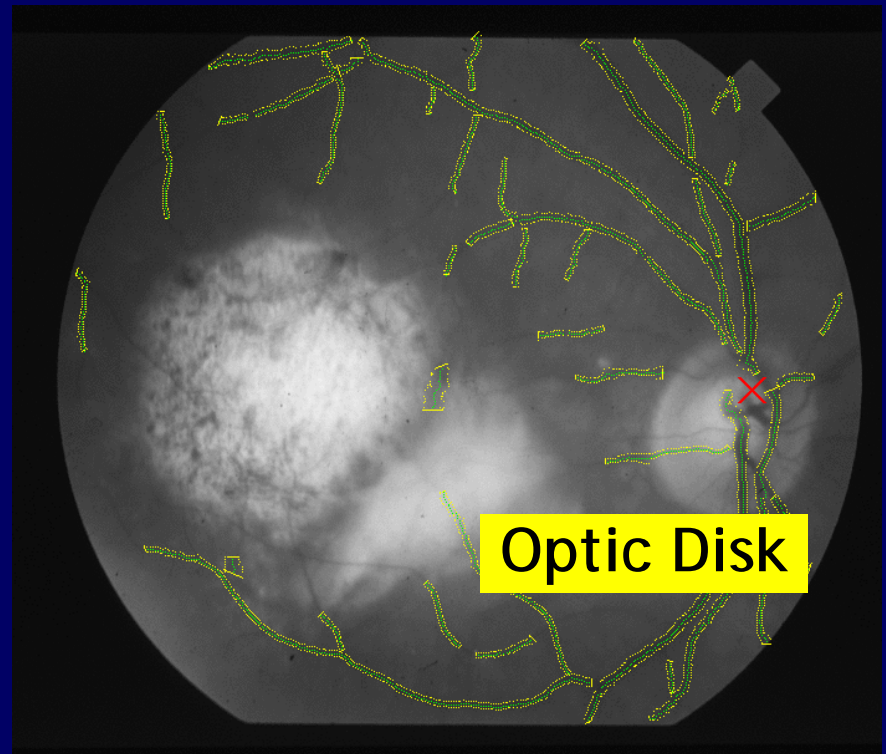
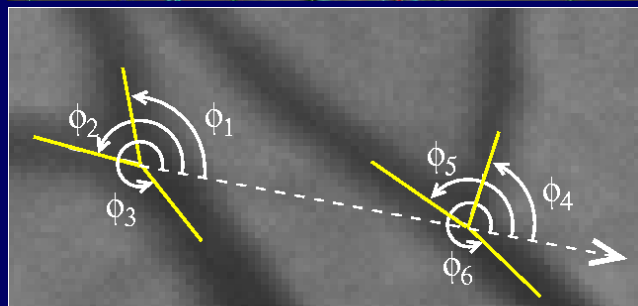
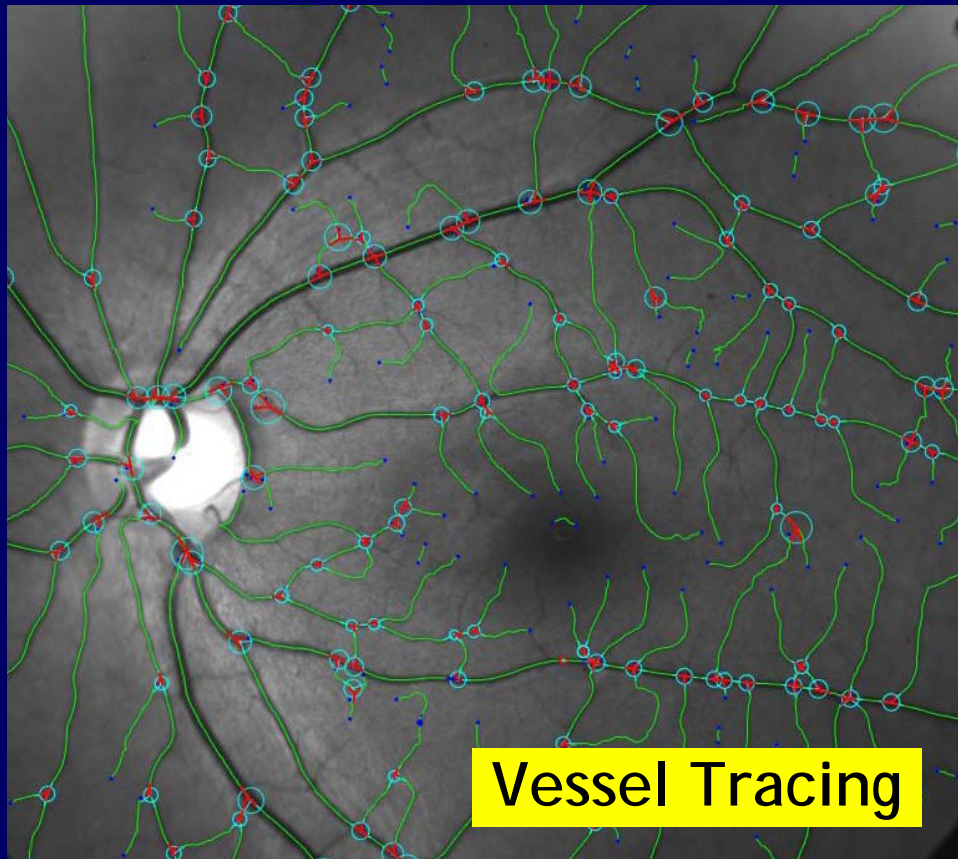
Towards a Smarter, Integrated System





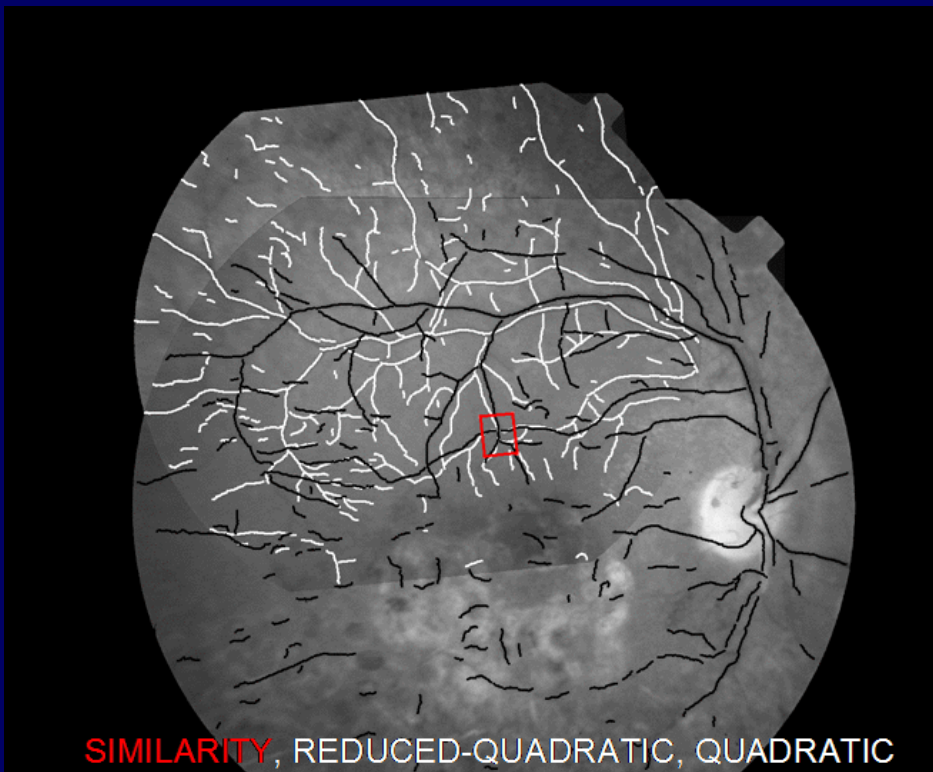
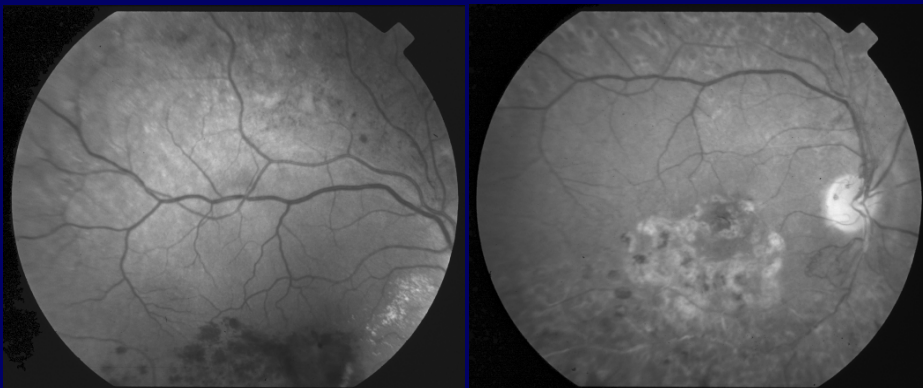
What it takes: Fast feature Extraction

- Fast and automatic
- Sub-pixel traces and interest points
- Detailed vessel morphometry





What it takes: Precise Registration

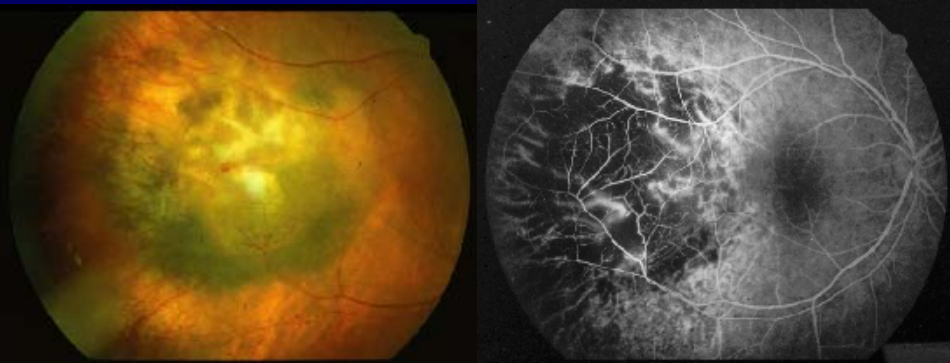


Main Ideas:

- 12-D model for the **curved retina** imaged by uncalibrated camera
- Dual-bootstrap registration:
 - Minimum initialization needed
 - Robust hierarchical estimation
 - Automatic model selection
 - Grow estimation zone based on uncertainty (view)
- Performance:
 - Large-scale Testing w/ 15,000 image pairs, 46 eyes covering 5 major diseases, up to 5 years apart
 - **99.5% success rate**

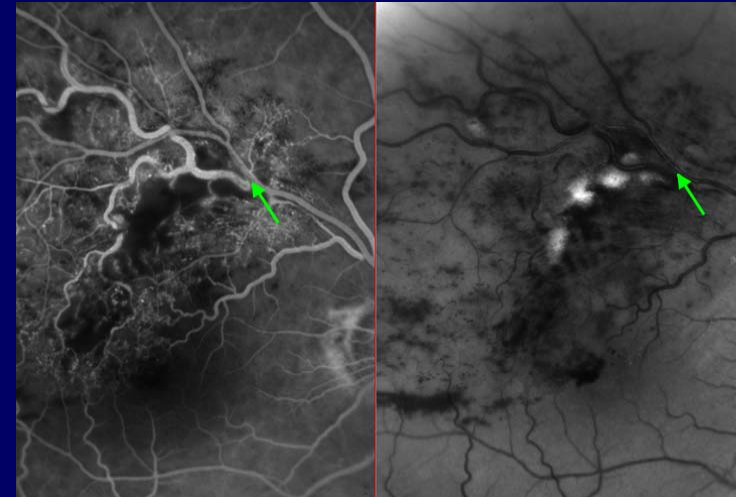


What it takes: Cross-Modality Mapping

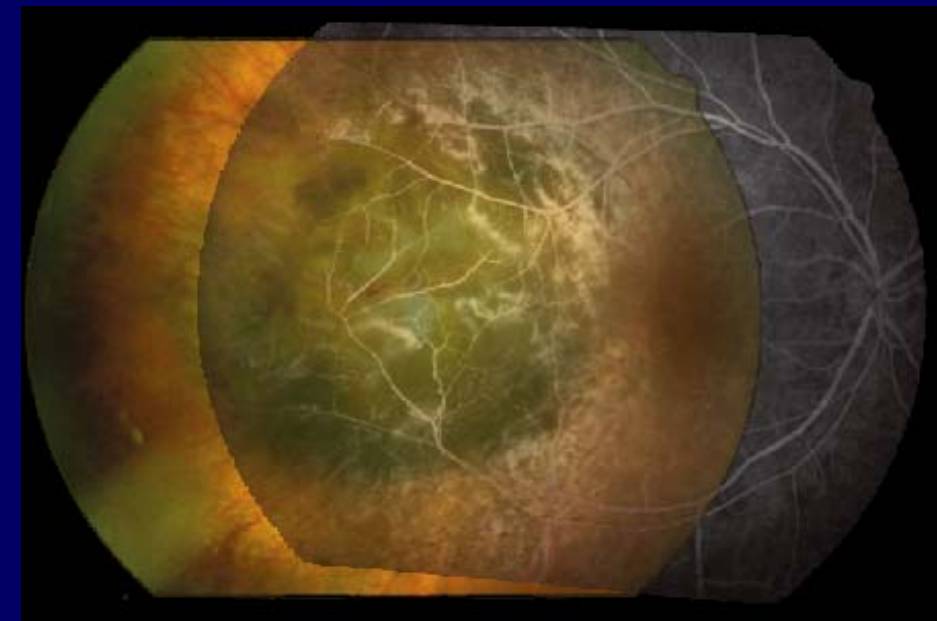


Visible

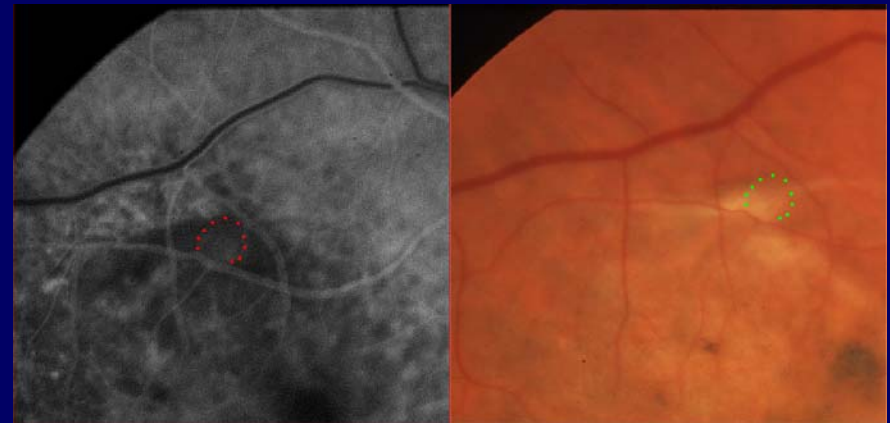
Fluorescein



Vein occlusion



Melanoma Example



Wet AMD

More Precise Mapping



Mapping Changes

BRVO w/ macular edema, neovascularization, ...



