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**MAGNETIC RESONANCE SPECTROSCOPY FOR BRAIN TUMORS**

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## TABLE OF CONTENTS

Section	Page
Table of Contents	2
Abstract	3
Introduction	8
Methods	22
Results: full published studies	28
Results: proceedings abstracts	63
Summary	76
Conclusion	83
Appendix A: Analytic Framework	84
Appendix B: Glossary	86
Evidence Table 1: Technical Feasibility Published Study Abstracts	87
Evidence Table 2: Technical Feasibility Proceedings Abstracts	89
Full Study and In-text References	90
Proceedings Abstract References	103

40

41 **Abstract**

42 **Magnetic Resonance Spectroscopy For Brain Tumors**

43 **Introduction**

44 Diagnosing and treating space-occupying tumors of the brain

45 presents special challenges due to the similarities of tumors to other  
46 pathologic entities on conventional imaging, the similarities of individual  
47 tumor cell types on conventional imaging, the inaccessibility of these  
48 lesions, and their proximity to complex brain structures. A non-invasive  
49 technique that could provide information about the chemical and histologic  
50 composition of brain tissue could greatly aid diagnosis and treatment of  
51 brain tumors by helping to avoid unnecessary biopsies, by helping to guide  
52 biopsies, and by providing additional information for improving treatment.  
53 The Centers for Medicare & Medicaid Services (CMS) requested a  
54 technology assessment by the Agency for Healthcare Research and  
55 Quality (AHRQ) to assess the value of Magnetic Resonance Spectroscopy  
56 (MRS) for diagnostic evaluation, surgical planning, and patient  
57 management of space-occupying brain tumors. The Tufts-New England  
58 Medical Center Evidence-based Practice Center was asked to conduct an  
59 assessment of this technology.  
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64 **Methods**

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66 An OVID search of the MEDLINE<sup>®</sup> database was conducted on  
67 November 6, 2002. Filters and limitations were used to eliminate  
68 inappropriate publications, with inclusion and exclusion criteria developed  
69 to identify articles to be reviewed. The search used applicable MeSH  
70 headings and textwords with appropriate Boolean operators. After filtering  
71 irrelevant publication types (such as publications not containing original  
72 clinical data), the search resulted in 959 citations for download and  
73 screening. Hand screening of the abstracts resulted in accepting 137  
74 citations for complete article retrieval. All abstracts were reviewed to  
75 identify full articles that met the criteria. In addition, abstracts from the  
76 following relevant professional society proceedings for the years 2001 and  
77 2002 were reviewed and included in the analyses: American Society of  
78 Neuroradiology (ASNR), Radiological Society of North America (RSNA),  
79 and the International Society for Magnetic Resonance in Medicine  
80 (ISMRM).

81

82 **Results**

83

84 Ninety-six articles met our inclusion criteria for evaluation, and 85 of  
85 these only provided information about technical feasibility. Eleven of the

86 articles provided information beyond the level of technical feasibility. Eight  
87 articles evaluated the test performance of MRS in various settings. Three  
88 articles addressed the impact of MRS on diagnostic thinking and  
89 therapeutic decision making. No article was found that addressed  
90 improvement of patient outcome.

91           Cho/Cr (choline/creatine) is the only metabolite ratio that has been  
92 found to be useful in differentiating neoplasm and non-neoplasm and  
93 supported by several studies. Among all the full articles examined in this  
94 technology assessment only one provided the most complete reporting of  
95 the metabolite signal intensities and ratios for each type of tumor found in  
96 their study population. However, no single metabolite or ratio, other than  
97 perhaps a very high Cho/Cr ratio to diagnose peripheral neuroectodermal  
98 tumors (PNET), by itself could differentiate among different neoplasms,  
99 among different tumor grades, or between neoplastic and non-neoplastic  
100 lesions.

101           The only study that addressed the incremental gain in the proportion  
102 of diagnostic tissue obtained demonstrated that MRS added to  
103 conventional MRI improved the number of correct diagnoses and reduced  
104 the number of incorrect or equivocal diagnoses.

105

106 Three studies addressed the potential impact of MRS results on  
107 diagnostic thinking or therapeutic decision making. Conclusions that can be  
108 drawn from these studies are severely limited due to the fact that the two  
109 prospective studies had only 15 and 17 patients, respectively, and the only  
110 large study was a retrospective analysis of medical records to identify  
111 potential opportunities of MRS to influence diagnostic thinking. No study  
112 explicitly evaluated the impact of voxel position on the accuracy of MRS.  
113 No study commented on the potential impact of operator error in placement  
114 of the voxel.

## 115 **Conclusion**

116  
117 Human studies conducted on the use of MRS for brain tumors  
118 demonstrate that this non-invasive method is technically feasible and  
119 suggest potential benefits for some of the proposed indications. However,  
120 there is a paucity of high quality direct evidence demonstrating the impact  
121 on diagnostic thinking and therapeutic decision making. In addition, the  
122 techniques of acquiring the MRS spectra and interpreting the results are  
123 not well standardized. In summary, while there are a large number of  
124 studies that confirm MRS' technical feasibility, there are very few published  
125 studies to evaluate its diagnostic accuracy and whether it can positively  
126 affect diagnostic thinking and therapeutic choice. Those studies that do

127 address these areas often have significant design flaws including  
128 inadequate sample size, retrospective design and other limitations that  
129 could bias the results.

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# 1. INTRODUCTION

## 1.1 Background

Diagnosing and treating space-occupying tumors of the brain presents special challenges due to the similarities of tumors to other pathologic entities on conventional imaging, the similarities of individual tumor cell types on conventional imaging, the inaccessibility of these lesions and their proximity to complex brain structures. Standard imaging diagnostic procedures include computerized tomography (CT), magnetic resonance imaging (MRI), single photon emission computed tomography (SPECT), and positron emission tomography (PET) imaging. Following is a summary of invasive and non-invasive means of diagnosing brain tumors:

Tech-nique	Degree of Invasiveness	Description
Biopsy	Invasive	Extraction of tissue for histopathological diagnosis. The reference standard.
CT	Noninvasive Uses ionizing radiation	Computed 2-dimensional map of the attenuation voxels of tissue using externally generated x-rays delivered in a circular fashion.
MRI	Noninvasive No ionizing radiation	Spatial localization of tissue properties that relate to alignment of protons in strong magnetic fields.
SPECT	Noninvasive Uses radio-isotopes	Spatially localizes emitted photons (gamma rays) after administration of radioactive agent.
PET	Noninvasive Uses radio-	Spatially localizes emitted positrons after administration of radioactive agent.



Technique	Degree of Invasiveness	Description
	isotopes	
MRS	Noninvasive No ionizing radiation	Spatial localization of tissue chemical properties that relate to alignment of protons in strong magnetic fields. Proton (hydrogen) MRS uses the frequency response of hydrogen, while other versions examine the frequency response of other elements (phosphorus and sodium).

143

144           Confirming the preliminary diagnosis requires tissue biopsy to assess  
145 the histologic composition of the brain tissue in question. A non-invasive  
146 technique that could provide information about the chemical and histologic  
147 composition of brain tissue could greatly aid diagnosis and treatment of  
148 brain tumors by helping to avoid unnecessary biopsies, by helping to guide  
149 biopsies, and by providing additional information for improving treatment.

150           Magnetic Resonance Spectroscopy is a technique related to  
151 magnetic resonance imaging (MRI). Both techniques rely on the tendencies  
152 of some proportion of protons to align with or against a strong magnetic  
153 field. MRI refers to localizing the total tissue signal produced by a small,  
154 localized collection of tissue (voxel). The tissue signal is produced by the  
155 rates of magnetic alignment (or decay) of the protons in two planes as well  
156 as the overall proton density. T1 relaxation refers to alignment with the  
157 magnetic field, and T2 relaxation refers to alignment perpendicular to the

158 magnetic field). This phenomenon is produced by stimulating the blocks of  
159 tissue with a broad-spectrum signal that disrupts the magnetic alignment.  
160 The signal is eventually produced, after electromagnetic manipulation, as  
161 the protons re-align themselves to their original configurations.

162 MRS, on the other hand, relies on a very different phenomenon of  
163 proton alignment with the magnet that is based on frequency. The ability of  
164 the alignment of protons to be disrupted is frequency dependent. The  
165 exact frequency that disrupts the alignment depends on the chemical  
166 structures containing the protons. In MRS, tissue blocks (or voxels) are  
167 stimulated with very narrow bandwidth frequencies, and a graph is made of  
168 the signal strength vs. the frequency of stimulation. This produces  
169 characteristic peaks related to the amount of certain chemical compounds  
170 present in the tissue. MRS, therefore, has the potential to provide  
171 information about specific metabolites in brain tissue that can indicate the  
172 presence of tumor, necrotic tissue, and other pathologic entities. It should  
173 be noted that MRS has been evaluated as a diagnostic tool for a variety of  
174 diagnostic applications including not only CNS tumors but other non-CNS  
175 conditions. In this report, we exclusively examine MRS for brain tumors.

176 Finally, the majority of brain tumor studies focus on proton (hydrogen)  
177 MRS, but other elements (i.e. phosphorus and sodium) are used. This

178 report deals with proton hydrogen MRS (to be referred herein simply as  
179 “MRS”).

180

## 181 **1.2 Requests by the Centers for Medicare and Medicaid Services**

182 The Centers for Medicare & Medicaid Services (CMS) requested a  
183 technology assessment by the Agency for Healthcare Research and  
184 Quality (AHRQ) to assess the value of MRS for diagnostic evaluation,  
185 surgical planning, and patient management of space-occupying brain  
186 tumors. Also requested was a review of factors that may affect the  
187 performance of MRS. The Tufts-New England Medical Center Evidence-  
188 based Practice Center was asked to conduct an assessment of this  
189 technology. For patients presenting with signs or symptoms of a space-  
190 occupying brain lesion, the key questions to be addressed were:

- 191 1. For what metabolic profiles does the yield of MRS provide  
192 equivalent, complementary, or more accurate diagnostic information  
193 for (i) initial diagnosis, (ii) recurrence, or (iii) assessing therapy than
  - 194 • Brain biopsy
  - 195 • Conventional anatomic imaging studies
  - 196 • MRS + conventional anatomic imaging studies vs. brain biopsy
- 197 2. Does the use of MRS lead to an improved net health outcome by

- 198           • Avoiding unnecessary biopsy
- 199           • Obtaining appropriate biopsy, from appropriate location
- 200           • Directing biopsy to an appropriate location
- 201           • Receiving appropriate treatment
- 202           • Avoiding an inappropriate treatment

203           3. Are voxel positions and operator error important factors in  
204           obtaining diagnostic images? If so, how do they impact MRS  
205           accuracy?