March 00



July 00



Sept 00

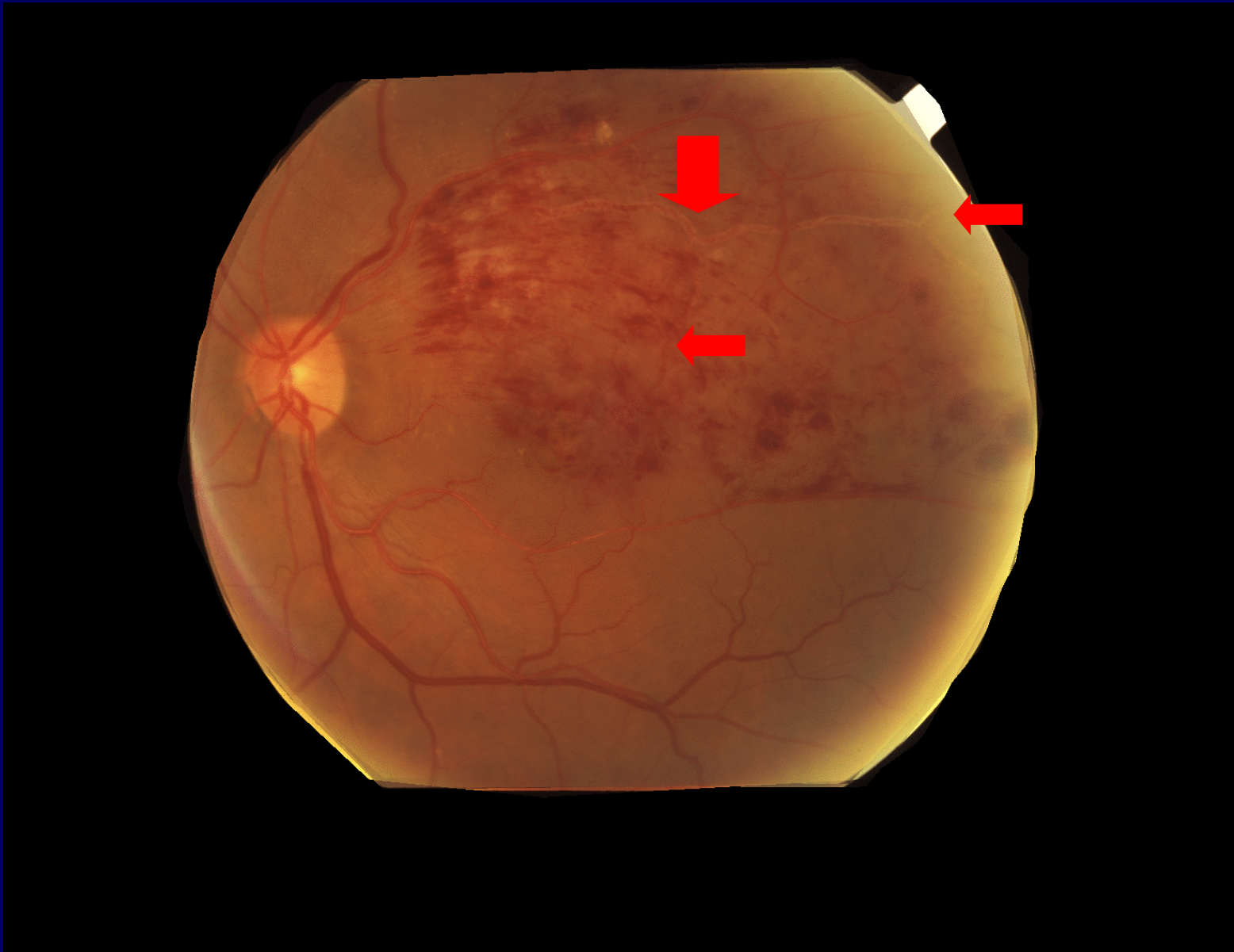


Feb 01

Data courtesy: Dr. A. Majerovics

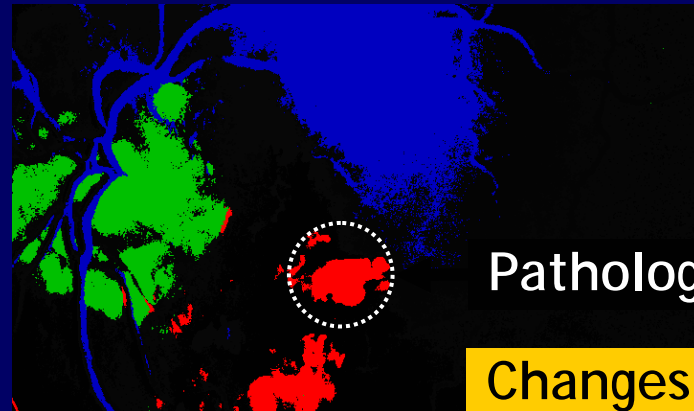
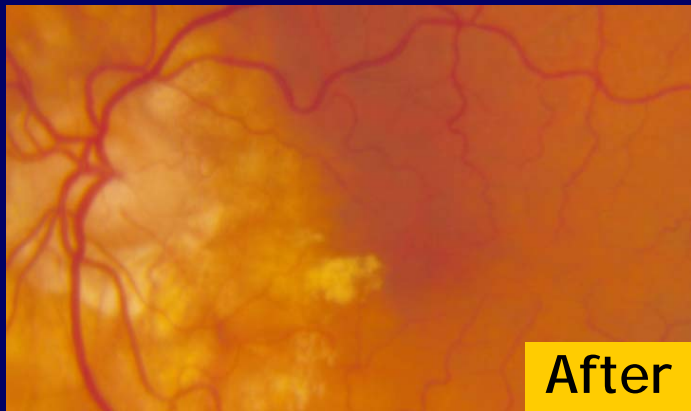
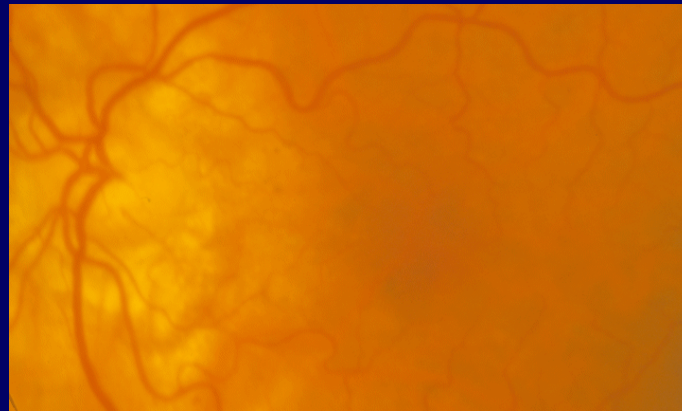


Registered Movie



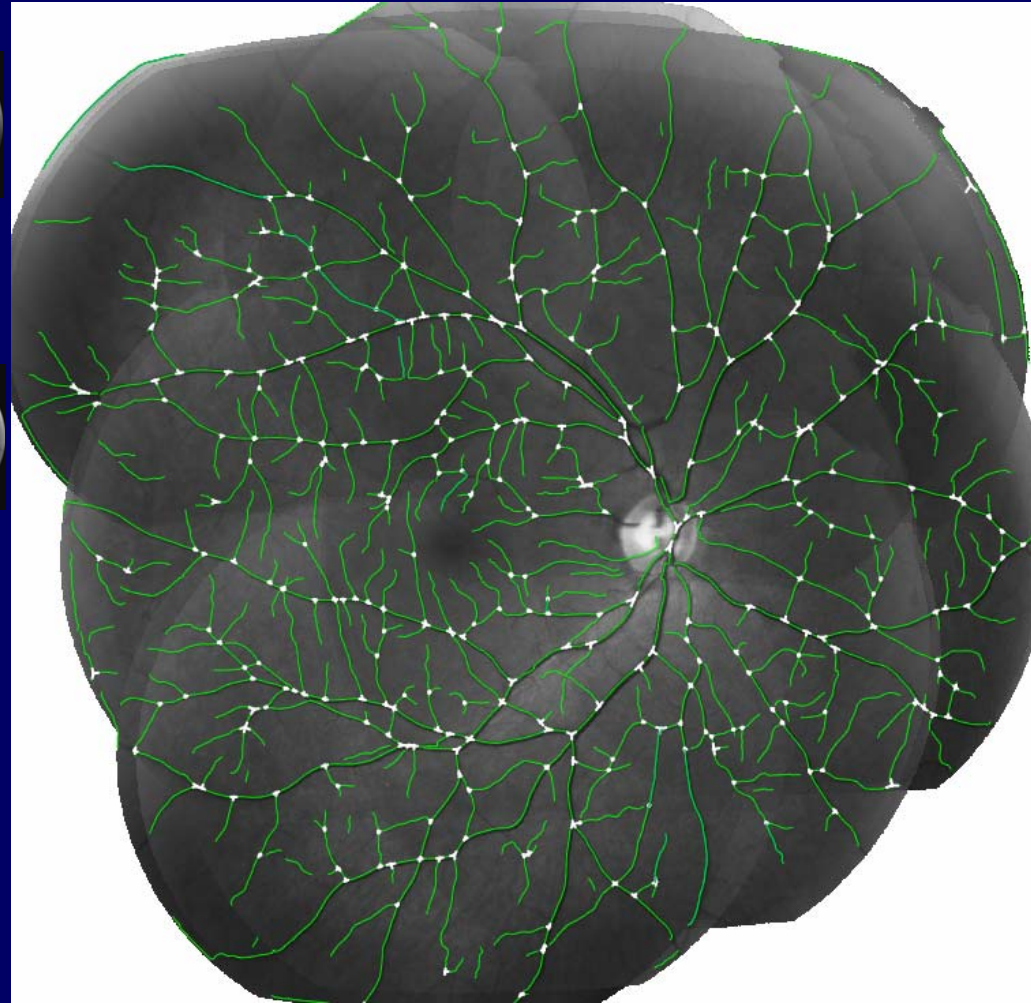
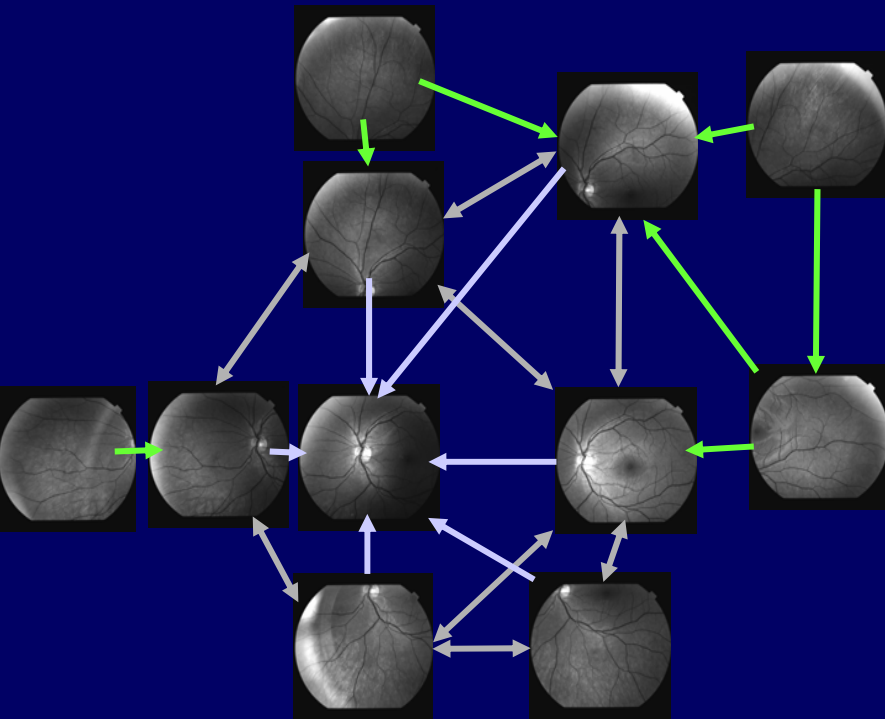


Change Detection



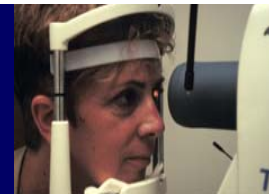


What it takes: Joint Mosaicing & Mapping



- **Direct applications**
 - Visualization
 - Corrections
 - Robust Change
- **Indirect applications:**
 - Basis for spatial mapping