206

### 207           **1.3 Analytic Framework**

208           To address these issues we developed an analytic framework  
209           describing each of the potential uses of MRS. Potential uses of MRS are  
210           described for patients newly diagnosed with a space-occupying brain mass  
211           as well as for patients with a previously diagnosed brain tumor undergoing  
212           treatment. The potential uses include diagnostic evaluation and  
213           prognostication, patient management and planning for surgery, and  
214           potential outcome measures for evaluating performance. Factors that might  
215           affect performance are also included in the framework, which is presented  
216           in Appendix A.

217

218           **1.3.1 Diagnostic evaluation**

219           Experimentation with in-situ Magnetic Resonance Spectroscopy  
220 (MRS) for tumor assessment has been ongoing since 1985 (Maris et al.,  
221 1985). It was initially hoped that MRS would provide definitive  
222 spectrographic signatures of tumor histologic types. Clinical MRS research  
223 has led to multiple specific applications of MRS for both diagnostic work-  
224 ups and treatment follow-up of CNS tumor. Combined with findings from  
225 conventional anatomic MRI, MRS may have the potential to improve the  
226 diagnosis and management of brain tumors.

227           Primary diagnostic categories where some authors have suggested  
228 that MRS may present important diagnostic information are:

229

230           **Distinguishing single metastatic lesions from primary tumors of**  
231           **the CNS, such as astrocytomas**

232           This distinction is important, because single brain metastatic lesions  
233 would trigger a whole-body diagnostic workup for the source of the tumor,  
234 whereas primary brain tumors would be staged and treated as such. The  
235 treatment regimens for different metastatic types of tumors vary greatly. In  
236 virtually all cases, metastatic lesions are treated with regimens

237 considerably different than primary brain tumors, so establishing the exact  
238 nature of the neoplasm is exceedingly important in treatment planning.

239

### 240 **In distinguishing abscesses from CNS tumors**

241 Diagnosing an abscess quickly is critical. The clinical presentation  
242 of tumors and CNS abscesses in the Medicare population overlap  
243 significantly. Mistaking an abscess for a tumor can lead to a significant  
244 delay in diagnosis that can be catastrophic, because diagnosing a tumor  
245 may involve a relatively long workup. Rapid intervention in the case of an  
246 abscess can result in minimizing neurologic damage, leaving the patient in  
247 a high-functioning state.

248

### 249 **Tumor grade**

250 In primary CNS tumors, MRS may provide a more accurate means  
251 of determining tumor grade, and hence prognosis, than conventional  
252 anatomic MRI imaging with the contrast agent, gadolinium. Currently,  
253 tumor grade is estimated by its potential to enhance with gadolinium. The  
254 specificity of this diagnostic means is only moderate. Establishing the  
255 grade is important in determining treatment protocol. Low-grade tumors  
256 are often simply watched, whereas high-grade tumors are often de-bulked,

257 irradiated and sometimes treated with chemotherapy. If a technique  
258 produces sufficient specificity for tumor grade, a biopsy could be foregone  
259 in many instances. MRS may have an advantage over biopsy in reducing  
260 sampling error as well.

261

262 **In distinguishing peripheral neuroectodermal tumors (PNET)**  
263 **from astrocytic lesions in adults**

264 The ability to distinguish these tumors reliably could speed treatment  
265 of PNETs. These are typically very aggressive tumors that may sometimes  
266 respond to chemotherapy more readily than astrocytic tumors. Similarly, it  
267 is important to distinguish “bright spots” on conventional T2-weighted MRI  
268 imaging, associated with neurofibromatosis type 1 (NF1), from astroglial  
269 tumors occurring in this same patient population. Neurofibroma bright  
270 spots are hamartomas that typically do not expand in size. Follow-up  
271 exams are usually not necessary. The astrocytomas associated with NF1  
272 are low grade, and typically do not progress to high-grade tumors.  
273 Nonetheless, they can grow in size and are typically followed with imaging  
274 studies.

275

276 **Biopsies**

277 MRS has also been recently investigated for use in biopsies. Biopsy  
278 guidance is an area where MRS may reduce sampling error associated  
279 with determination of tumor grade (and prognosis) in primary CNS tumors.  
280 Accurate determination of tumor grade is important in determining  
281 prognosis and adjuvant therapy.

282

283 **1.3.3 Patient management and planning for surgery**

284 The management of CNS tumors depends on tumor type and  
285 multiplicity. In primary astrocytomas of the CNS, treatment depends on  
286 grade. Low-grade tumors (WHO classification grades 1-2) are usually  
287 observed, with follow-up, if small, and do not represent an immediate  
288 neurological crisis. In cases of neurologic crisis, tumors are either excised  
289 or debulked. In high-grade astrocytomas, tumors are debulked surgically,  
290 followed by whole-brain radiation.

291 Single metastatic brain lesions have conventionally been excised  
292 when in accessible locations. Excision is often accompanied by  
293 chemotherapy. Multiple lesions have conventionally been treated with  
294 whole brain radiation and chemotherapy. Gamma knife therapy (focused  
295 stereotactical radiation) has become an important and increasingly used



296 alternative means of treating both single and multiple metastatic lesions.  
297 Its use in single lesions depends on the primary tumor's sensitivity to  
298 radiation.

299 In patients treated for CNS tumors, MRS may provide important  
300 diagnostic criteria for:

301

### 302 **Determining tumor recurrence**

303 Tumor recurrence changes the prognosis of patients. Because  
304 recurring brain tumors are associated with a shortened life span, prognosis  
305 is important for patients to plan the final stages of their lives. Prognosis  
306 can, in some cases, be improved by additional focused radiation. This  
307 treatment, either alone or with additional chemotherapy, is usually not  
308 administered until there is definite evidence of tumor recurrence.

309

### 310 **Distinguishing radiation necrosis from tumor recurrence**

311 The rate of tumor recurrence has prognostic value, as well as  
312 therapeutic implications. However, the presence of mixed recurrent tumor  
313 and radiation necrosis is common. Radiation necrosis would contraindicate  
314 additional radiation. While the effects are significant, they are not usually  
315 related to eventual mortality. Investigators have suggested that MRS could

316 distinguish recurrent tumor from radiation necrosis under some  
317 circumstances.

318

### 319 **Determining tumor response to therapy**

320 Establishing that tumors are responding to the designated treatment  
321 is imperative, in determining if treatment (with its associated morbidity)  
322 should be continued, discontinued or changed to a different regimen.

323

### 324 **Surgical treatment planning**

325 Claims have been made that MRS provides important information for  
326 guidance of gamma knife therapy. It has been suggested that MRS has  
327 improved accuracy in determining tumor extent and better delineates the  
328 area to be treated with focused radiation.

329

## 330 **1.3.4 Factors that may affect performance of MRS**

331

### 332 **Location of lesion including proximity to bone and sinuses**

333 The technique of MRS requires careful “shimming” of the magnetic  
334 fields --- adjusting the magnetic fields around the tissue of interest so that  
335 these fields are homogeneous. Variations in the magnetic fields mis-  
336 register the spectral peaks, as the frequency sensitivities of chemical

337 structures are also affected by the external magnetic field strength.  
338 Sudden dramatic changes in tissue composition, such as adjacent air or  
339 bone, can result in the inability to correctly shim the magnet field. This can  
340 result in distorted and non-usable data. Therefore, lesions that are small,  
341 and abut bone or air-filled structures, such as the sinuses, can present  
342 problems during MRS analysis.

343

#### 344 **Operator issues**

345 While standard MRI technologists are seldom specifically trained in  
346 MRS, commercial software has become available that is less sensitive to  
347 operator error. Nevertheless, many current uses of MRS for brain tumors  
348 require precise localization that demands an understanding of MRS  
349 positioning requirements that with which many technologists are not  
350 acquainted. Multivoxel MRS techniques may have reduced these problems  
351 to some degree. However, accurate placement to achieve the desired  
352 results is still necessary. It may therefore be necessary for a trained  
353 neuroradiologist familiar with MRS to be available for voxel placement.

354

355           **Size/position of voxel**

356           Current commercial software enables either multivoxel or single voxel  
357 spectroscopy to be performed. Manufacturers have pre-set values for slab  
358 thickness and voxel size in their software. However, if mandated by  
359 conditions, these parameters may be changed by the investigator.  
360 Likewise, in single voxel studies, there are default values for voxel size and  
361 position. However, specific conditions, such as tumor size, location and  
362 relative positioning of the voxels near artifact-producing structures can  
363 require changes in size. The investigator must remember that the time of  
364 acquisition changes with the cube of the volume or square of the area.  
365 Additionally, the voxels must avoid overlapping with structures containing  
366 only cerebrospinal fluid, such as the ventricles, Sylvian fissure and  
367 choroidal fissures. These regions contain some, but not all, of the chemical  
368 compounds analyzed in the brain. Hence they can distort key ratios in the  
369 compounds used in interpretation.

370

371           **Concurrent disease**

372           Concurrent disease can occasionally produce problems when using  
373 MRS for evaluating tumors. Tumors lying near areas of old infarcts and  
374 ischemic changes can distort chemical ratios used in interpretation.

375 Similarly, concurrent demyelinating disease can produce additional  
376 distortions. In general, with single voxel technique, careful voxel  
377 placement, and containing voxels from appropriate control areas can  
378 alleviate the problem. Alternatively, selecting appropriate voxels from  
379 control areas in a multivoxel study could accomplish the same objective.

380

### 381 **Hardware and software**

382 Hardware and software both affect the application of MRS. In  
383 general, studies on magnets with field strengths less than 1.5 tesla (unit of  
384 magnetic flux) require too much time to be used on a routine basis. High  
385 field strength magnets, such as current 3 tesla systems have a time  
386 advantage (that can be converted into a space localization advantage).