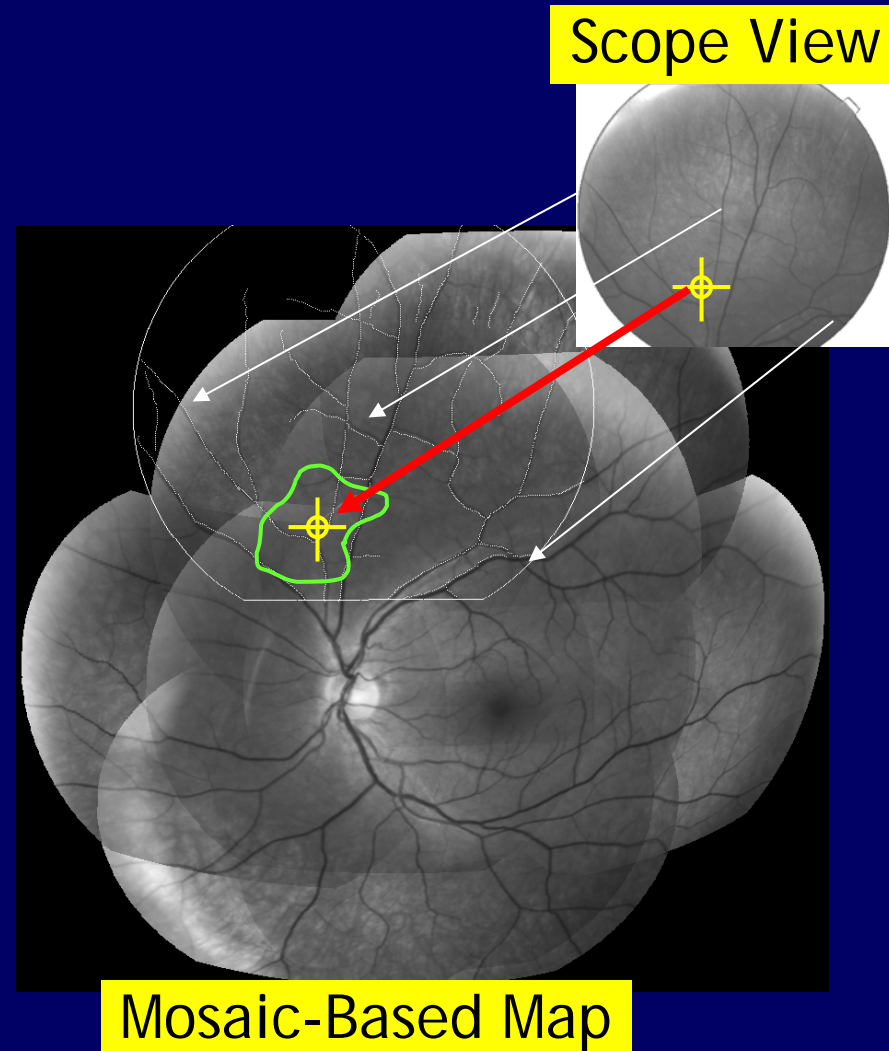
~ 70° Mosaic of Retina





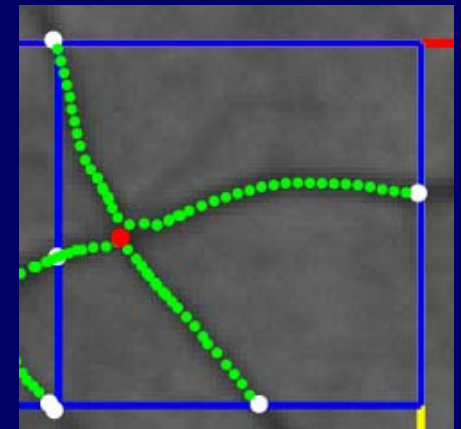
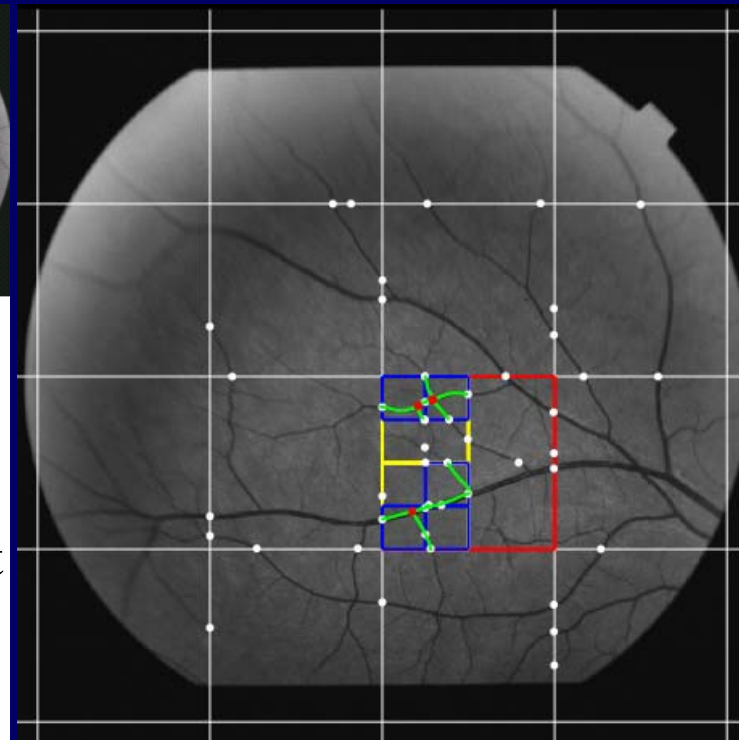
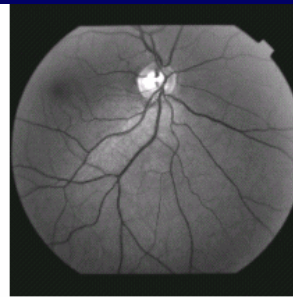
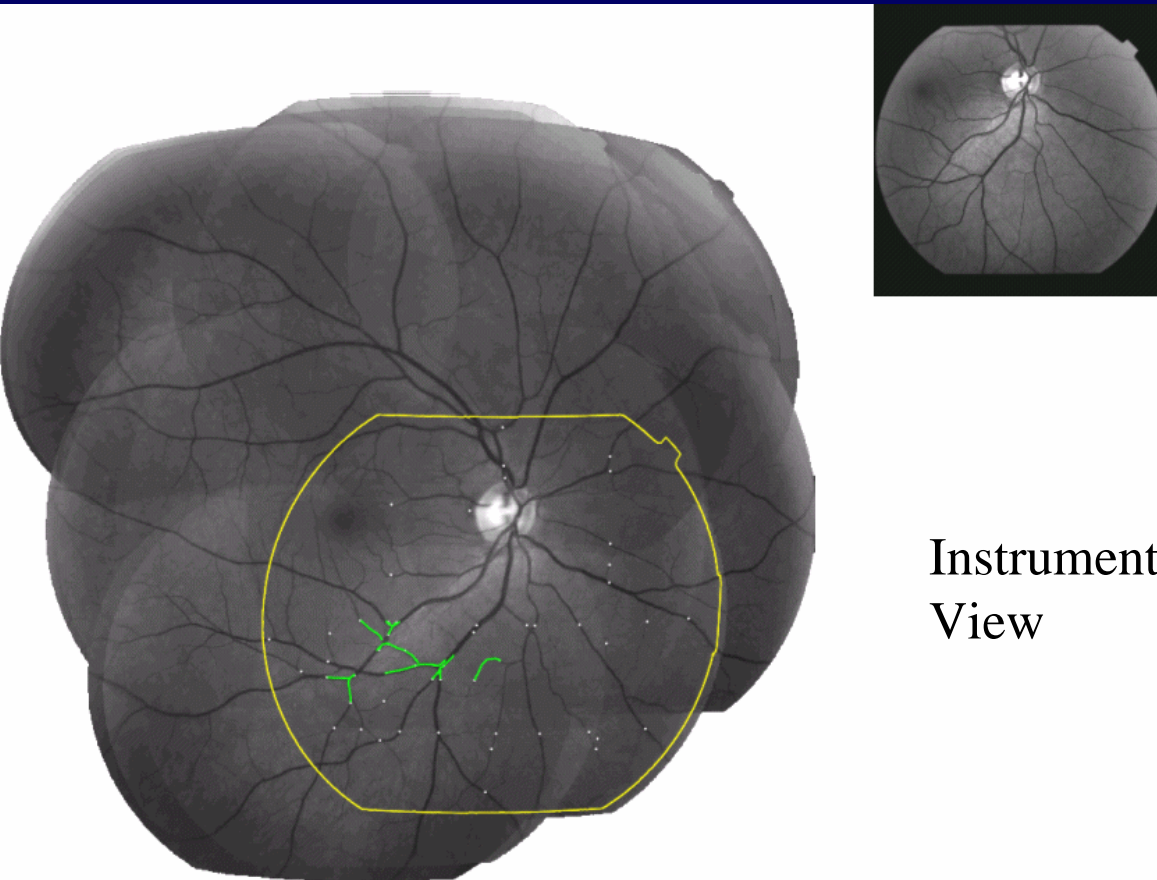
What it takes: On-line Registration

- Determine location of laser with respect to pre-computed spatial map
-
- Issues:
 - High variability
 - Inter-patient
 - Intra-patient
 - Speed (30-200fps)
 - High data rate (1M pixels x frame rate x channels)
 - Minimize light levels and total time
 - Camera sensitivity
 - Discomfort
 - Predictability for real-time control





Fast Map-based Positioning

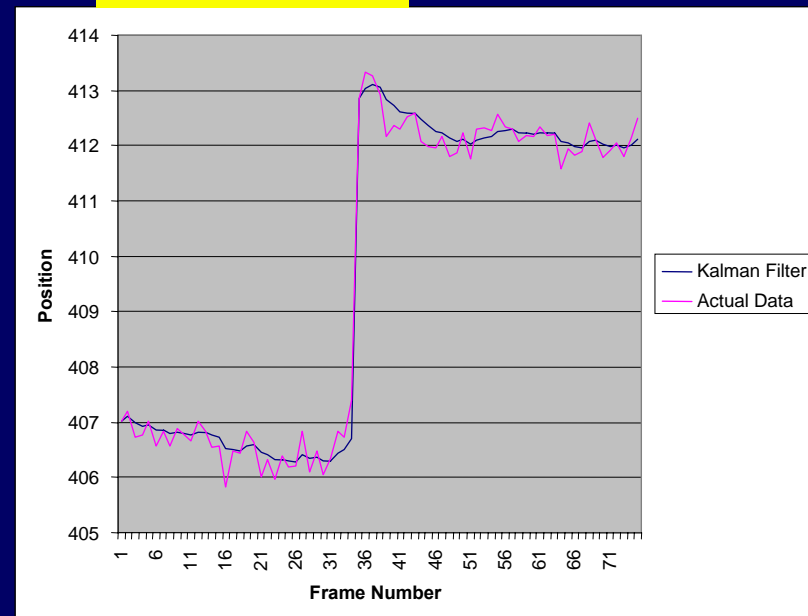
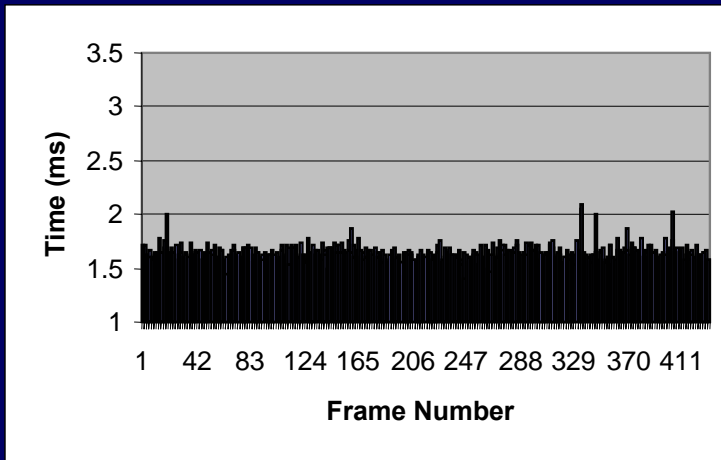
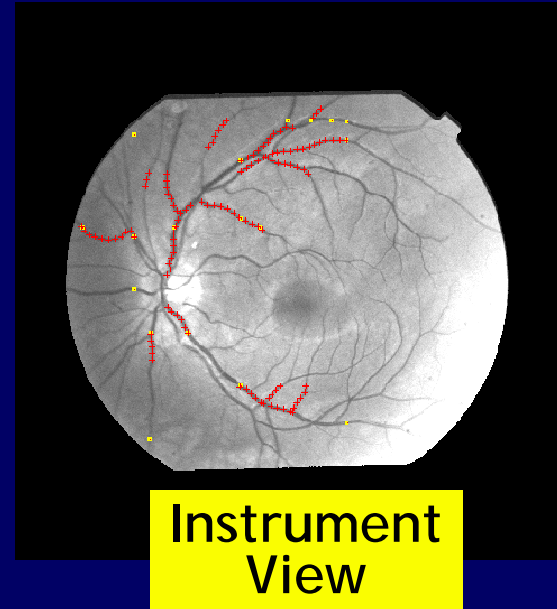
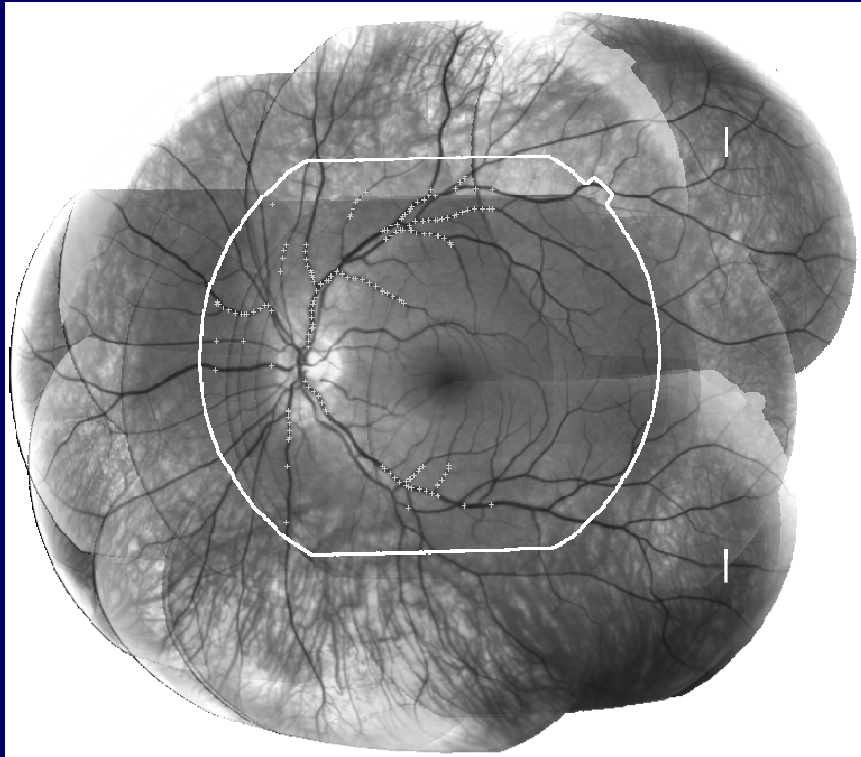


Key ideas:

Just-sufficient, opportunistic,
Progressive, imprecise computation
Atlas = Mosaics + structure indexing
database + treatment map



Hybrid Tracking and Referencing



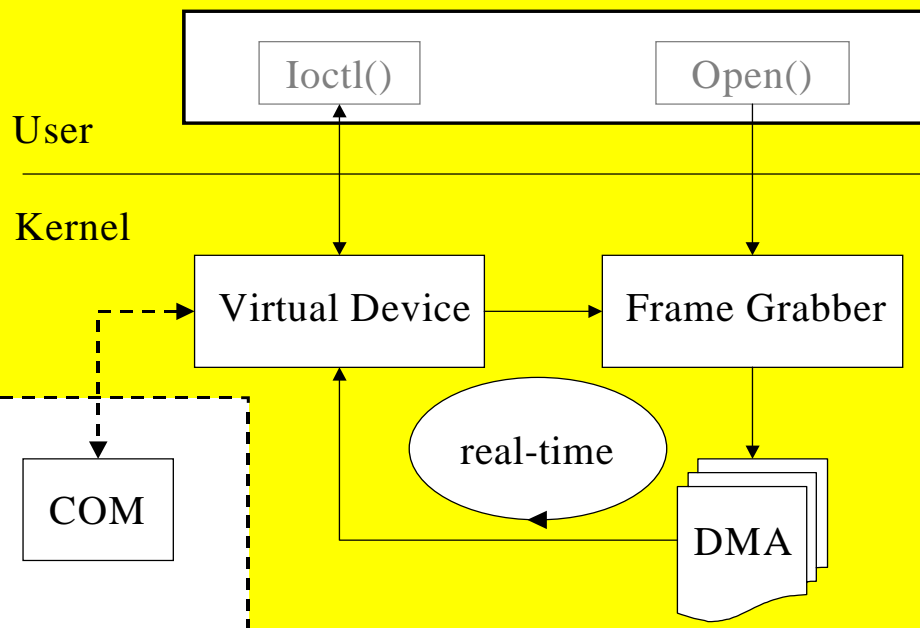


Real-Time Computing Issues

Off-Line
Vision Algorithm
Object Code

??