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## **2. METHODS**

### **2.1 Classification of diagnostic studies**

The Medicare Coverage Advisory Committee (MCAC) report on “Recommendations for Evaluating Effectiveness; Executive Committee Working Group Medicare Coverage Policy” (Executive Committee Working Group, 2001) (<http://www.cms.hhs.gov/mcac/8b1-i9.asp>) developed recommendations for evaluating evidence. It pointed out that although direct evidence is preferable, few studies directly measure the effect of diagnostic tests on health outcomes. Rather, studies typically focus on whether diagnostic tests are technically feasible or on effects on accuracy. These points apply to MRS. Few well-designed studies evaluate the impact of this test on clinical outcomes.

To systematically review the level of assessment of each study, we used a model described by Fineberg et al. (1977), Fryback and Thornbury (1991), and Adams (1997) to categorize the level of assessment achieved by the studies:

406

407

### CATEGORIES OF DIAGNOSTIC ASSESSMENT

CATEGORY	CATEGORY DESCRIPTION	EXAMPLES OF MEASURES
1	Technical feasibility and optimization	Ability to produce consistent spectra
2	Diagnostic accuracy	Sensitivity and specificity
3	Diagnostic thinking impact	% of times clinicians' subjective assessment of diagnostic probabilities change
4	Therapeutic choice impact	% of times therapy planned prior to MRS changed after MRS
5	Patient outcome impact	% of patients who improved with MRS compared to % without MRS
6	Societal impact	Cost-benefit analysis

408

409 Note that the Institute of Medicine has also described similar criteria for  
 410 evaluating diagnostic tests.

411 According to the MCAC assessment criteria, the studies most useful  
 412 for assessing MRS would be Category- 2 or higher. In consultation with  
 413 AHRQ and CMS, it was decided to review in depth only Category- 2 and  
 414 higher studies.

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419           **2.2 Literature search**

420           An OVID search of the MEDLINE<sup>®</sup> database was conducted on  
421 November 6, 2002. Filters and limitations were used to eliminate  
422 inappropriate publications, with inclusion and exclusion criteria developed  
423 to identify articles to be reviewed. The search used applicable MeSH  
424 headings and textwords with appropriate Boolean operators. After filtering  
425 irrelevant publication types, the search resulted in 959 citations for  
426 download and screening. Hand screening of the abstracts resulted in  
427 accepting 137 citations for complete article retrieval. All abstracts were  
428 reviewed to identify full articles that met the criteria.

429           In addition, abstracts from the following relevant professional society  
430 proceedings for the years 2001 and 2002 were reviewed and included in  
431 the analyses:

- 432           • American Society of Neuroradiology (ASNR)
- 433           • Radiological Society of North America (RSNA)
- 434           • International Society for Magnetic Resonance in Medicine (ISMRM)

435

436           Note that the information available from abstracts in such proceedings is  
437 extremely limited in comparison to that available in full articles. Additionally,  
438 the peer review process is generally not comparable to the process for full



439 articles. Finally, the International Network of Agencies for Health  
440 Technology Assessment (INAHTA) (<http://www.inahta.org/>) and National  
441 Guidelines Clearinghouse (NGC) (<http://www.guideline.gov/index.asp>)  
442 databases were searched for relevant citations.

443

### 444 **2.3 Inclusion/Exclusion Criteria**

445 The inclusion criteria for accepting studies included the use of  
446 hydrogen proton magnetic resonance spectroscopy (hydrogen) MRS on  
447 patients with suspected or known brain tumors. Only in vivo studies with a  
448 minimum of six adult human subjects were included. Explicitly excluded  
449 were studies of only healthy patients or studies of exclusively HIV/AIDS  
450 patients. In addition, studies of phosphorus or other types of MRS were  
451 excluded.

452

### 453 **2.4 Search Results**

454 One hundred thirty-seven publications were retrieved. Further review  
455 of those retrieved publications with application of inclusion criteria yielded  
456 85 studies for inclusion in the report. The detailed search strategy follows:

457

458

459 MEDLINE <1966 to October Week 4 2002>

460

461 #	461 Search History	461 Results
463 1	463 exp Magnetic Resonance Spectroscopy/	463 92891
464 2	464 limit 1 to human	464 22632
465 3	465 limit 2 to English language	465 20499
466 4	466 exp neoplasms/	466 1409117
467 5	467 (tumor or cancer\$ or neoplasm\$ or neoplas\$ or	
468	468 lesion\$ or mass).tw.	468 1131920
469 6	469 (brain or cranial or cerebr\$).tw.	469 479504
470 7	470 5 and 6	470 71583
471 8	471 4 and 6	471 50293
472 9	472 7 or 8	472 93338
473 10	473 exp brain neoplasms/	473 69674
474 11	474 3 and (9 or 10)	474 1231
475 12	475 limit 11 to (addresses or bibliography or biography or	
476		

477

478 #	478 Search History	478 Results
480	480 dictionary or directory or editorial or festschrift or	
481	481 historical article or interview or lectures or legal cases or	
482	482 legislation or letter or news or newspaper article or	
483	483 patient education handout or periodical index)	483 24
484 13	484 Case Report/	484 1059907
485 14	485 11 not (12 or 13)	485 959

486

487

488 Two hundred forty-one abstracts were identified in the search of the  
489 three professional society proceedings and fifty-one met the inclusion

490 criteria and are included in this report. No relevant material was identified  
491 in either the INAHTA or NGC databases.

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## **2.5 Data Extraction**

496 As described above, our review entailed classifying each study into  
497 five categories. For those studies in Category- 1 we extracted data  
498 summarizing the following aspects of each study for later use in an  
499 evidence table: study characteristics (design, enrollment, patient  
500 characteristics), MRS technical aspects (number and volume of voxels),  
501 and study objectives (differential diagnosis and treatment planning).

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For the studies in Category- 2 and above, narrative analyses were  
504 provided for each study. Studies in these categories were also evaluated  
505 with respect to their methodological adequacy.

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### 3. RESULTS: Full Published Studies

The following table shows the number of studies in each of the categories. After reviewing the 959 abstracts and 137 retrieved articles, 75 studies were classified as Category-1 Technical feasibility studies. Ten studies were identified as providing information beyond that of the technical feasibility category. An additional 10 studies were added to Category- 1 and 1 study added to Category- 2 from references given by peer reviewers of the draft version of this report. In this section we report on the 96 published full-length studies classified using the approach described above. There were eight articles for Category-2, two articles for Category-3 (one study also qualify for Category-4), two articles for Category- 4 (one article shared with Category-3), and none for Category- 5 or Category- 6. Nearly all the studies identified were in Categories- 1 and 2, with the vast majority in Category- 1. The following table summarizes these results:

CATEGORY	DESCRIPTION	#
1	Technical feasibility and optimization	85
2	Diagnostic accuracy	8
3	Diagnostic thinking impact	2*
4	Therapeutic choice impact	2*
5	Patient outcome impact	0
6	Societal impact	0

522 \*One study overlapped Category- 3 and Category- 4.

523 **3.1 Category- 1 studies: Technical Feasibility**

524  
525 Evidence Table 1 shows selected characteristics of the technical  
526 feasibility (Category- 1) studies. Included in this table are the year of  
527 publication, country in which the research was conducted, study  
528 characteristics including number of diseased (case) and non-diseased  
529 (control) patients, method of patient enrollment, diagnostic status, and age.  
530 The table also shows the size of the volume of tissue (voxel) of interest as  
531 well as whether single or multiple voxel sampling was used. Finally, the  
532 table indicates the principal clinical study objectives: tumor differentiation,  
533 tumor grading, distinguishing primary tumor tissue from recurrent tumor  
534 and from metastases, and identifying necrotic tissue.

535 We reviewed 85 Category- 1 studies published from 1988 through  
536 2003 involving approximately 2434 patients; fifty (59%) of the studies were  
537 published before 2000. There was extensive international representation in  
538 these studies. Twenty-four (28%) were from the US, 15 (18%) were from  
539 Japan, and 19 other countries were represented. The ages of patients  
540 included in the studies varied considerably; the range was from 1- 88  
541 years, but we excluded studies that consisted predominantly of pediatric  
542 patients.

543           Almost all of the studies were prospective, with several retrospective  
544 and several of unknown design. The largest study included 120 cases.  
545 Many of the studies did not include control patients; for those studies that  
546 did, however, the maximum number of healthy controls was 151. One  
547 study reported approximately 300 diagnostic studies of controls. The  
548 mechanism used to enroll patients was generally not reported. In almost all  
549 of the studies, the disease status of the participants was ascertained via  
550 biopsy, although in a few instances the ascertainment was via clinical  
551 assessment only.

552           Single voxel sampling was the predominant methodology, although  
553 multiple sampling was also often used, and a combination of the two  
554 approaches was sometimes employed. In some articles the technique was  
555 not reported. Voxel volumes ranged widely.

556           Tumor differentiation (36 studies) and grading (30 studies) were the  
557 most frequently cited clinical objectives. Identifying necrotic tissue (15  
558 studies) was also a frequent objective. Distinguishing metastases from  
559 primary tumors (5 studies) and recurrent from primary tumors (four studies)  
560 were less frequent objectives.

561 While not shown in the table, nearly all of these studies reported that  
562 metabolite peaks were obtained and metabolite ratios calculated. The  
563 authors analyzed spectral patterns using these measures.

564

### 565 **3.2 Category-2: Studies that Evaluate Test Performance**

566 Eleven studies were identified as providing information beyond the  
567 technical feasibility category. There were eight articles for Category-2, two  
568 articles for Category-3 (one study also qualify for Category-4), two articles  
569 for Category-4 (one article shared with Category-3), and none for Category-  
570 5 or Category-6.

571 A total of eight studies provided data for Category-2. Studies in this  
572 category could be further grouped into studies with the main purpose of  
573 differentiating tumors from non-tumors (three), grading of tumors (two),  
574 differentiating intracranial cystic lesions (one), and assessing the  
575 incremental value of MRS added to MRI (one). The purposes of the studies  
576 within the same group were sufficiently different so that combining or  
577 comparing studies within the same group was infeasible.