Real-time
Implementation



Issues:

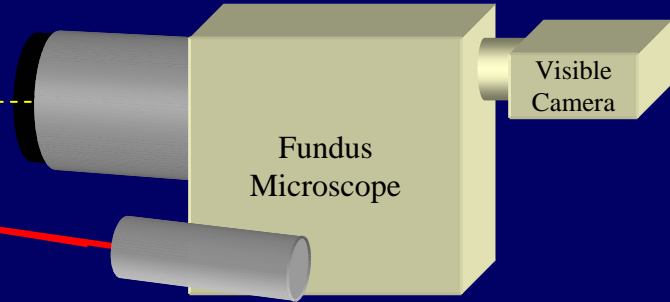
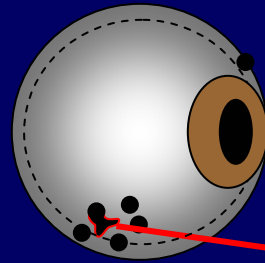
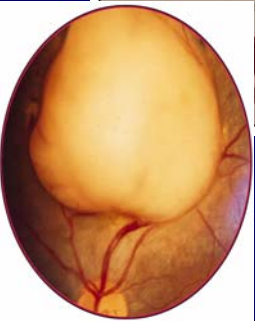
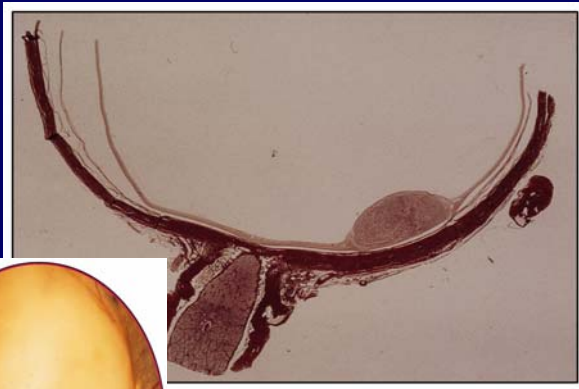
- **Large and complex code libraries** (`libc`, `vxl`, `libm`,...etc)
 - Too expensive to re-write, and evolve
 - Unpredictable operations such as dynamic memory allocation
- **Interrupts, Scheduling, Virtual Memory overheads, Computational efficiency.**
- **COTS a good match to exploratory vision code, hyper-threaded CPUs**

Solution:

- **Linux kernel-based virtual devices**

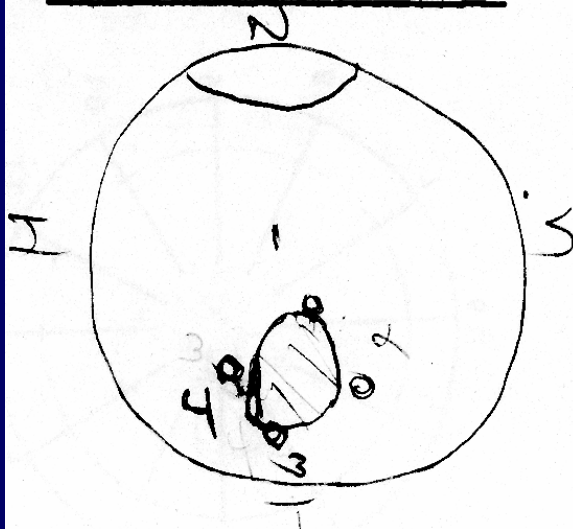


Treating Intra-Ocular Tumors



Proton Beam

Operating Room Drawing

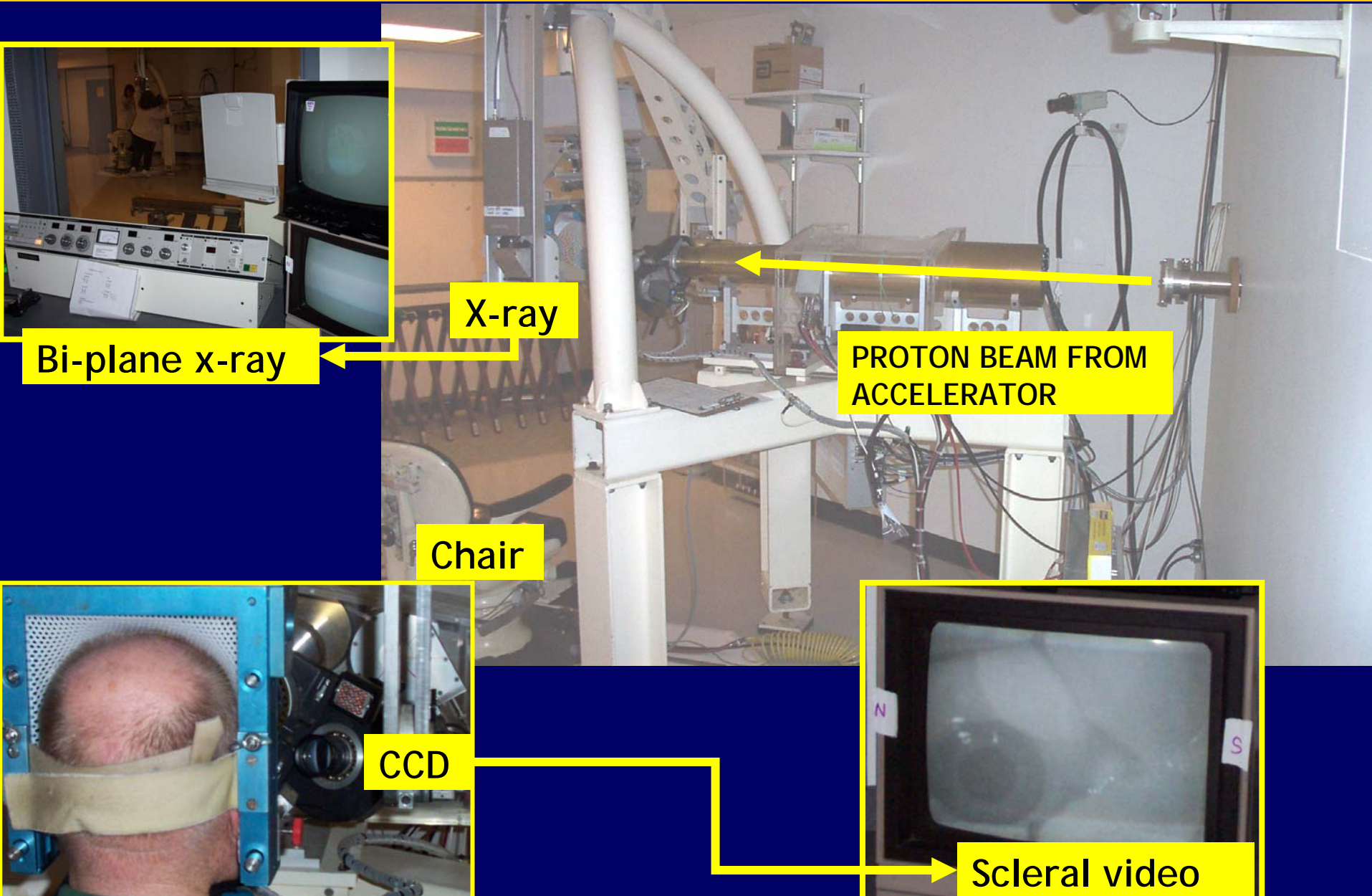


Requires 3-D radiation treatment plan to:

- Maximize tumor dosage
- Minimize non-tumor dosage
- Motion compensation
- Safety Shutoffs
- Spatial Dosimetry



Current Proton Beam Therapy



Bi-plane x-ray

X-ray

PROTON BEAM FROM ACCELERATOR

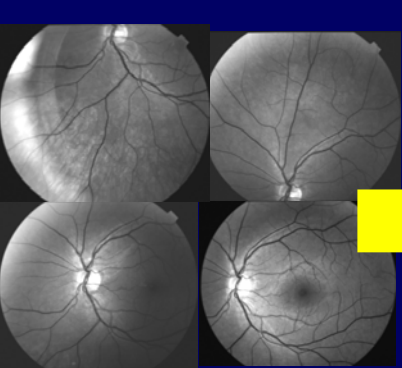
Chair

CCD

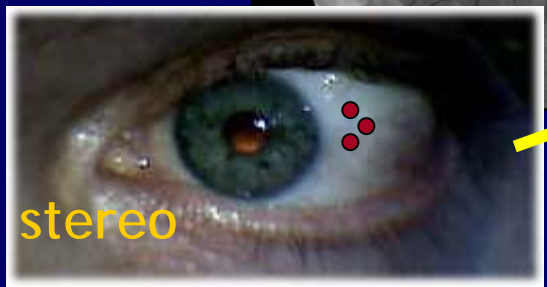
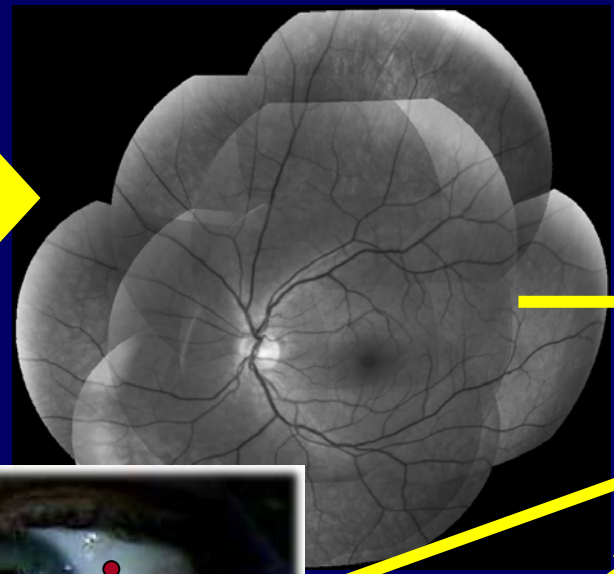
Scleral video



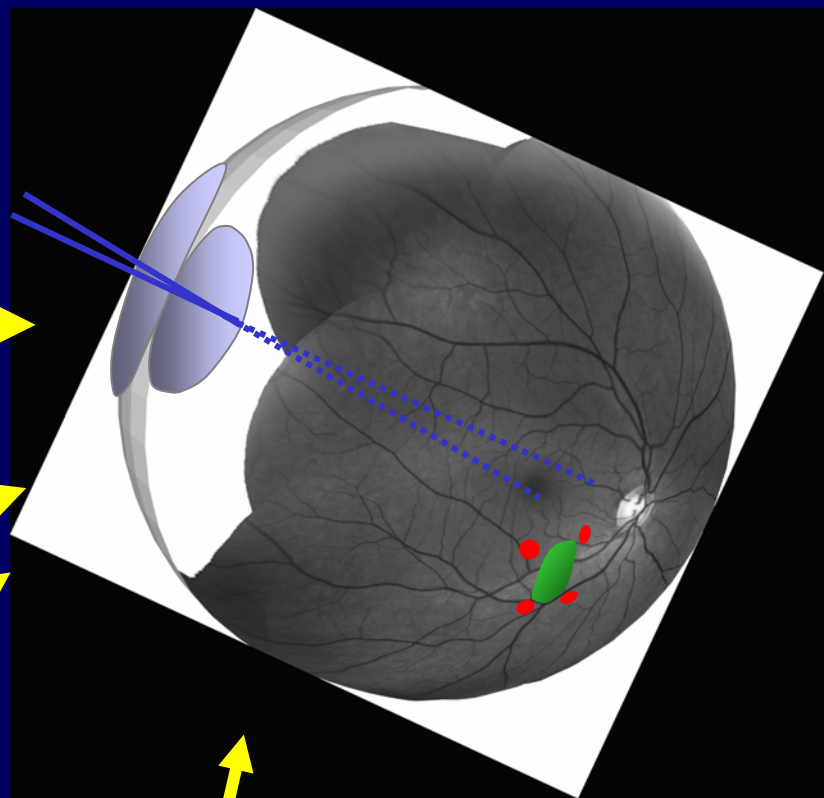
Generalized 3-D Ocular Atlas



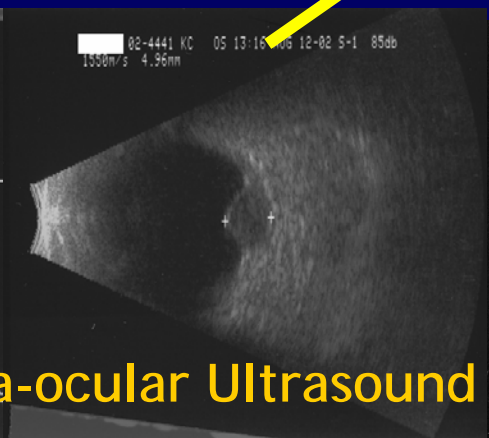
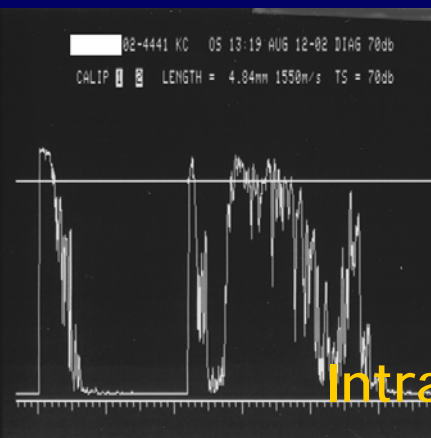
Retinal



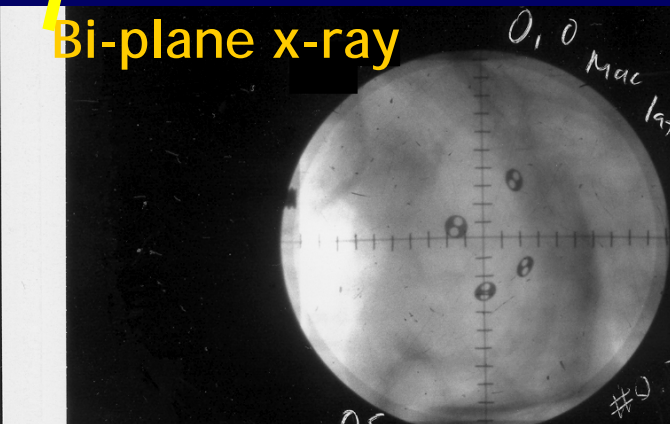
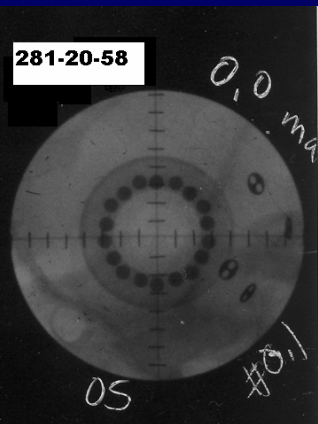
Scleral stereo



Bi-plane x-ray

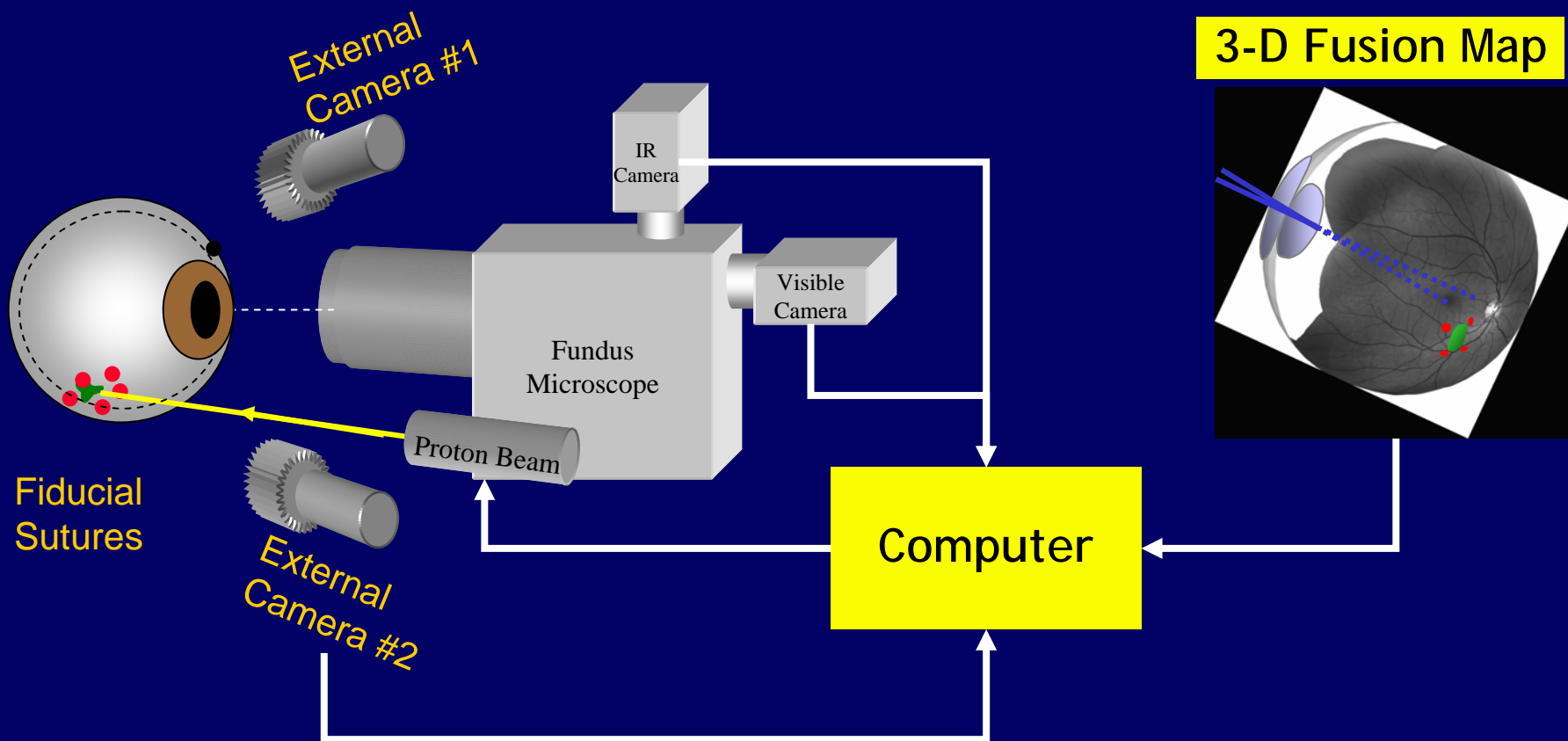


Intra-ocular Ultrasound



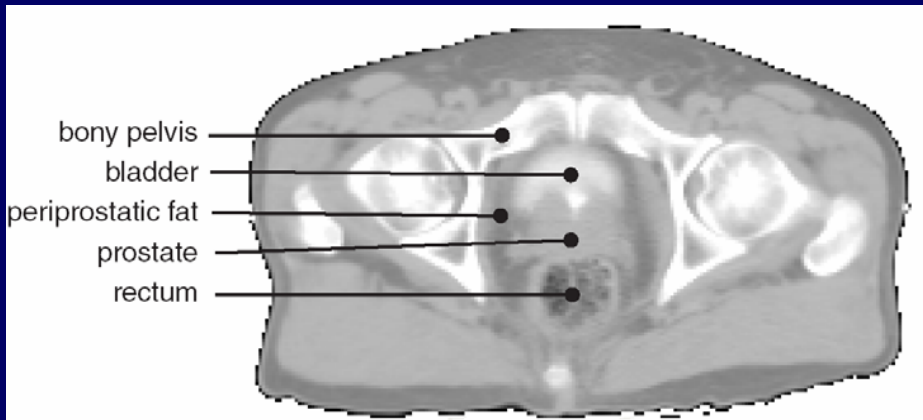


Future IGT System

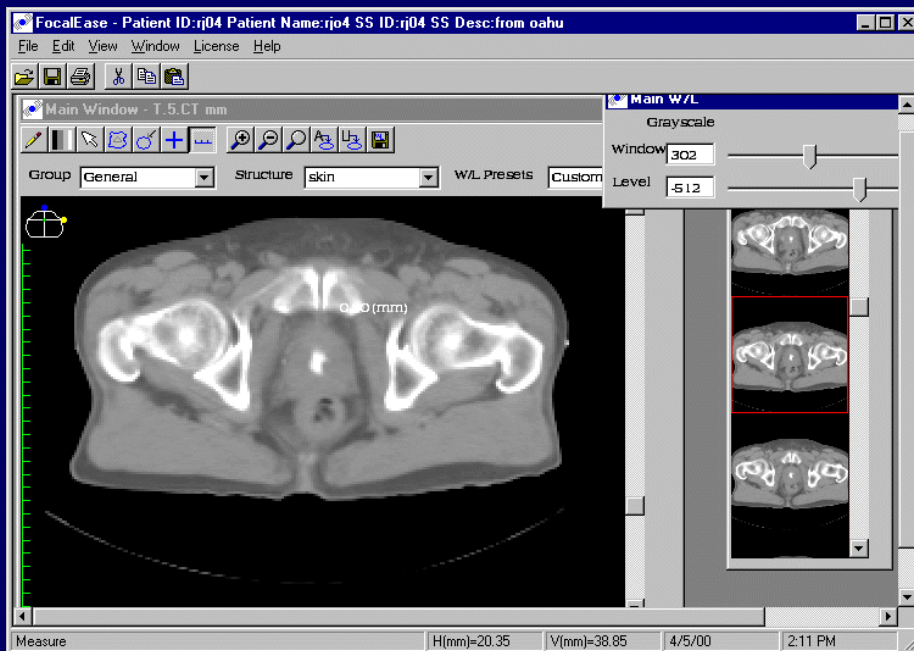




IGT for Deformable Structures



- **Examples:**
 - Prostate, lung
- **4D Systems needed**
 - Visualization
 - Segmentation
 - Planning Tools
 - Delivery Tools
- **Multiple motions and deformations**
 - Intra-fractional motion: (lung, abdomen)
 - Inter-fractional motion: (organ deformations & change)
 - Motion of beam delivery system

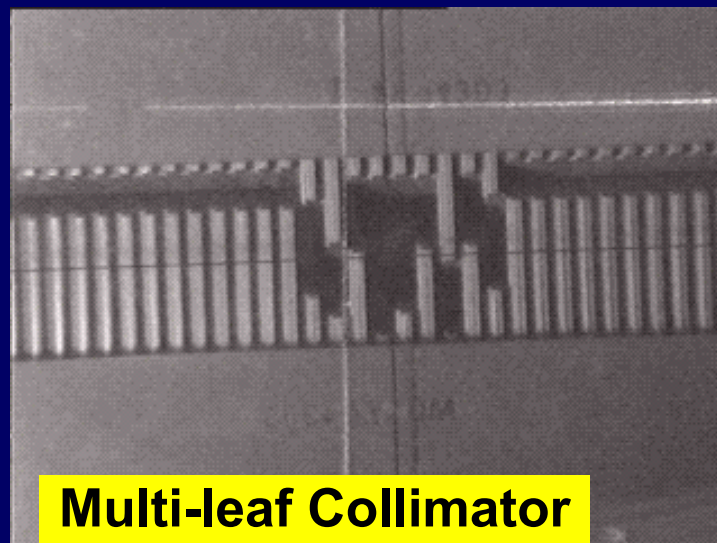




Current Method



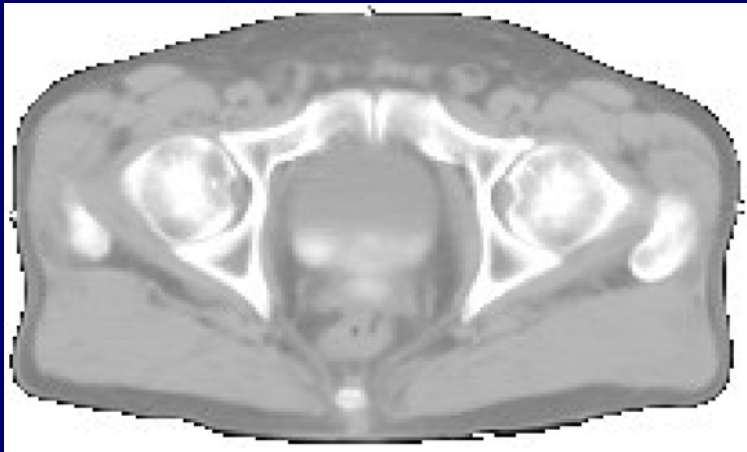
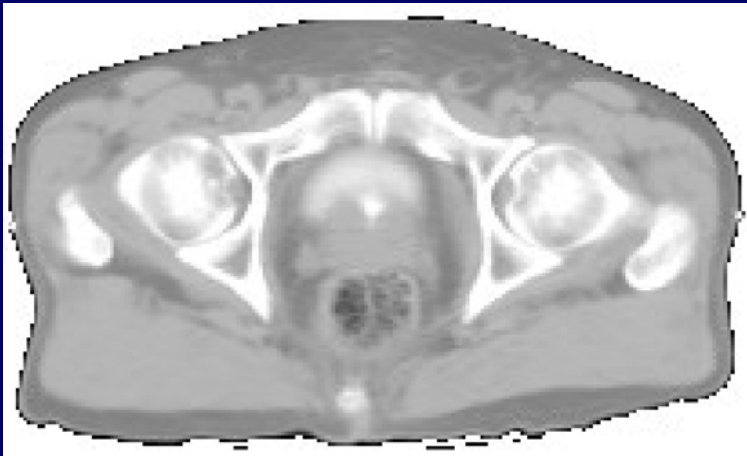
- Patient in restraint
- 3D CT “du jour” taken
- Patient-specific fractional dose calculations & adjustments
- Transfer patient to Linac for dose delivery
 - Conformal radio-therapy
 - Intensity-modulated radio-therapy



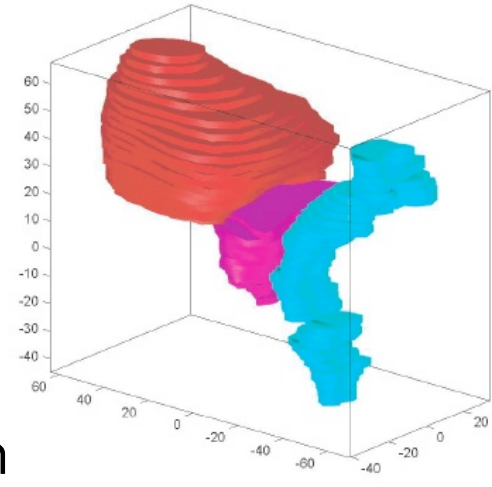
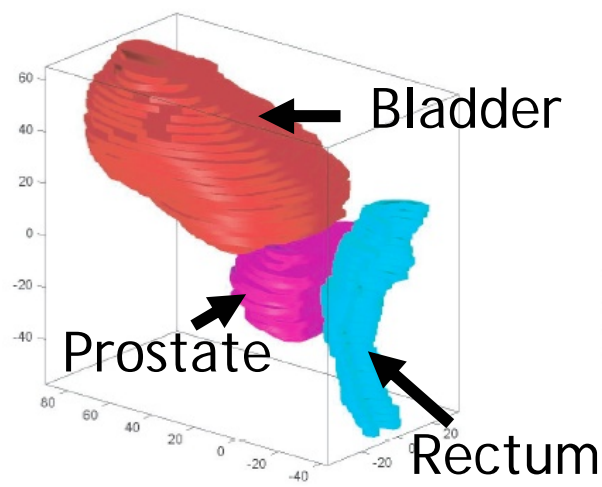
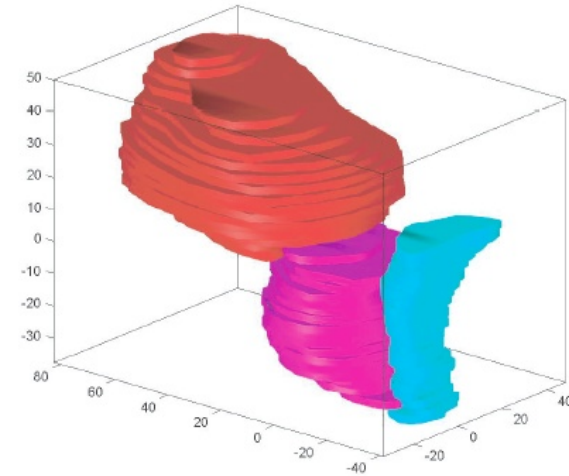
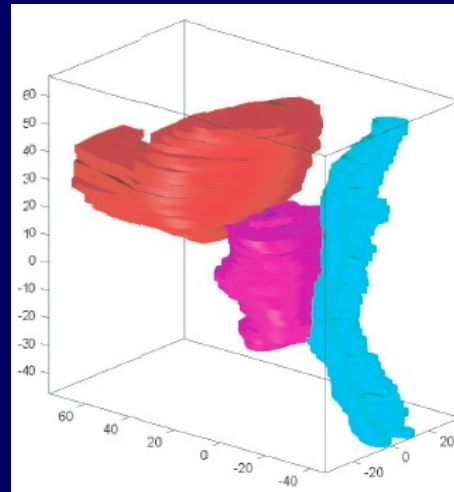
Multi-leaf Collimator