578 One group of investigators from the Medical College of Wisconsin  
579 published three articles (Rand et al., 1997; Adamson et al., 1998; Butzen et  
580 al., 2000) using overlapping patient samples but addressing different

581 research issues. Fifty-five MRS spectra belonging to 53 patients in the  
582 1997 article were included in the 99 MRS spectra evaluated in the 2000  
583 article. The study by Adamson et al. (1998) was a retrospective analysis of  
584 78 patients from the same study population and is discussed under the  
585 Category-4 section.

586

### 587 **3.2.1 Studies Differentiating Neoplasm from Non-neoplasm**

588

589 Rand et al. (1997) evaluated 55 brain lesions in a consecutive series  
590 of 53 patients between September 1994 and December 1995. The patients  
591 included 31 males and 22 females between the ages of 14 and 81 years  
592 (mean 45 years), and they had suspected brain neoplasm or recurrent  
593 neoplasia. The purpose of the study was to measure the accuracy of  
594 single-voxel, image-guided proton MRS in distinguishing normal from  
595 abnormal brain tissue and neoplastic from non-neoplastic brain disease.

596 Using voxel sizes of 1 to 3 cm<sup>3</sup>, MRS spectra were obtained using a  
597 clinical 0.5 Tesla MR system (manufacturer not stated) with a prototype  
598 head coil or a receive-only conformal surface coil. The voxel was centered  
599 over solid portions of the lesion and avoided necrotic debris or edema.

600 Spectra were interpreted by visual inspection. At the time of MRS,  
601 one of the four neuroradiologists and one MR spectroscopist prospectively



602 wrote a formal report using available clinical data and imaging studies. The  
603 unblinded readers interpreted the spectra as diagnostic or not, and if  
604 diagnostic, as neoplasia or non-neoplasia. Four neuroradiologists blinded  
605 to the clinical data and MRI results interpreted spectra retrospectively. The  
606 blinded readers classified the spectra as diagnostic or not, if diagnostic as  
607 normal or abnormal, and when abnormal as neoplasia or non-neoplasia.

608         For blinded interpretations, control and patient spectra were  
609 presented in random order. Blinded readers interpreted the results  
610 independently. Additional measures were taken to minimize biases in the  
611 interpretation of results.

612         The blinded readers rated the spectra from one to 100 as normal or  
613 abnormal, and as neoplastic or non-neoplastic, respectively. For the  
614 purpose of estimating test performance, a score of less than 50 was  
615 defined as negative (normal or non-neoplastic), a score of 50 and above  
616 was defined as positive (abnormal or neoplastic). The full range of the  
617 scores from each reader was used to create receiver operating  
618 characteristic (ROC) curves.

619         Sensitivity, specificity, positive predictive value, negative predictive  
620 value, and accuracy were calculated for the unblinded reader and each  
621 blinded reader for untreated patients and treated patients separately.

622 Spectra from 55 brain lesions in 53 patients were included in the  
623 analysis. In two patients, two lesions were studied. Fourteen patients (15  
624 lesions) had received treatments for brain neoplasia before undergoing  
625 MRS. Histological diagnoses were available for 50 lesions. Diagnoses were  
626 established in three cases of infarcts by clinical follow-up and serial  
627 radiologic studies (CT, MRI, MR angiography, catheter angiography, or a  
628 combination) in which the lesions diminished in size. Diagnoses were  
629 established in two cases of acute demyelinating disease by clinical follow-  
630 up and reduction of lesion size on serial MRI.

631 The distribution of 42 neoplasia final diagnoses included: one  
632 astrocytoma-not otherwise specified, four astrocytoma grade I, four  
633 astrocytoma grade II, two astrocytoma grade III, 10 astrocytoma grade IV –  
634 one glioblastoma multiforme, one giant cell astrocytoma, one  
635 oligodendroglioma, four mixed glioma, one ganglioglioma, one  
636 ependymoma, six meningioma, four metastases, and two dysembryoblastic  
637 neuroepithelial tumor. The distribution of 13 non-neoplasia final diagnoses  
638 included: one Rathke's pouch cyst, three infarct, one parasitic infection,  
639 one sarcoidosis, one acute inflammation and gliosis, two demyelinating  
640 disease, one radiation necrosis without neoplasm, one vasculitis, one

641 arteriovenous malformation with old hemorrhage, and one neuroglial (gyral)  
642 dysplasia.

643         Blinded readers disqualified 20 (9%) of 213 patient spectra as non-  
644 diagnostic because of unacceptably low signal to noise ratios, ambiguous  
645 resonance assignments, unacceptably broad resonances, lack of  
646 detectable metabolite resonance, equivocal findings of neoplasm versus  
647 non-neoplasm, or a combination of the above.

648         Unblinded readers produced 40 true-positive, 12 true-negative, no  
649 false-positive, and two false-negative diagnoses. One spectrum was  
650 interpreted as nondiagnostic. Compared to the reference standard, the  
651 sensitivity, specificity, PPV, NPV, and accuracy of MRS to distinguish  
652 between neoplastic and non-neoplastic spectra for the unblinded readers  
653 were 0.95, 1.00, 1.00, 0.86, and 0.96, respectively.

654         Compared to the reference standard, the four blinded readers  
655 accumulated 12 false-positive interpretations on eight spectra and 22 false-  
656 negative interpretations on 13 spectra. The sensitivity, specificity, PPV,  
657 NPV, and accuracy of MRS to distinguish between neoplastic and non-  
658 neoplastic spectra for the four blinded readers averaged 0.85, 0.74, 0.92,  
659 0.61, and 0.83, respectively. The test performance showed better results  
660 when only untreated patients were analyzed.

661 This study was exemplary for many aspects in this category. This  
662 was a prospective study and included a variety of diagnoses, used ROC  
663 analysis and multiple blinded readers to interpret the spectra results, and  
664 used well-defined reference standards and methods to minimize bias. The  
665 number of patients with and without neoplasm and the number of  
666 diagnoses was relatively small, however. The lack of a quantitative  
667 analysis of the MRS spectra profile also diminishes the ability to compare  
668 their results with other studies.

669 The population studied by Butzen et al. (2000) from the Medical  
670 College of Wisconsin is a superset of the patient population studied by  
671 Rand et al. in 1997. The purpose of this study was to compare a logistic  
672 regression (LR) model with blinded and unblinded qualitative MRS  
673 interpretations for the discrimination of neoplastic from non-neoplastic brain  
674 lesions using MRI-guided single voxel proton MRS data. The MR system  
675 and technique used were described in the paper by Rand et al. Ninety-nine  
676 consecutive patient spectra (the number of patients was not reported) with  
677 suspected brain neoplasms or recurrent neoplasia referred for MRS were  
678 evaluated by the LR model, of which 55 were evaluated by Rand et al. in  
679 the earlier study.

680           The LR model computed the probability of neoplasm ranging from  
681 zero to one. A cutoff probability of 0.8 for a positive MRS examination for  
682 neoplasia was determined by adjusting the cutoff to obtain equal rates of  
683 false-negative and false-positive results. Qualitative interpretations were  
684 made by two blinded neurologists and by one of five unblinded staff  
685 neuroradiologists and one staff spectroscopist.

686           The LR model was applied to 99 spectra with a sensitivity of 87% and  
687 a specificity of 85%. One blinded reader evaluated 86 spectra with a  
688 sensitivity of 75% and a specificity of 90%. The second blinded reader  
689 evaluated 90 spectra with a sensitivity of 88% and a specificity of 58%. The  
690 unblinded reader evaluated 95 spectra with a sensitivity of 89% and a  
691 specificity of 92%. The results of the blinded and unblinded readers were  
692 similar to those in the earlier study. Using a threshold of greater than one  
693 for the metabolite ratio Cho/NAA (NAA = N-acetylated compounds) to  
694 classify tumors, the sensitivity for 99 spectra was 79% and the specificity  
695 was 77%.

696           McKnight et al. (2002) tested a statistical index derived from a linear  
697 model of choline vs. NAA for discriminating neoplastic from non-neoplastic  
698 brain lesions. A subset of 26 patients in this study with high grade tumors  
699 were also reported on by Pirzkall et al. in a Category-1 study. Multi-voxel (1

700 cm<sup>3</sup>) 3D-MRSI was performed with a 1.5 Tesla General Electric Medical  
701 Systems Signa scanner (General Electric Medical Systems, Signa;  
702 Milwaukee, WI) on 68 patients (ages unknown) with suspected gliomas.  
703 The statistical model yielded an MRS-derived score (Cho-NAA Index—the  
704 “CNI”) summarizing the degree of difference between relative Cho and  
705 NAA levels in a specific voxel and that of a population of control voxels for  
706 each patient.

707         Of the original 68 patients, biopsies revealed that 26 had Grade II  
708 gliomas, 26 had Grade III gliomas, and 16 had Grade IV gliomas. Only 44  
709 patients gave consent for their surgeons to be guided during the biopsy by  
710 MRS-guided instructions to sample four voxels --- one each with a high CNI  
711 score, one with a low score and two with intermediate values. (The  
712 remaining 24 patients’ MR images and CNI scores were used in another  
713 analysis of the distribution of metabolic abnormality with hyper intense  
714 lesions on T<sub>2</sub>-weighted MR images and contrast-enhancing lesions.)

715         The one hundred biopsy samples from the 44 patients yielded the  
716 following histological classification of gliomas: Grade II: 36; Grade III: 34;  
717 and Grade IV: 23. Seven of the samples were nontumorous. The patient-  
718 level distribution of gliomas was: Grade II: 12; Grade III: 21; and Grade IV:  
719 11. None of the patients were tumor-free.

720           The difference between CNIs of tumor and non-tumorous samples  
721 was highly significant. An analysis to assess the ability of the CNI to  
722 differentiate between tumor and non-tumorous samples yielded an ROC  
723 area of .94. With a CNI cutoff of 2.5, the sensitivity of this test was 90%  
724 and the specificity was 86%. The 95% bootstrap confidence interval for the  
725 sensitivity was 84 -96% and for specificity was 56-100%. These  
726 sensitivities were tumor-level, not patient-level.