Challenges: Appearance & Shape Variability



Intra-patient variability,
10 days apart



Inter-patient variability

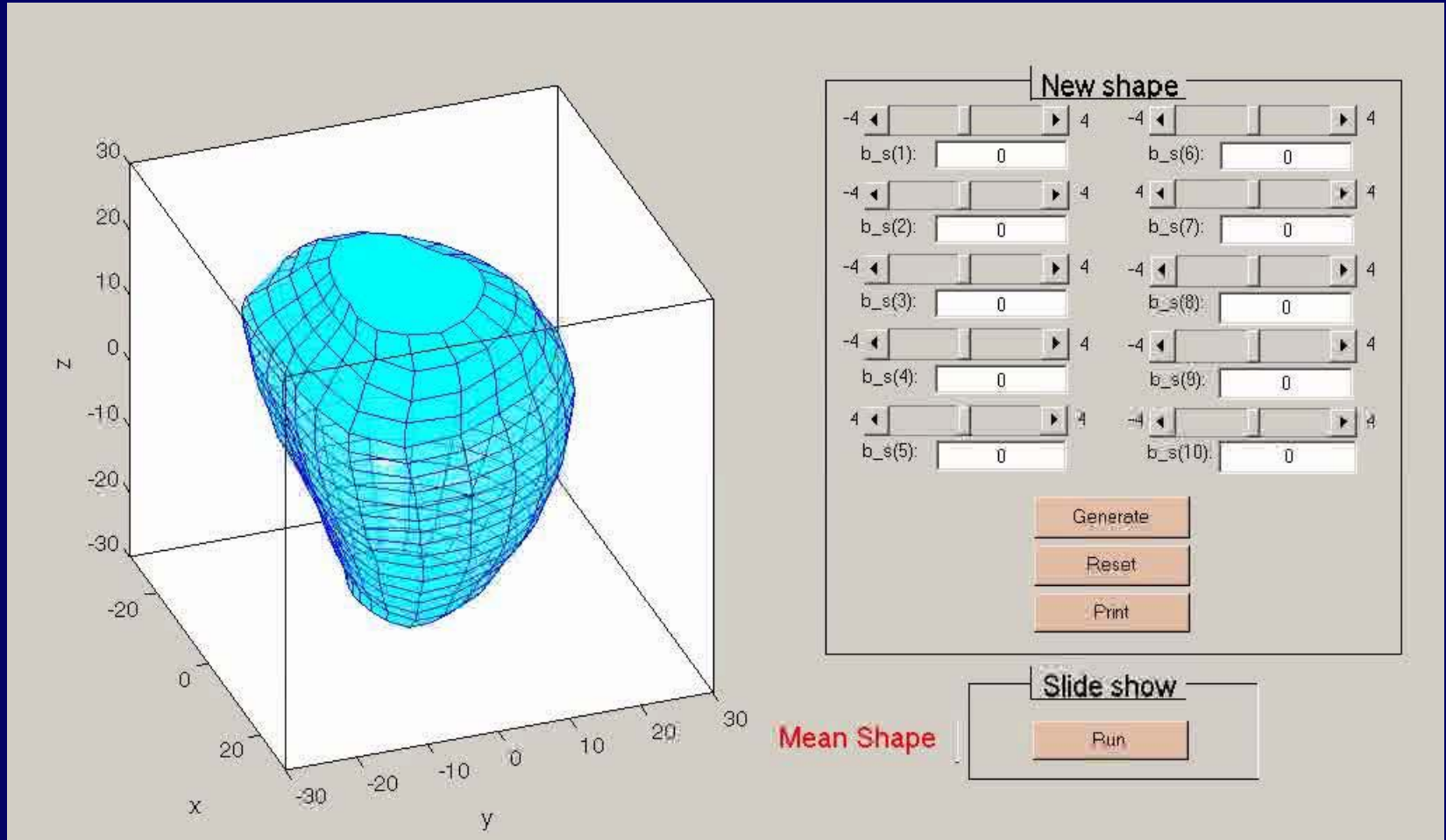


Engineering Implications

- Problem:
 - Given a new daily CT scan, just prior to a radiation fraction, segment the prostate, bladder, rectum, etc. for IGT and conformal avoidance
- Approach:
 - Construct effective low-dimensional models for intra- and inter-patient variability
 - Robust fitting of models to image data
 - Update the treatment plan
- Current Limitations:
 - Timeliness and verifiable accuracy of the model fitting
 - Expert manual segmentation takes 15-45 mins



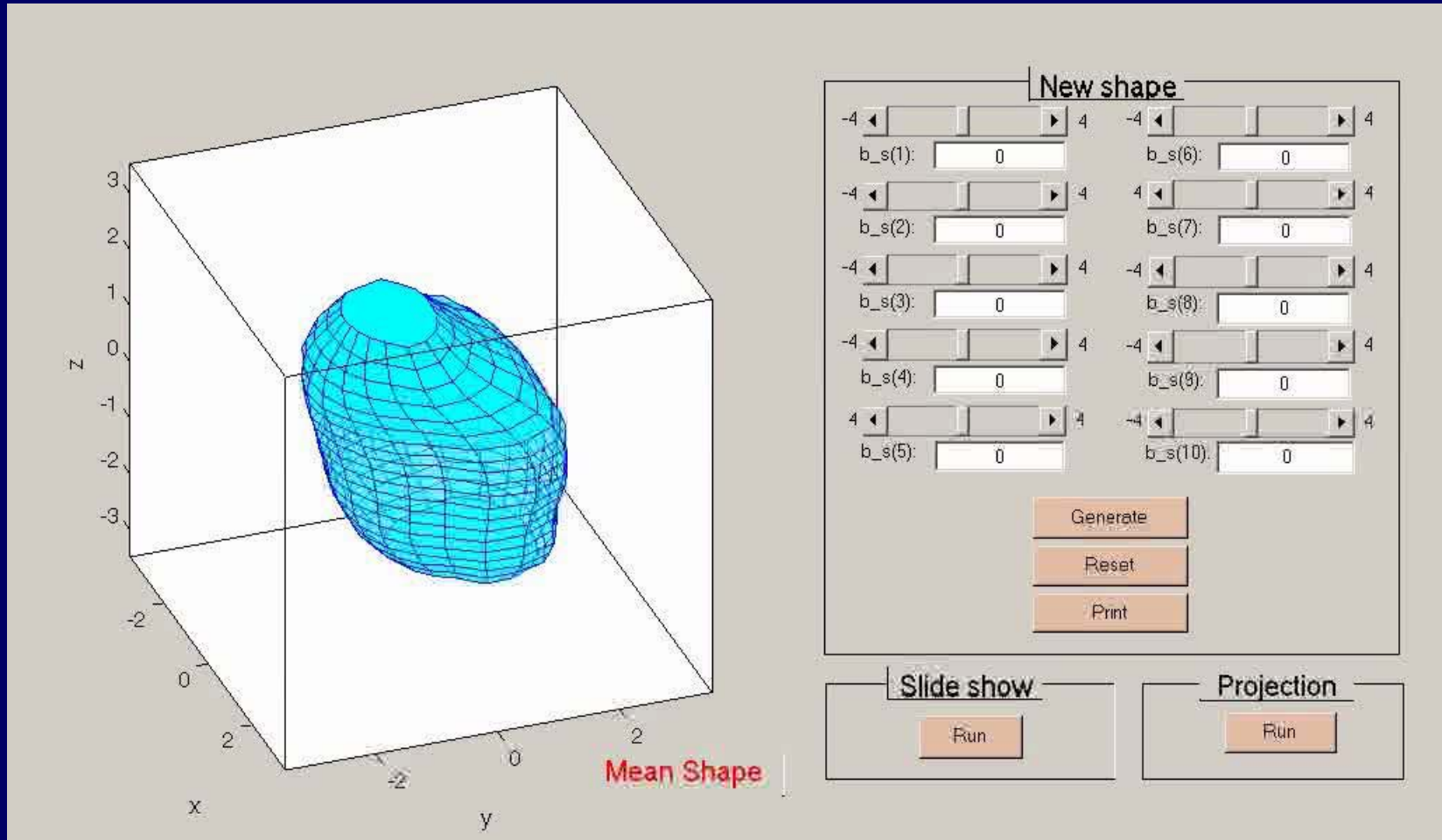
Inter-Patient Modes of Variation



Modes learned from MGH data (25 scans)



Intra-Patient Modes of Variation

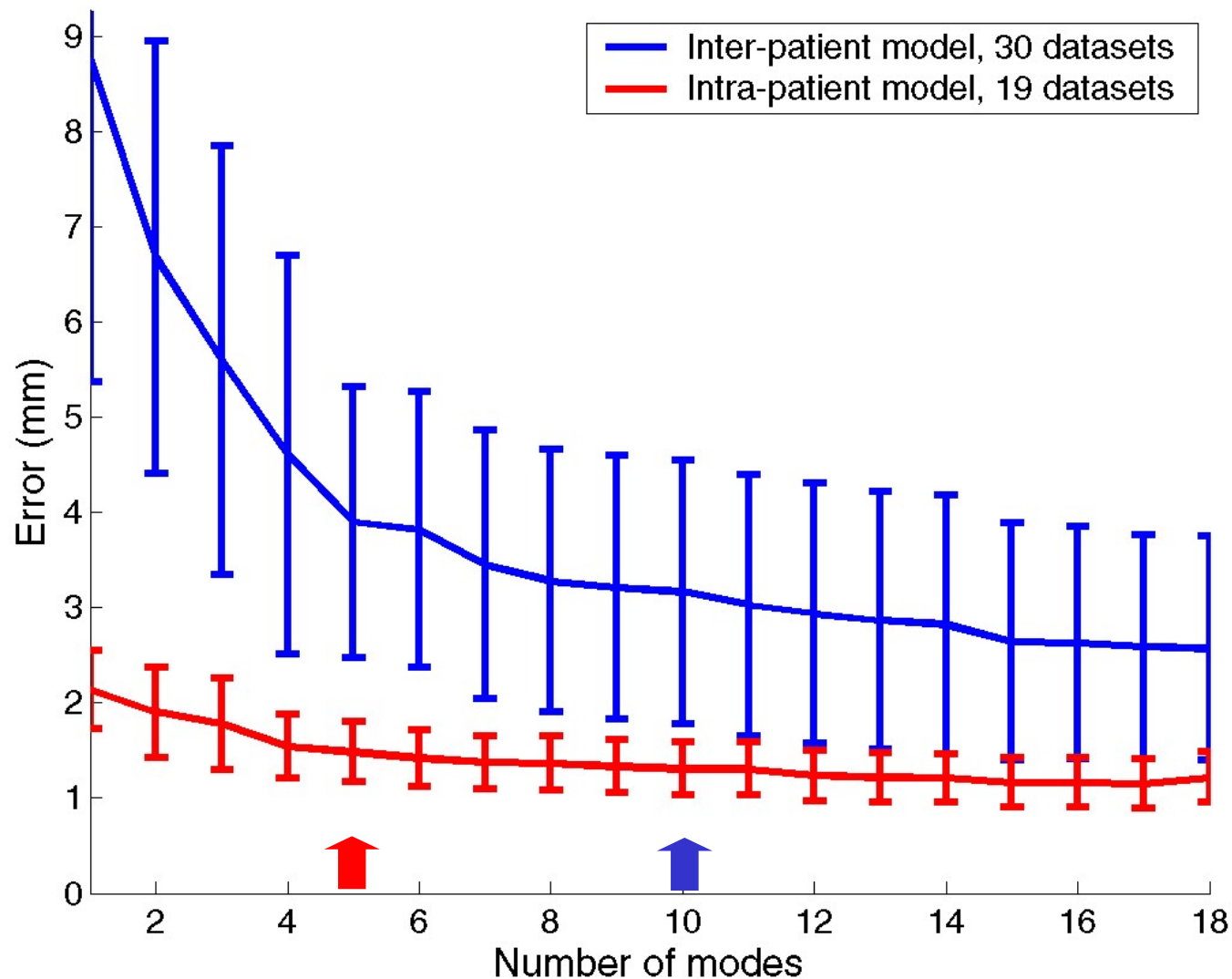


Modes learned from MSKCC data (19 scans)



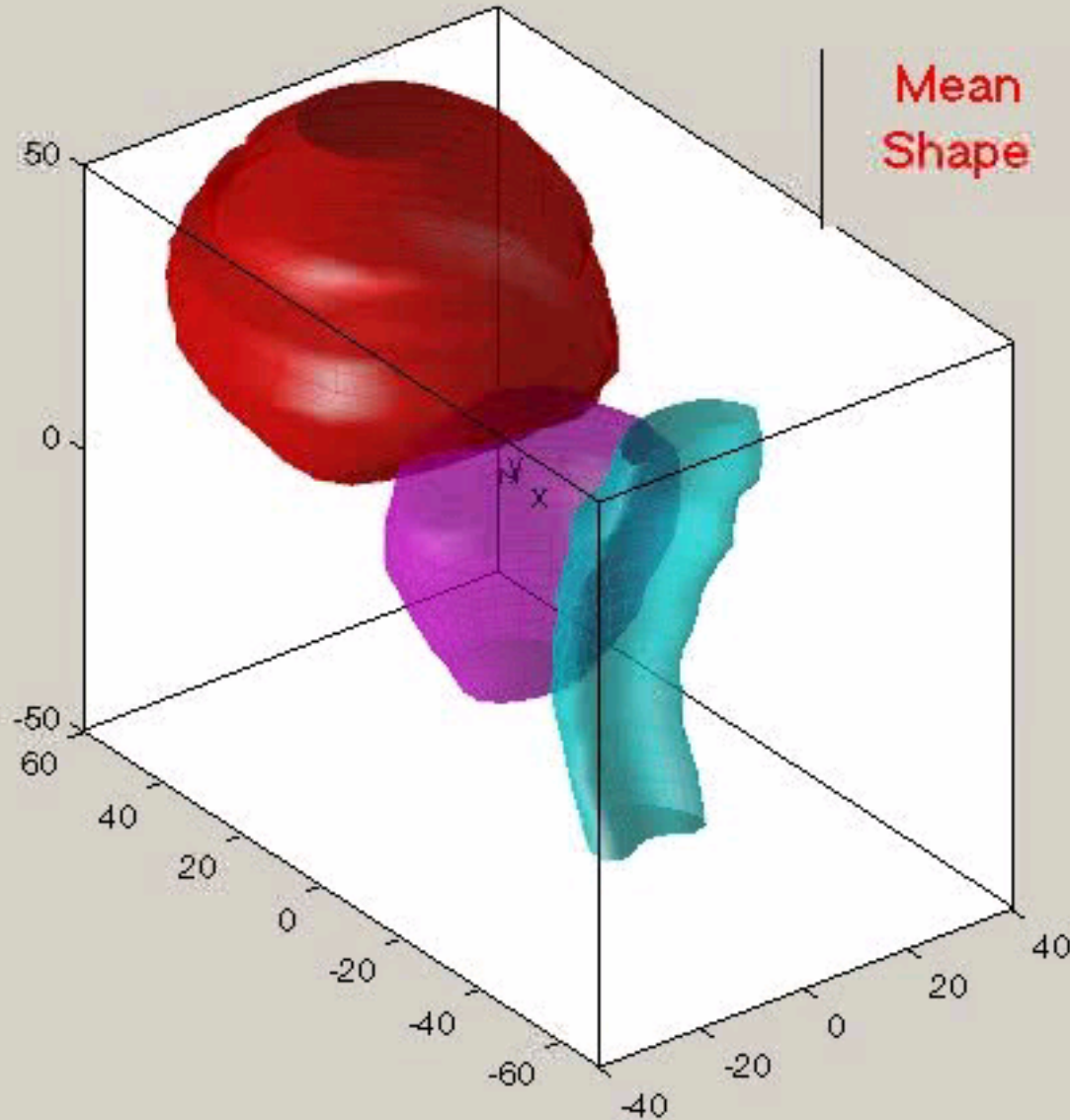
How Many Modes to Consider?

Mean fitting error vs. number of modes





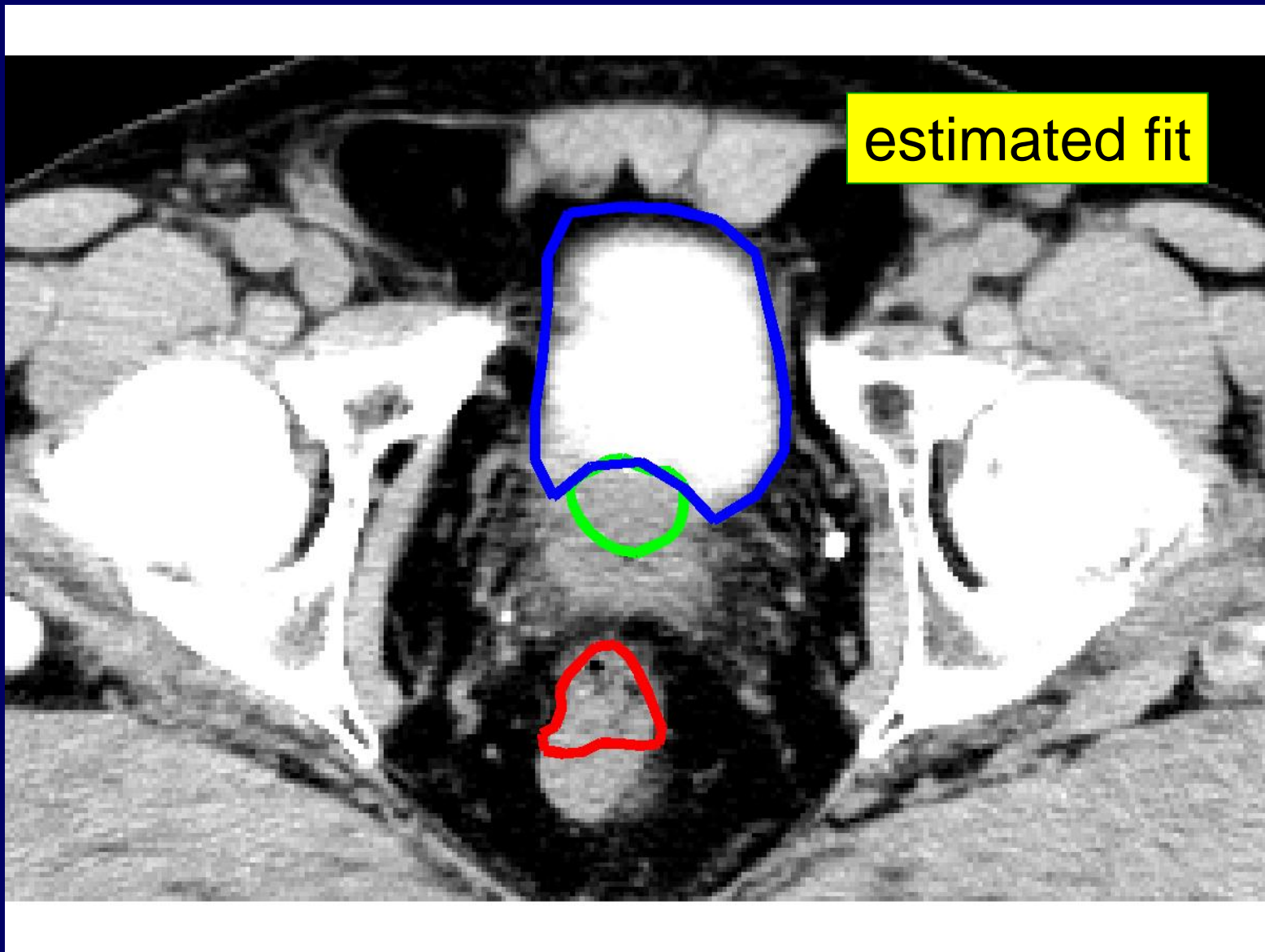
Joint Modeling of Variations



Joint shape model of prostate, bladder, and anterior rectal wall



Fitting the Model to a New Image

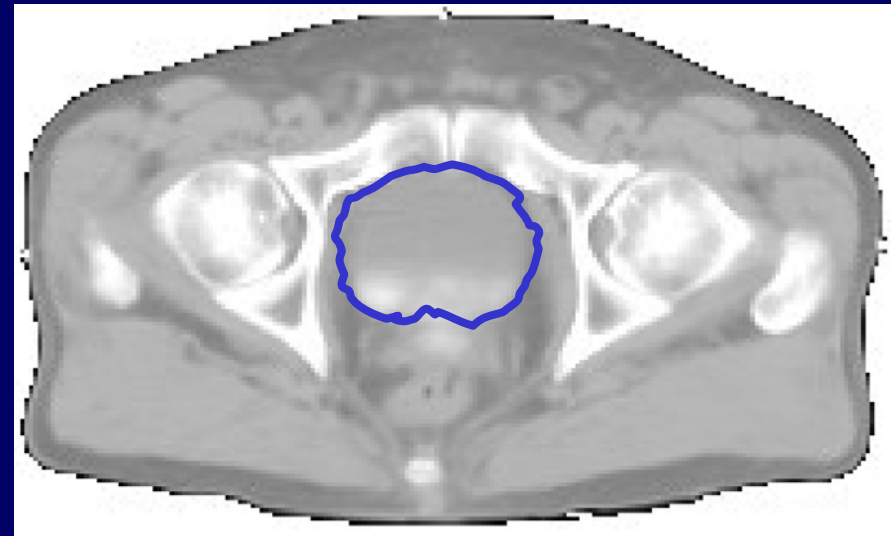
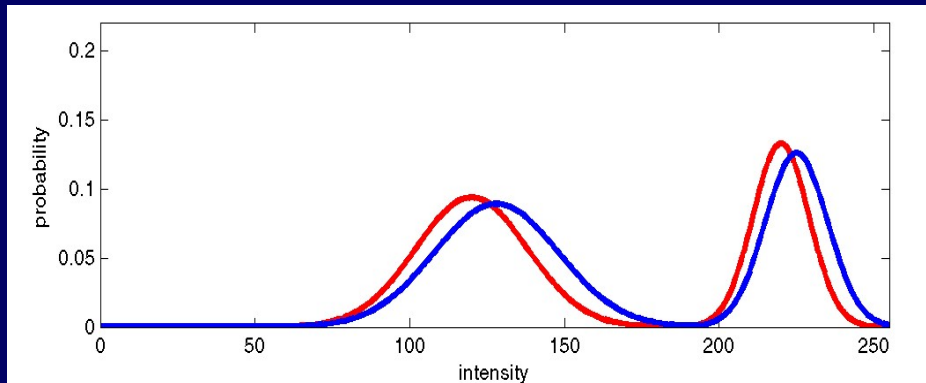


estimated fit



Density Matching Algorithm

Find the enclosing surface $\omega(b)$ whose sample density p is closest to the model density q , *subject to position and shape constraints imposed by the coupling.*



Kullback-Leibler
divergence

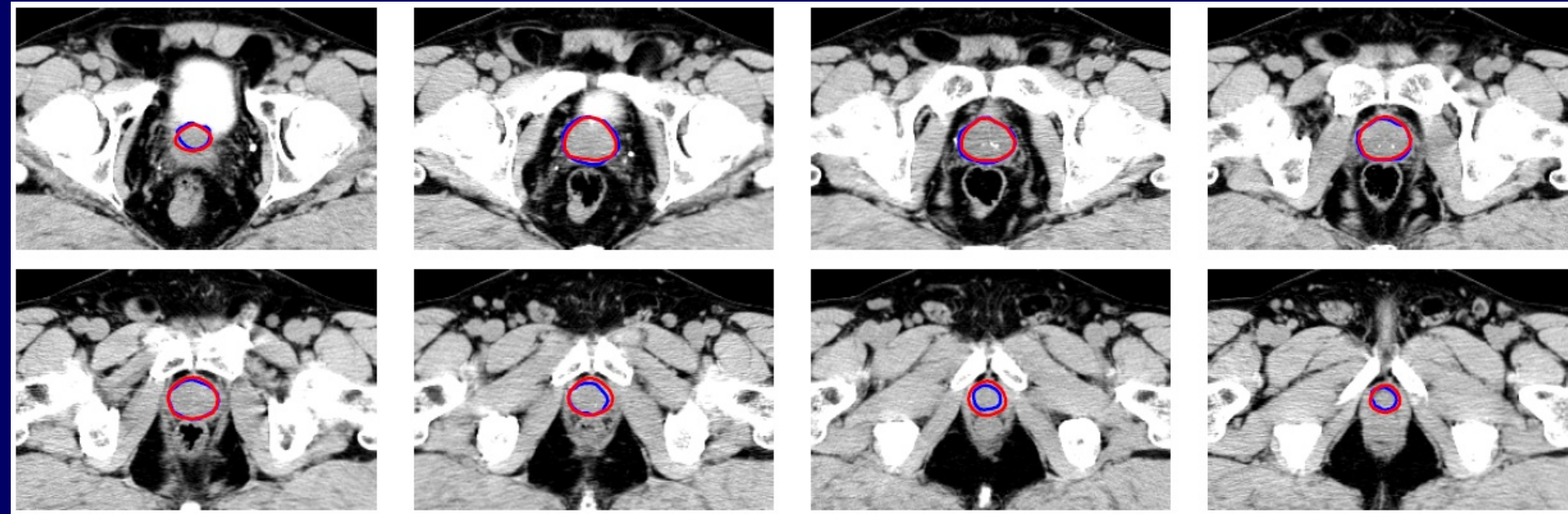
$$K(\omega(b)) = \int q(z) \log \left(\frac{q(z)}{p(z; \omega(b))} \right) dz$$

sample density

model density



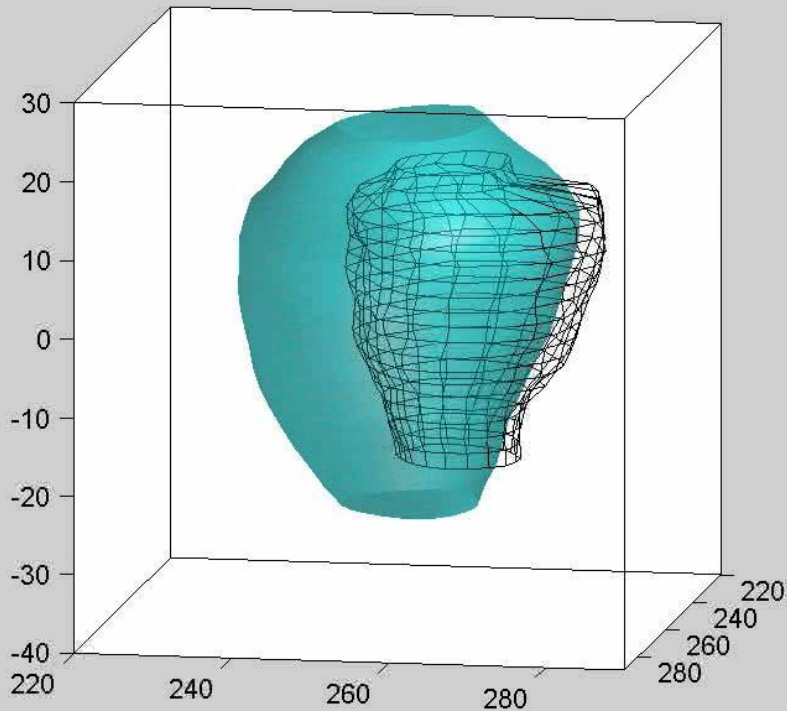
Prostate Model Fitting



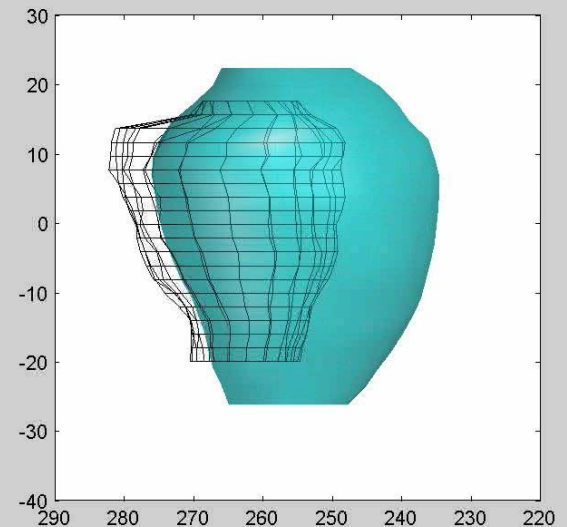
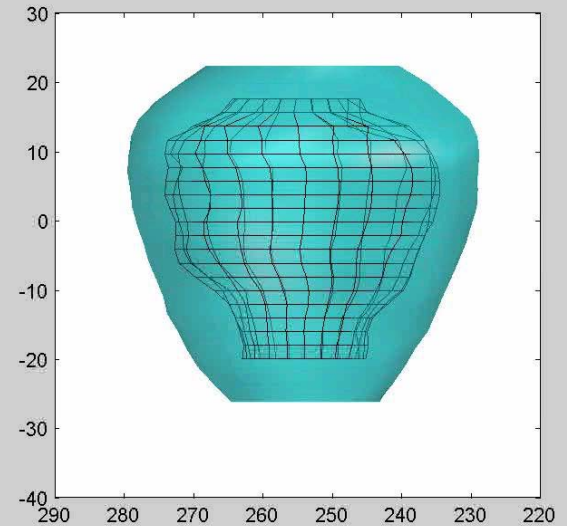
8 of 17 axial slices
Blue = Ground Truth
Red = Algorithm Result (55 sec)