727           This study also used the MRS CNI methodology to examine the  
728 proportion of patients of all 66 patients with evidence of tumor outside the  
729 area of contrast enhancement. Regardless of tumor grade, 41-45% of  
730 hyperintense lesions showed metabolic evidence of tumor (CNI >2.5), and  
731 36-45% of non-enhancing lesions also showed such evidence.

732           Finally, a sub-analysis analyzed grade. There were 7 tumors with  
733 heterogeneous histological findings; in three of these cases, the CNIs did  
734 not correlate with the histological grade.

735           This study had several limitations. The authors do not describe how  
736 patients were enrolled in the study, nor was the analysis of MRS results  
737 blinded to final diagnosis. The small number of non-tumorous samples  
738 limited statistical power, and the restriction of tumors to gliomas limited  
739 generalizability. There may have been bias due to the number of dropouts.

740 Kimura et al. (2001) retrospectively evaluated the accuracy of single-  
741 voxel MRS spectra in patients with ring-like enhanced lesion using  
742 gadolinium-enhanced MRI. Forty-five patients including 29 men and 16  
743 women between the ages of 26 to 75 years with various brain lesions were  
744 studied. The diagnoses included 19 metastases, 10 glioblastoma, seven  
745 radiation necrosis, five brain abscesses, and four cerebral infarctions.

746 MRS was performed with a 1.5 Tesla Signa Horizon System (GE  
747 Medical System, Milwaukee, WI). The investigators evaluated two types of  
748 volume of interest (VOI). One VOI was selected to include the whole ring-  
749 like enhanced rim and the central region of the lesion (whole lesion). The  
750 second type of VOI was selected to include only the non-enhanced inner  
751 region. The size of the voxel was not reported in the article. Quantitative  
752 analyses of spectra were performed on Cho, Cr, NAA, Lac, and Lip signals  
753 (Cho = choline; Cr = total creatine; NAA = N-acetylated compounds;  
754 Lac=lactate; Lip = lipids, protein, and lactate). Three metabolite ratios  
755 (Cho/Cr, Lac/Cr, NAA/Cr) were calculated and used for analyses.

756 For the whole lesions, the mean Cho/Cr ratio of metastases was 4.56  
757 and 4.12 for glioblastoma. The mean Cho/Cr ratio for radiation necrosis  
758 was 2.33 and 1.48 for cerebral infarction. Significant differences were found  
759 for: metastases and radiation necrosis, metastases and cerebral infarction,



760 and glioblastoma and cerebral infarction. Significant differences in the  
761 Cho/Cr ratios between the whole lesion and inner region were found in the  
762 spectra of metastases and glioblastoma. There were no significant  
763 differences among the lesion types for the Cho/Cr ratios in the inner region.

764 The investigators found that using a Cho/Cr ratio of 2.48 for the whole  
765 lesion, the lowest rate of misdiagnosis was achieved in differentiating  
766 neoplasm from non-neoplasm. The positive predictive value using this  
767 threshold for metastatic brain tumors and glioblastoma was 89% (95% CI,  
768 65 - 99%) and 60% (95% CI, 26 - 88%), respectively. The positive  
769 predictive value of a Cho/Cr ratio of less than 2.48 for diagnosing radiation  
770 necrosis and cerebral infarction were 71% (95% CI, 29 - 96%) and 100%  
771 (95% CI, 40 - 100%), respectively.

772 The lowest rate of misdiagnosis in differentiating metastases and  
773 radiation necrosis was achieved using a Cho/(Lip or Lac) ratio of 0.3 for the  
774 whole lesion. The positive predictive value of using a threshold value of  
775 greater than 0.3 to diagnose metastases was 94% (95% CI, 73 - 99%). The  
776 positive predictive value of using a threshold value of less than 0.3 to  
777 diagnose radiation necrosis was 100% (95% CI, 59 - 100%).

778           The relatively small sample size, narrow spectrum of brain lesions,  
779 and retrospective nature of this study limited the generalizability of this  
780 study. In addition, abscesses were excluded from the analyses.

781

### 782           **3.2.2 Clinical Utility of MRS added to MRI**

783

784           Moller-Hartman et al. (2002) evaluated the clinical utility of MRS  
785 added to MRI for the differentiation of intracranial neoplastic and non-  
786 neoplastic mass lesions. The study population consisted of a consecutive  
787 series of 176 patients presented to the neuroradiology department with  
788 focal intracranial mass lesions following MRI and/or CT imaging.  
789 Spectroscopic studies were performed using a 1.5 Tesla whole-body MR  
790 scanner (Magnetom Vision, Siemens). All patients underwent a single voxel  
791 MRS with a mean voxel volume of 8 cm<sup>3</sup> (range 4 - 12 cm<sup>3</sup>). The voxel was  
792 placed in the solid part of the lesion excluding necrotic or cystic tumor parts  
793 or adjacent edematous areas. An acceptable voxel had to contain at least  
794 an estimated 70 percent tumor tissue. Whenever feasible, a reference  
795 spectrum of the same voxel size was acquired in the homologous region in  
796 the contralateral brain.

797           Within 10 days of MRS, histological diagnosis was obtained by  
798 stereotactic biopsy or craniotomy and open biopsy, except in nine (of 25)

799 cases of brain abscesses or focal inflammatory brain disease and nine (of  
800 nine) cases of cerebral infarction. Features on MRI or CT, clinical course,  
801 cerebrospinal fluid findings, and blood tests made the final diagnoses of the  
802 non-biopsied cases. Twelve out of the 176 spectra were of poor quality and  
803 were excluded from further evaluation. Final diagnoses for the remaining  
804 164 interpretable spectra included 23 low-grade astrocytomas, 28  
805 anaplastic astrocytomas, 39 glioblastomas, four PNETs or  
806 medulloblastomas, 18 metastases, nine meningiomas, nine neurinomas, 25  
807 cerebral abscesses and nine brain infarctions.

808         Two neuroradiologists independently reviewed the combined MRI  
809 and MRS results blinded to the final diagnoses and two other  
810 neuroradiologists independently reviewed only the MRI results blinded to  
811 the final diagnoses. A diagnosis was classified as “correct” if the reader  
812 correctly assigned the case to the type of intracranial mass lesion and the  
813 tumor grade, according to the WHO classification of the final diagnoses. A  
814 “no evidence diagnosis” was assigned if the neuroradiologist could not  
815 decide between several diagnoses. The article did not report whether the  
816 two neuroradiologists read all the images or spectra in the same group or  
817 how discrepancies between the readers were resolved.

818 Tumor metabolite signal intensities were expressed as the  
819 percentage of the corresponding metabolites of the reference spectrum  
820 using measurements of the peak area signal intensity of each metabolite  
821 (NAA, Cr, and Cho) in the lesion. Two metabolite ratios (Cho/Cr and  
822 NAA/Cr) were also calculated.

823 Compared with the reference spectrum on the contralateral side of  
824 the brain, the Cr level was about 75-80% among the gliomas and there  
825 were no significant differences between the different tumor grades. The  
826 levels of Cr in the metastases, abscesses, and infarctions were about 40-  
827 50%, compared to the reference. The Cho levels decreased to 70-80% in  
828 infarctions and abscesses, and increased in metastases, PNET, and  
829 gliomas. The Cho level progressively increased with the tumor grade. The  
830 Cho/Cr ratios were: infarction = 1.45; astrocytoma I = 1.33; astrocytoma II =  
831 2.13; astrocytoma IV = 3.93; PNET = 18.4; metastases = 3.97; abscesses  
832 = 1.52; meningioma = 4.81; neurinoma = 3.08.

833 Of the 176 spectra, conventional MRI alone made 97 (55.1%) correct  
834 diagnoses, 27 (15.3%) incorrect diagnoses, 52 (29.6%) no evidence  
835 diagnoses, and no examinations without diagnostic value. MRS added to  
836 MRI produced 124 (70.5%) correct diagnoses, 16 (9.1%) incorrect  
837 diagnoses, 24 (13.6%) no evidence diagnoses, and 12 (6.8%)

838 examinations without diagnostic value. There was no case in which a  
839 correct diagnosis made by MRI alone was interpreted incorrectly by the  
840 combination of MRI and MRS.

841

### 842 **3.2.3 Studies on Tumor Grading**

843

844 Roser et al. (1997) prospectively evaluated 35 MRS spectra in 17

845 patients with suspected glial brain tumors. The purpose of the study was “to

846 apply the metabolic features found in a previous study of 21 healthy

847 controls and humans with gliomas to a new cohort of patients with a

848 suspected glial brain tumor and other healthy volunteers.” The age and sex

849 of the patient population were not reported. None of the patients had

850 received stereotactic biopsy, open surgery, or radiation therapy before

851 MRS. Sterotactic biopsy or open surgery was performed within a few days

852 after MRS.

853 MRS spectra of single-voxel size  $8 \text{ cm}^3$  were acquired using a 1.5

854 Tesla MR system (Siemens Magnetom SP 400, Siemens Medical Systems,

855 Erlangen, Germany). The VOI was placed as close as possible to the tumor

856 center and covered at least 75% of the tumor tissue.

857 Using “training” data from an earlier study of 21 healthy controls and

858 patients with gliomas, the investigators calculated five ratios (NAA/Cr,

859 MGG/Cr, Cho/Cr, Gl/Cr, Lip/Cr) using 6 metabolite resonance  
860 measurements (NAA = N-acetylated compounds; Cr = total creatine; MGG  
861 = macromolecules, glutamine, and glutamate; Cho = choline; Gl = glycine  
862 and myo-inositol; Lip = lipids, protein, and lactate). These five metabolite  
863 ratios were used in an orthonormal discriminant vector (ODV) analysis  
864 (Kauppinen et al., 1993) to construct a graph of two-dimensional metabolite  
865 space. The two axes were the ODV results based on a linear combination  
866 of the five metabolite ratios. By plotting the two ODV results of the  
867 metabolite ratios of individual patients from the training data, different tumor  
868 grades and healthy controls occupy distinct regions in the graph that could  
869 be classified as high grade, low grade and healthy volunteers.

870         In the validation study, the correlation of superimposing new patients'  
871 data onto the classification derived from the training data was noted.  
872 Histological diagnoses of the new patients included ten glioblastoma  
873 multiforme, two astrocytoma grade III, and five astrocytoma grade II. All ten  
874 cases of glioblastoma multiforme were in the proximity of the high grade  
875 region defined by the training data. Four of five astrocytoma grade II were  
876 classified as low grade gliomas, and one was classified as high grade. One  
877 of the two astrocytoma grade III was classified as high grade and the other  
878 as low grade. In addition, the contralateral normal-appearing matter of

879 tumor patients was assigned as normal in six cases and low grade in two  
880 cases.

881 The results of this study cannot readily be generalized. Only 21  
882 healthy subjects and patients with glial brain tumor were selected in the  
883 development of the ODV equations. In the prospective validation study, all  
884 17 patients also had glial brain tumors; thus the results of this study cannot  
885 be generalized to populations with a broader spectrum of brain lesions. A  
886 much larger number of patients with a broader spectrum of brain lesions is  
887 needed to develop the diagnostic criteria and to verify the results.

888 Tedeschi et al. (1997) prospectively studied 27 patients with known  
889 brain gliomas to test the hypothesis that MRS can help detect malignant  
890 degeneration and/or recurrence (progressions). The 27 patients received  
891 from two to five MRS studies, a total of 72 MRS imaging studies were  
892 performed over 3.5 years. Repeated MRS studies were not based on a  
893 fixed time interval and the reasons for the repeated studies were not  
894 explicitly stated.

895 A 1.5 Tesla MR imager (manufacturer not stated) was used to  
896 acquire multi-voxel spectra. Nominal voxel size was  $0.83 \text{ cm}^3$ . At the time  
897 of each MRS study, a combination of clinical examination, MRI, positron  
898 emission tomography with  $^{18}\text{F}$ -fluorodeoxyglucose, and biopsy findings

899 (when available) were used to categorize each patient as having either  
900 stable or progressive disease.

901 The signal amplitude of each metabolite (Cho, NAA, Cr, Lac) in the  
902 tumor region of interest was normalized to the corresponding amplitude in  
903 a matching region of interest from a normal area of the contralateral brain  
904 in order to calibrate the signal intensities from different imaging studies and  
905 individuals to a common scale. The investigators used the percentage  
906 changes in the normalized Cho signal intensity between two consecutive  
907 studies to categorize patients into stable and progressive groups. They  
908 found that all progressive cases could be correctly classified using a Cho  
909 signal increase of more than 45% and all stable cases had increases of  
910 less than 35%. Thus, using a threshold of 40% Cho signal increase  
911 between visits, the sensitivity was 100% and specificity was 100%.

912 In addition to the normalized Cho measurements, the investigators  
913 also analyzed normalized NAA, Cr, and Lac, as well as the within-voxel  
914 metabolite ratios (NAA/Cho, NAA/Cr, Cho/Cr). Other than the normalized  
915 Cho measurement, they found no association of the other measurements  
916 with disease progression.

917



### 3.2.4 Differentiating Intracranial Cystic Lesions

918  
919  
920 Shukla-Dave et al. (2001) prospectively evaluated the accuracy of  
921 MRS in the differentiation of intracranial cystic lesions. Fifty-one patients  
922 including 23 men and 28 women between the ages of eight and 50 years  
923 (mean 33 years) with intracranial cystic lesions on conventional MRI were  
924 studied. Single-voxel MRS was performed using a 1.5 Tesla MR system  
925 (Magnetom, Siemens) on lesions greater than 8 cm<sup>3</sup>. A VOI of 4 to 8 cm<sup>3</sup>  
926 within the confines (sometimes including the rim) of the lesion was selected  
927 for MRS.

928 The criteria used to establish the diagnosis of cystic lesions were:

- 929 • Abscesses: lipid/lactate at 1.3 and amino acids at 0.9 ppm in all  
930 with/without additional resonances of succinate, acetate, alanine  
931 and glycine
- 932 • Glioma: lipid and/or lactate with choline
- 933 • Arachnoid cyst: presence of small resonance of lactate with very  
934 low signal to noise spectrum
- 935 • Hydatid cyst: very large succinate peak with lactate, alanine,  
936 acetate with absence of amino acids

937 Two investigators who did not know the MRI results, except that the  
938 lesions were cystic, interpreted the MRS spectra independently. However,

939 the rate of discrepancies and the method of resolution of discrepancies in  
940 the interpretation of the spectra results between the two investigators were  
941 not reported. The pre-operative diagnosis was based solely on the MRS  
942 results. All patients presumably underwent surgery for the intracranial  
943 cystic lesions. The final diagnosis was based on the results of  
944 histopathology, aspiration and culture of the contents. Fifty MRS spectra  
945 out of 51 were interpretable. Data for one case of acoustic neuroma was of  
946 poor quality and not included in the analysis.

947         Of the 51 cases, MRS correctly identified all 21 cases of abscess, all  
948 19 cases of glioma, all three cases of arachnoid cyst, and all three cases of  
949 hydatid cyst. MRS incorrectly diagnosed one case of xanthogranuloma and  
950 one case of infarct as glioma. A total of three inconclusive MRS diagnoses  
951 were later found to be glioblastoma multiforme, gliependymal cyst, and  
952 acoustic neuroma. Thus, MRS correctly diagnosed the pathology of  
953 intracranial cystic lesions in 46 of 51 (90%) cases, did not contribute to the  
954 diagnosis in three cases (6%) and falsely diagnosed benign lesions as  
955 malignant in two cases (4%).

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### **3.3 Category-3: Studies Conducted to Evaluate Diagnostic**

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#### **Thinking Impact**

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Two small prospective studies qualified for this category. The purpose of the study by Hall et al. (2001) was “to determine the utility of intraoperative MRS for targeting during brain biopsy using a skull-mounted trajectory guide.” The trajectory guide is commercially available and has been approved by the Food and Drug Administration (FDA) for the placement of deep brain stimulators, drug delivery catheters, and brain biopsies (Hall et al., 2001). The successful use of intraoperative MRS-guided brain biopsy might replace the conventional frame-based or frameless stereotactic techniques guided by either computed tomography (CT) or magnetic resonance imaging (MRI). In this setting, the CT or MRI are typically performed immediately or a few days before the biopsy. However, the opening of the dura mater and with the loss of cerebrospinal fluid may result in shifting the position of the lesion identified in the imaging studies (brain shift), which in turn might result in non-diagnostic stereotactic biopsy. A review of stereotactic brain biopsies found a diagnostic yield (proportion of biopsies containing useable diagnostic tissue) of 91% (Hall, 1999).

976 A total of 17 patients including 13 men and four women between the  
977 ages of 16 and 80 years suspected of brain tumors were evaluated in Hall's  
978 2001 prospective study. All patients had "turbo spectroscopic imaging  
979 (TSI)" (a multi-voxel MRS method) and seven patients had single-voxel  
980 spectroscopy in addition, for purposes of comparison. MRS spectra were  
981 obtained using 1.5 Tesla MR system (ACS-NT; Philips Medical Systems,  
982 Best, Netherlands) located within an intraoperative MRI suite. The VOI in  
983 the single voxel spectroscopy was  $1.5 \times 1.5 \times 1.5 \text{ cm}^3$  and the TSI used a  
984  $32 \times 32$  grid of spectra in a single plane with a spatial resolution of  
985  $0.66 \times 0.66 \times 2.0 \text{ cm}^3$ .

986 Turbo spectroscopic imaging was successfully obtained in all 17  
987 patients. The investigators noted that the TSI spectra in one case of  
988 radiation necrosis did not correlate well with the single voxel spectra. The  
989 TSI spectra in general had lower spectroscopic resolution and often  
990 contained lipid signals that were not evident on single voxel spectra. Three  
991 lesions did not demonstrate regions of elevated choline on the TSI images,  
992 which were later histologically confirmed to be brain tumors.

993 All 17 biopsies guided by MRS yielded diagnostic tissues, which  
994 included six glioblastoma multiforme, three anaplastic astrocytoma, three  
995 anaplastic oligodendroglioma, two radiation necrosis, one germinoma, one

996 ganglioglioma, and one astrocytoma. No radiographically or clinically  
997 significant hemorrhage associated with MRS guided brain biopsies using  
998 the trajectory guide was reported among the 17 patients.

999         The authors concluded that “intraoperative MRS-guided brain biopsy  
1000 using a trajectory guide is a simple, safe, and accurate technique for  
1001 accessing areas of the brain of diagnostic interest.” They further  
1002 commented that with the development of intraoperative MRS, it is now  
1003 possible to biopsy lesions located in the brain without the use of rigidly  
1004 fixed head frames (traditional stereotaxy) and in near real-time, thus  
1005 improving the accuracy and diagnostic yield. The use of the trajectory guide  
1006 with MRS may also reduce intracerebral hemorrhage complications by  
1007 minimizing the number of needed passages of the biopsy needle.

1008         While the combination of trajectory guide and intraoperative MRS in  
1009 this study appears promising in achieving high yield in brain biopsies, the  
1010 number of patients studied was small. The need for an intraoperative MRI  
1011 suite limits the generalizability. It should also be noted that three of the four  
1012 authors of this study disclosed a financial interest in the company that  
1013 produces the trajectory guide.

1014         Lin et al. (1999) prospectively evaluated the utility of single voxel  
1015 MRS when used as an alternative or adjunct to brain biopsy in patients with

1016 lesions suggestive of brain tumors initially identified by MRI. This study  
1017 provided information for diagnostic thinking impact (Category- 3) as well as  
1018 for therapeutic choice impact (Category- 4).

1019         Fifteen patients between the ages of seven and 58 (there was only  
1020 one child of age 7) were studied. Among the diagnoses based on histology  
1021 were six anaplastic astrocytoma, one astrocytoma, one oligodendroglioma  
1022 grade II, one oligodendroglioma grade III, one glioblastoma multiforme, and  
1023 one abscess. Three additional patients did not have biopsy and the lesions  
1024 resolved on serial scans. One patient with a history of treated brain stem  
1025 mass subsequently died from progressive disease on follow-up. A  
1026 neurosurgeon defined a treatment plan that would be carried out in the  
1027 absence of a diagnostic MRS study prior to the MRS examination, to  
1028 determine whether MRS directly impacted upon and altered clinical  
1029 decision-making. MRS interpretations were directly incorporated into the  
1030 clinical decision-making and a treatment plan was determined. Patients  
1031 were then followed to determine if subsequent treatment and outcomes  
1032 were in accordance or discordance with the MRS findings.