Prostate Model Fitting

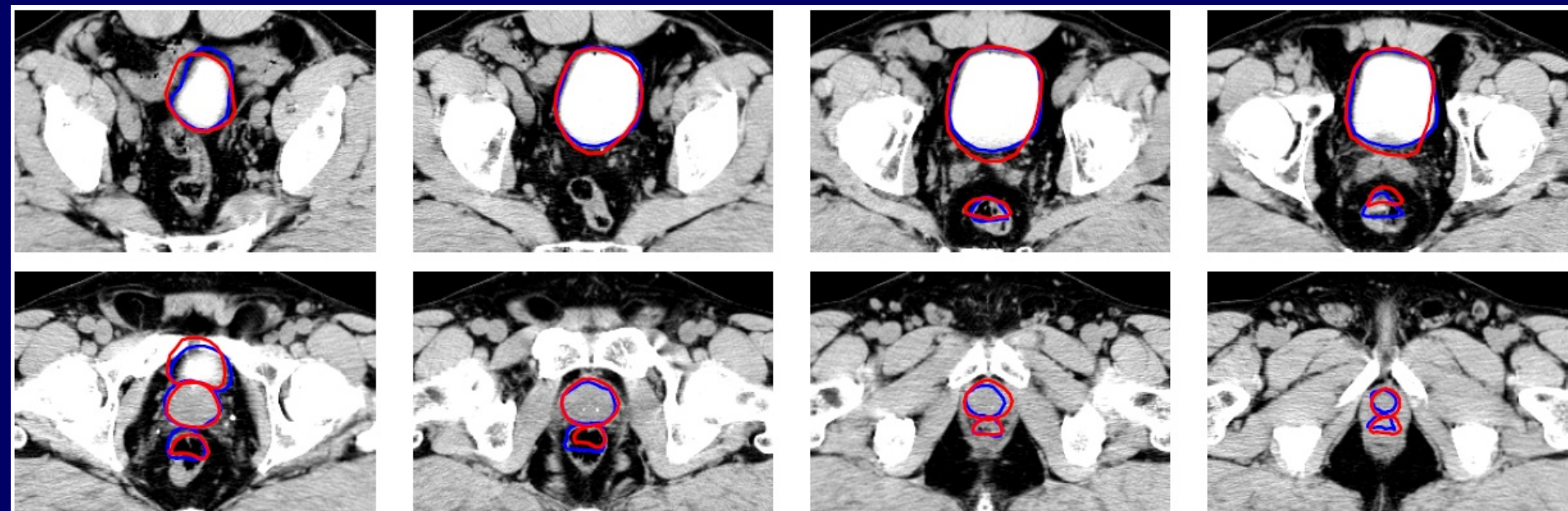


Volume error: $1.4e3 \text{ mm}^3$
Centroid error: 2.7 mm





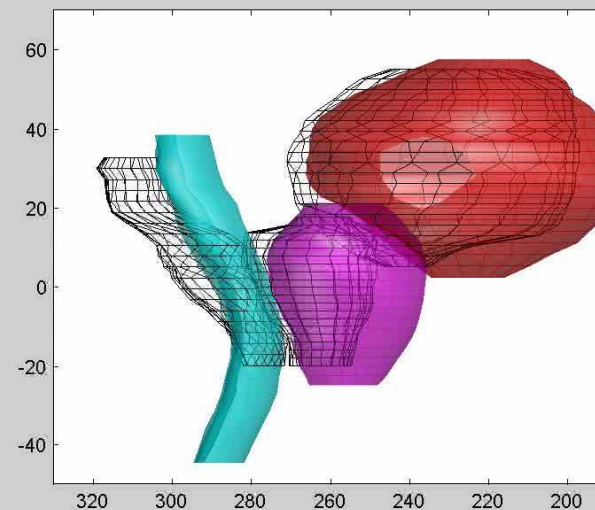
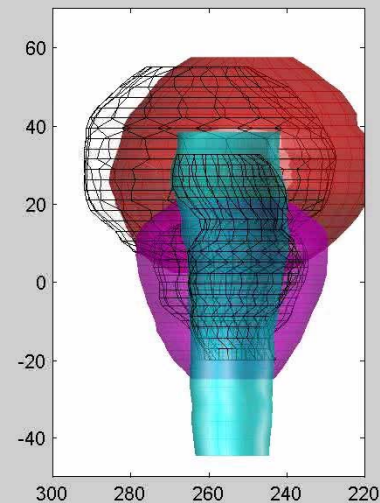
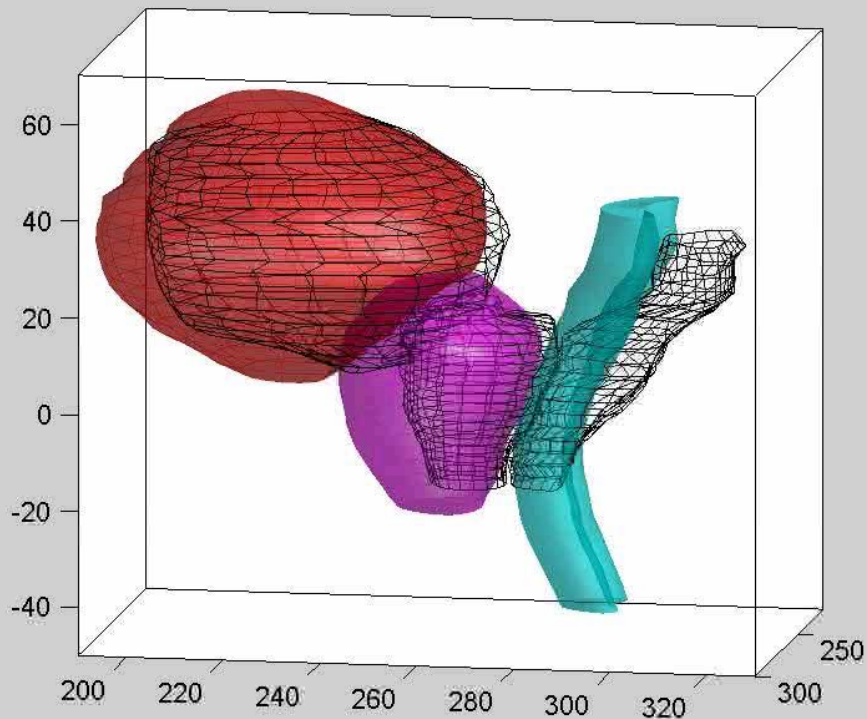
Joint Model Fitting



8 of 35 axial slices
Blue = Ground Truth
Red = Algorithm Result (307 sec)



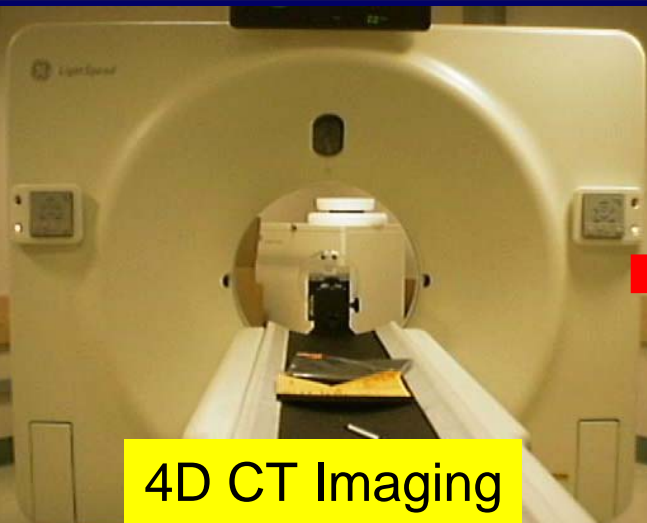
Joint Model Fitting



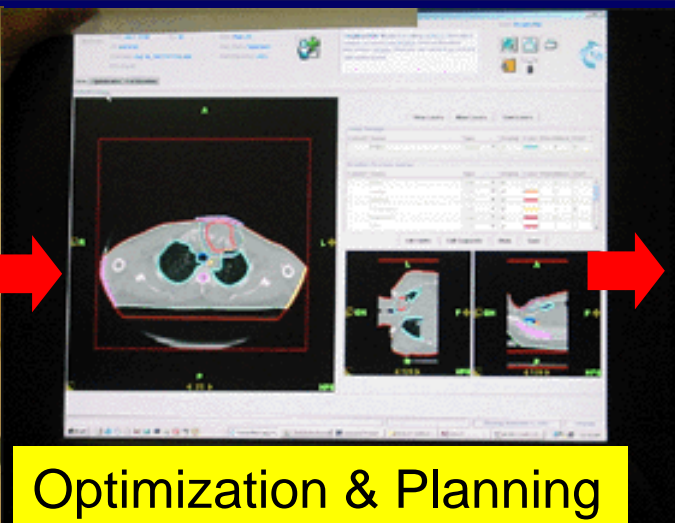
- Automatic fitting algorithm is 5 to 10X faster than manual contouring
- Accuracy comparable to manual segmentation
 - Can be edited as needed
 - Will enable accurate radiation delivery on day of treatment



Towards 4D Systems



4D CT Imaging



Optimization & Planning



IGT

GE MEDICAL SYSTEMS
 Lightspeed QX/i CT06_0C0
 Ex: 2563
 Ss: 100 PROC
 Im: 1+C
 SN
 DFOV 50.0cm

S 246

Massachusetts General Hospital

M
 anon2563
 Sep 23 2002
 01:46:59 PM
 512 X 512
 Mag = 1.00
 FL:
 ROT:

A



P

2
 5
 0



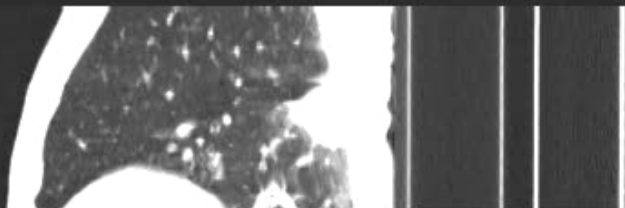
Lung Tumor Motion

GE MEDICAL SYSTEMS
LightSpeed QXi CT06_OC0
Ex: 2563
Se: 100 PROC
Im: 1+C
SN
DFOV 50.0cm

S 246

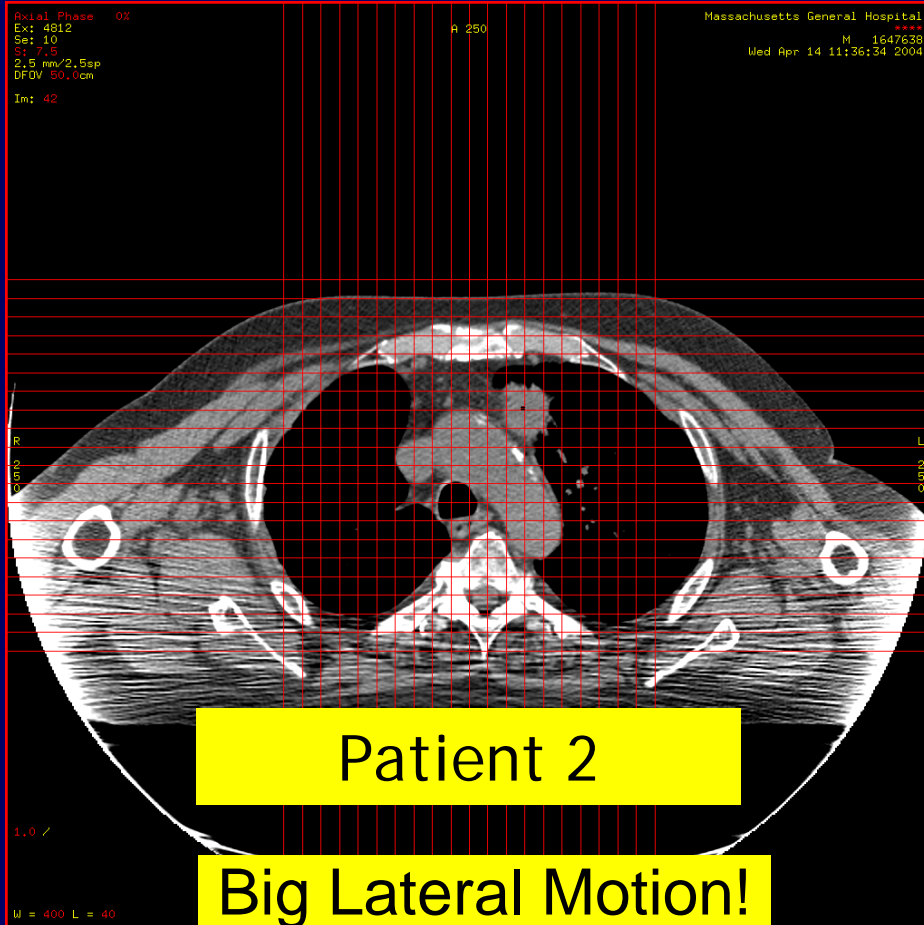
Massachusetts General Hospital

M
anon2563
Sep 25 2002
01:46:59 PM
512 X 512
Mag = 1.00
FL:
ROT:



Patient 1

Peak to Peak 1.3 cm



Patient 2

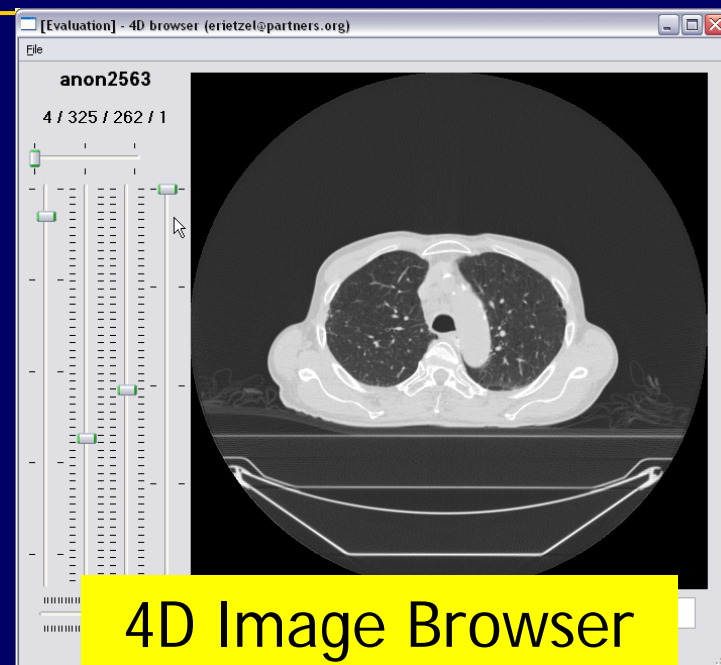
Big Lateral Motion!

Caveat: Single cycle looped!



Challenges and Opportunities from 4D

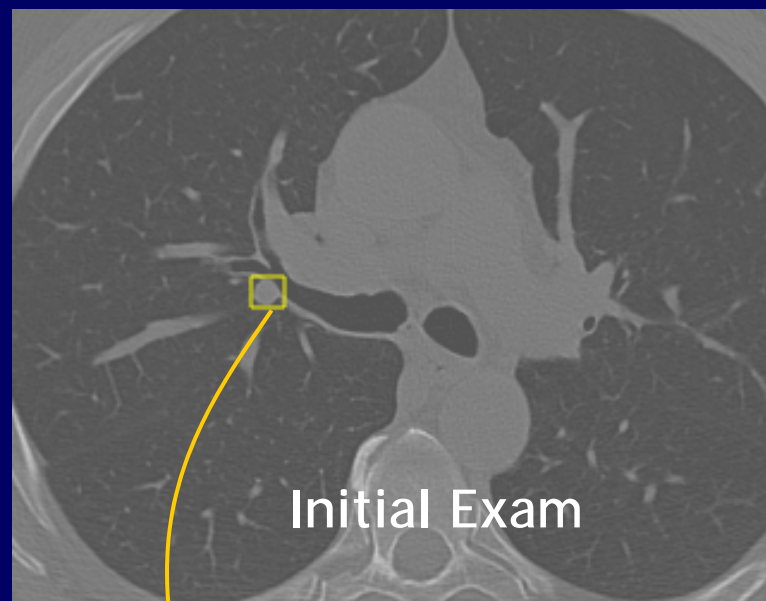
- **Artifact-free 4D Imaging**
 - Need for motion-compensated reconstruction
- **Effective visualization tools needed**
- **Effective and **timely** segmentation**
 - Variability
 - Low contrast, poor edges
 - Massive data volume!
 - Verification/visualization tools
- **4D Dose calculation tools**
- **4D Dose delivery systems**
- **Deformable registration with change intelligence**





Improving Deformable Registration

- **Temporal Registration of CT Lung Volumes for Improved Radiation Treatment**
- **Sub-millimeter accuracy desired notwithstanding lung deformations**
- **New B-spline registration algorithm: uncertainty driven hybrid of intensity-based and feature-based techniques**
- **Preliminary tests:**
 - **B-spline deformation model: 1.5mm accuracy**
 - **Current State of the Art 11.7mm accuracy**





Summary

- **Image-guided intervention is a powerful multi-disciplinary technology driver**
 - **Several disciplines**
 - Computer vision
 - Imaging
 - Systems
 - Imaging Systems
 - Chemistry and Physics
 - High-speed Computing
 - **Common, pervasive themes across applications**
 - Need to enhance cross-disciplinary collaboration
 - Need to achieve greater efficiency in building new systems
 - Toolboxes, Frameworks, Taxonomy,...
 - **Could be applied to several other areas:**
 - Cell and tissue level work
 - Biotechnology automation
 - Environmental remediation



Thank you & keep in touch!



Badri Roysam

**Professor of Electrical, Computer, & Systems
Engineering**

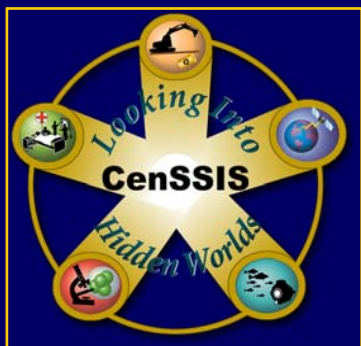
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