1033         Single-voxel MRS was performed on a 1.5 Tesla Signa Scanner (GE  
1034 Medical Systems, Milwaukee, WI). The VOI was determined by the  
1035 neurosurgeon based on MRI results prior to the MRS exam. The voxel size

1036 was adjusted to optimize the amount of homogeneous abnormal tissues  
1037 within the voxel, while minimizing the amount of necrotic tissue. Voxel size  
1038 varied between 2.35 to 9.68 cm<sup>3</sup>.

1039         The MRS spectra were quantified with an external standard although  
1040 it was not described. NAA/Cr ratios were consistently and significantly  
1041 elevated in non-neoplastic spectra whereas Cho/Cr demonstrated the  
1042 opposite trend. Lipid and lactate were only observed in abscesses and one-  
1043 half of neoplastic spectra. They could not reliably differentiate necrotic  
1044 tumor from radiation necrosis or abscess. Myoinositol/creatine ratios were  
1045 not significantly different between groups.

1046         Forty-one VOI from 15 patients were analyzed. Thirty-five (85%) of  
1047 the spectra were considered to be of good or excellent quality, four (9%) of  
1048 poor but interpretable quality, and two (4%) non-interpretable. For 10  
1049 patients with previously documented tumors, MRS was interpreted as  
1050 consistent with recurrent tumors in seven cases and consistent with  
1051 radiation necrosis in three cases.

1052         In one patient with two regions of interest on MRI, MRS suggested  
1053 tumor in one lesion, but interpreted another lesion as edematous white  
1054 matter without tumor. Disease progression occurred in the edematous  
1055 white matter lesion 9 months after initial surgery, indicating that MRS was

1056 unsuccessful in identifying infiltrating tumor in this instance. A retrospective  
1057 review of the spectra in that region suggested that the effect of averaging  
1058 over a large volume might have resulted in the misinterpretation. The  
1059 authors suggested that a multi-voxel MRS might have been able to provide  
1060 a more accurate diagnosis.

1061         In the absence of MRS, the neurosurgeon would have recommended  
1062 stereotactic biopsy in eight cases, serial MRI at six week intervals in three  
1063 cases, repeat craniotomy in three cases, and empiric chemotherapy in one  
1064 case. MRS was used in place of biopsy in seven cases, and correlated with  
1065 clinical course in six of these cases. Overall, MRS was found to directly  
1066 alter clinical management in 12 of 15 patients and provided greater support  
1067 for clinical management in 14 of 15 patients. Had MRS been relied upon in  
1068 every case, it might have avoided biopsy in nine cases, and influenced  
1069 clinical management in 13 of 15 patients.

1070         The small number of patients, narrow spectrum of diagnoses, and the  
1071 inclusion of only one neurosurgeon's decision limit the generalizability of  
1072 this study.

1073



1074 **3.4 Category-4: Studies Conducted to Evaluate Therapeutic**

1075 **Choice Impact**

1076 **Prospective studies**

1077 The prospective study by Lin et al. (1999) also provided limited  
1078 information on the use of the test on therapeutic choice impact. See the  
1079 discussion under Category-3 above.

1080

1081 **Retrospective study**

1082 Adamson et al., (1998) conducted a retrospective review of medical  
1083 records to assess the influence of single-voxel MRS findings on the  
1084 treatment of patients suspected of having a brain tumor. This publication  
1085 appears to be based on the same overlapping patient population from the  
1086 Medical College of Wisconsin that had been used in two other Category-2  
1087 publications.

1088 The medical records of 90 patients who had MRS between May and  
1089 December of 1995 were examined. Seventy-eight met the inclusion criteria  
1090 and provided sufficient data for analysis. The patients were categorized into  
1091 two groups based on the interpretation of the MRS findings:

- 1092 • Group 1, MRS findings positive for neoplasm
- 1093 • Group 2, MRS findings negative for neoplasm

1094 The investigators examined all available medical records, including  
1095 discharge summaries, progress notes, and outpatient reports to determine  
1096 the outcome and treatment subsequent to the MRS examination. The  
1097 patients were further categorized on the basis of whether they underwent  
1098 biopsy before treatment. Pathology records in those patients who  
1099 underwent surgical intervention or biopsy were reviewed.

1100 MRS was classified as having a potential positive influence on  
1101 treatment if no biopsy was needed before the initiation of treatment. If MRS  
1102 results did not agree with the subsequent clinical diagnosis, the results  
1103 were considered to have a potential negative influence on patient  
1104 treatment. In all other cases, the effect of MRS was presumed to be  
1105 negligible or indeterminate.

1106 Neuroradiologists interpreted MRS spectra on the basis of the relative  
1107 amplitudes for lactate, lipids, NAA, creatine and phosphocreatine, choline-  
1108 containing compounds, and myo-inositol. A Cho/NAA ratio greater than 1.0  
1109 was considered to be positive for neoplasm. Smaller increases in the  
1110 choline concentration were not considered diagnostic for neoplasm. The  
1111 presence of lactic acid or lipid was consistent with relatively high-grade  
1112 neoplasia if the choline concentration was elevated. Elevation of lactic acid

1113 without elevation of the choline concentration was considered more  
1114 consistent with infarct than with tumor.

1115 MRS was positive for neoplasm in 49 of the 78 patients. In eight of  
1116 these 49 patients, MRS was classified as having a potential positive  
1117 influence. These eight patients received radiation therapy, chemotherapy,  
1118 or both, for a presumed neoplasm without a biopsy to confirm the presence  
1119 of a tumor. MRS was negative for neoplasm in 29 of 78 patients. In 15 of  
1120 these 29 patients, MRS was classified as having a potential positive  
1121 influence.

1122 MRS was classified as having a potential negative influence on  
1123 patient treatment in two of the 49 patients diagnosed as having neoplasm  
1124 by MRS. One of these two patients underwent biopsy, which showed  
1125 inflammatory reaction as probably being secondary to demyelination. The  
1126 other patient underwent surgery and was found to have arteriovenous  
1127 malformation. MRS had no influence on patient treatment in 37 patients  
1128 diagnosed with brain tumor by MRS.

1129 Because of the nature of retrospective medical record review, there  
1130 were several problems with this study. Fourteen of the 78 patients had  
1131 incomplete follow-up information, two from the MRS- diagnosed “tumor”  
1132 group and 12 from the MRS “non-tumor” group. The patients study were

1133 highly selected. The decision to perform MRS was based on CT and MRI  
1134 results in which a neoplasm was considered to be the prime candidate in  
1135 the differential diagnosis.

1136

1137 **3.5 Category- 5: Studies Conducted to Evaluate the Impact of**  
1138 **Test on Health Outcomes**

1139 No study was identified for this category.

1140

1141 **3.6 Category 6: Studies Conducted to Evaluate the Use of Test**  
1142 **on Societal impact**

1143 No study was identified for this category.

1144

1145 The following table summarizes our assessment of the Category-2 and  
1146 above studies described above.

Author	Objective	Sample N/gender/mean age	Design	Assessment of accuracy or usefulness of MRS	Limitations
<b>CATEGORY 2: TEST PERFORMANCE</b>					
<ul style="list-style-type: none"> <li>Differentiating neoplasm from non-neoplasm</li> </ul>					
Rand et al. (1997)	Normal vs. non-normal; neoplasm vs. non-neoplasm	31 ♂ 22 ♀ age=41	Prospective series of patients. with suspected or recurrent neoplasm	Moderate	small sample size
Butzen et al. (2000)	Neoplasm vs. non-neoplasm	99 spectra 31 ♂ 22 ♀ age=41	Logistic regression analysis	Moderate	Only study to use Cho/NAA ratio
McKnight et al. (2002)	Neoplasm vs. non-neoplasm	100 biopsies	Prospective Linear model	Moderate	Unclear enrollment, unblinded, limited generalizability
Kimura et al. (2001)	Neoplasm vs. non-neoplasm	29 ♂ 16 ♀ age 26-75	Retrospective patients with lesions	Moderate	Selection bias, small sample, homogeneous lesions
<ul style="list-style-type: none"> <li>Clinical utility of MRS added to MRI</li> </ul>					
Moller-Hartman et al. (2002)	Neoplasm vs. non-neoplasm	176	Consecutive series of patients with lesions	High	Did not report how reading discrepancies resolved
<ul style="list-style-type: none"> <li>Grading of tumors</li> </ul>					
Roser et al. (1997)	Grading glial tumors	17	Suspected glial tumors	Moderate	Small sample; homogeneity of lesion type
Tedeschi et al. (1997)	Malignant degeneration and recurrence	27	Prospective 3 yr. follow-up of patients w/known tumors	High	Small sample
<ul style="list-style-type: none"> <li>Differentiate intracranial cystic lesions</li> </ul>					
Shukla-Dave et al, (2001)	Differentiating Intracranial cystic lesions	23 ♂ 28 ♀ age=33	Prospective patients w/intracranial lesions dx. by MRI	High	Possible observer bias due to non reporting of method for resolving difference in interpreting spectra; sample size?

1147

Category	Author	Objective	Sample	Design	Assessment of accuracy or usefulness of MRS	Limitations
<b>CATEGORY 3: DIAGNOSTIC THINKING IMPACT</b>						
	Hall et al. (2001)	Utility of MRS for targeting biopsies	13 ♂ 4 ♀ age 16-80	Prospective patients w/suspected tumors	High	Small sample; need for intra-operative MRI suite
	Lin et al. (1999) (also Category-4)	Supporting brain biopsy for MRI-identified lesions	15 Age 7-58	Prospective	High	Small sample, homogeneous group of diagnoses, limited observer verification
<b>CATEGORY 4. THERAPEUTIC CHOICE IMPACT</b>						
	Adamson et al. (1998)	Evaluation of impact of MRS on biopsy decision	90 initial; 78 final	Retrospective patients w/suspected neoplasms dx. By CT or MRI See Rand et al.; same data.	Low	Retrospective, losses to follow-up; medical record reviews
	Lin et al. (1999) (also Category-3)	Supporting brain biopsy for MRI-identified lesions; some patients were treated based on MRI findings	15 Age 7-58	Prospective	High	Small sample, homogeneous group of diagnoses, limited observer verification

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#### 4. RESULTS: Abstracts

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As described above, abstracts and proceedings from following professional societies for the years 2001 and 2002 were reviewed:

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- ASNR-American Society of Neuroradiology
- RSNA-Radiological Society of North American
- ISMRM-International Society for Magnetic Resonance in Medicine

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Because these were abstracts and not full papers, data on basic study design information such as patient gender and means of enrolling patients were frequently unavailable. Of the 241 proceedings-generated abstracts reviewed, 44 were provided information beyond the technical feasibility category. The following table summarizes the distribution of abstracts by category:

CATE-GORY	DESCRIPTION	(#/%)
1	Technical feasibility and optimization	44
2	Diagnostic accuracy	8*
3	Diagnostic thinking impact	1
4	Therapeutic choice impact	0
5	Patient outcome impact	0
6	Societal impact	0

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\*One study shown in this category could also be considered a Category-3 study.

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#### **4.1 Category-1 Abstracts: Technical Feasibility**

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Evidence Table 2 shows selected characteristics of the 44 technical feasibility (Category 1) abstracts. Similar to Evidence Table 1 containing technical feasibility studies, it summarizes: year of publication, country in which the research was conducted, study characteristics including number of diseased (cases) and non-diseased (control) patients, method of patient enrollment, diagnostic status, and age. The table also shows the size of the volume of tissue (voxel) of interest as well as whether single or multiple voxel sampling was used. Finally, the table indicates the principal clinical study objectives: tumor differentiation, tumor grading, distinguishing primary tumor tissue from recurrent tumor and from metastases, and identifying necrotic tissue. In addition, there were two instances where there were duplicate abstracts for the same studies from different proceedings.

There were forty-seven abstracts reviewed for Category 1 from 3 different proceedings for 2001 and 2002. Forty-four unique studies remained after removing four duplicate studies. In addition, there were a minimum of four instances of overlapping population represented in the abstracts. The abstracts reported on 1,445 patients. One study reported on



1189 174 diagnostic 'studies' without mentioning the number of patients and one  
1190 reported the results of 14 'studies'. Twenty studies (42.5%) were from the  
1191 US. The ages of patients described in eight of the abstracts varied  
1192 considerably; ranging was from 8 to 84 years. As in the complete studies  
1193 reviewed, we excluded abstracts that were predominantly pediatric.

1194 Five studies were reported as prospective and five were  
1195 retrospective. The remaining abstracts reported no data on study design.  
1196 The largest sample reported in an abstract was 130 patients. Most  
1197 abstracts did not include controls. Single voxel and multiple voxel sampling  
1198 were used approximately equally. In six studies no voxel data were  
1199 reported and in four a combination of both approaches were employed.

1200 Tumor differentiation (14 studies) and grading (10 studies) were the  
1201 most frequently cited clinical objectives. Other clinical objectives varied  
1202 widely such as characterization of metabolite ratios (six abstracts),  
1203 prognosis (two abstracts), measure of lipid levels (two abstracts), and  
1204 tumor response to treatment (two abstracts).

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## 1207 **4.2 Category-2: Studies that Evaluate Test Performance**

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1209

The proceedings abstracts described eight studies in this category.

1210 Studies in this category could be further grouped into studies with the main

1211 purpose of differentiating tumors from non-tumors, grading of tumors,  
1212 differentiating intracranial cystic lesions, and to assess the incremental  
1213 value of MRS added to MRI.

1214

#### 1215 **4.2.1 Abstracts of Category-2 Studies Differentiating Neoplasm** 1216 **from Non-neoplasm**

1217

1218 Yin et al. (2002) evaluated 40 lesions in 35 patients with suspected  
1219 brain neoplasms or recurrent neoplasm. The purpose of this study was to  
1220 measure the accuracy of multivoxel 3D MRS proton MRS in distinguishing  
1221 neoplastic from non-neoplastic brain lesions (blinded vs. unblinded). Final  
1222 diagnoses were assessed by clinical examination, biopsy and serial MRI.

1223 The specificity for distinguishing between neoplastic and non-  
1224 neoplastic lesions was 88.6%. Of the 35 cases, 21 had neoplasms and 19  
1225 had non-neoplastic lesions. Of 16 glioma, 14 were correctly identified  
1226 through increased Cho and decreased NAA for the gliomas. The metabolic  
1227 profiles of the following types of tissue were studied: abscess (increased  
1228 Lac), metastasis (increased Cho and Lac and no NAA peak), demyelinating  
1229 lesion (decreased NAA and normal Cho), lymphoma (high Cho and lipids),  
1230 and necrosis (high Cho and decreased metabolism). There was also little  
1231 diversity of lesions, no information about patient ages, no statistical

1232 analysis, and no comparative data. The study did, however, report a form  
1233 of blinding, but no detail was provided.

1234 Herminghaus et al. (2002a) evaluated 293 consecutive patients  
1235 diagnosed with focal brain lesions. The purpose of this study was to  
1236 assess the potential of single voxel MRS (1.5 T Siemens Magnetom Vision)  
1237 to differentiate between neoplastic and non-neoplastic lesions, between  
1238 high grade tumors and metastases or lymphomas, and between different  
1239 types of tumors. The authors studied 25 types of lesions.

1240 Discriminant analysis was used to “confirm significance” of  
1241 differences between clusters formed by the authors. The analysis yielded  
1242 five clusters: one containing glioblastoma (unknown grade), gliosarcoma,  
1243 and embryonal tumors (IV WHO). A second cluster included anaplastic  
1244 astrocytomas, anaplastic oligoastrocytomas, anaplastic  
1245 oligodendrogliomas, anaplastic meningeoma (WHO III), and lymphomas.  
1246 The third cluster included glial low grade tumors, gangliogliomas,  
1247 gangliocytomas, neurominomas, and glioses and abscesses. The fourth  
1248 cluster contained tumor necrosis, tumor cysts, infectious cysts, and  
1249 meningeomas. The fifth cluster contained metastasis, glioblastoma,  
1250 gliosarcoma, and embryonal tumor grade IV WHO. The authors concluded  
1251 that MRS can be helpful in differentiating:

1252

- 1253 • Low grade from high grade tumors
- 1254 • Metastasis and lymphomas from benign or low grade tumors
- 1255 • Abscesses from glioblastoma and metastasis
- 1256 • Silent infarct from low grade tumors
- 1257 • Tumor cysts, infectious cysts, and necrotic tissue from each other and
- 1258 from other lesions
- 1259 • WHO I/II meningiomas from metastasis

1260

1261 The authors concluded MRS could not distinguish:

- 1262 • Between different tumor types of the same grade.
- 1263 • Lymphomas from grade III tumors
- 1264 • Metastasis from glioblastoma
- 1265 • Low grade brain tumors from gliosis

1266

1267 “Success rates” were reported for the above classifications, but the  
1268 level of detail provided in the abstract is insufficient for meaningful  
1269 interpretation of these statistics. Finally, the fact that this study did not  
1270 describe the standard against which the focal brain tumors were  
1271 diagnosed, makes its difficult to interpret its conclusions.

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#### **4.2.2. Abstracts of Category-2 Studies Detecting Tumor**

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##### **Recurrence**

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Kovanlikaya et al. (2002) prospectively examined 16 lesions in seven

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men and seven women (mean age 50 yrs) to determine the value of multi-

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voxel MRS (1.5 T; 1 cm<sup>3</sup> spatial resolution) of glial neoplasms in detecting

1278

tumor recurrence after treatment with surgical excision, radiotherapy, and

1279

chemotherapy. The neoplasms included 12 astrocytomas, one

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oligodendroglioma and three mixed tumors of Grade II (5), Grade III (5) and

1281

Grade IV (6). Voxels showing the highest choline levels were analyzed for

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levels of NAA, creatine and lactate/lipid values and compared to the

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matched contralateral normal side of the brain. The results were assessed

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pathologically (6 lesions) and clinically (10 lesions).

1285

Tumor recurrence was observed in eight of the 14 patients. Choline

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levels were much higher (114% elevation) in the recurrent lesions, with

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much lower levels in stable patients (7% depression). Choline elevation

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had a high sensitivity for detecting tumor recurrence (100%; positive

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predictive value = 82%). The specificity of choline depression for detecting

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stability was 72% (negative predictive value = 100%.) The authors, despite

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the small numbers, also suggested that the lactate/lipid peak in three

1292 patients was highly specific for detecting necrosis but not sensitive for  
1293 detecting recurrence. There was no independent verification of the results.

1294 Lefkowitz et al. (2002) prospectively examined 27 lesions in 22  
1295 patients whose brain tumors had been surgically excised and/or irradiated  
1296 to evaluate MRS' usefulness for diagnosing recurrent neoplasms. Single  
1297 and multivoxel MRS was used to obtain maps of NAA and Cho  
1298 concentration, ratio maps of Cho/Cr peak areas and heights, and tables of  
1299 Cho/Cr ratios to identify potential tumor-containing voxels. A Cho/Cr ratio  
1300 greater than or equal to 2.0, behavior of control voxels, and other spectral  
1301 features were considered for tumor/non-tumor designations. Biopsy or  
1302 follow-up imaging was used to confirm tumor status.

1303 For the 27 MRS results, there were 19 gliomas, five metastases, two  
1304 lymphomas, and one medulloblastoma. Sensitivity for detecting tumor  
1305 recurrence was 89% (positive predictive value = 73%). Specificity was 33%  
1306 (negative predictive value = 60%). Overall accuracy was 70%. Tests of  
1307 statistical significance and confidence intervals were not reported. There  
1308 was no independent verification of results.

1309 Shah et al. (2002) assessed how well MRS performed in identifying  
1310 tumor recurrence compared to SPECT and CT/MRI. These authors studied  
1311 nine patients who had undergone surgery and radiotherapy or radiotherapy

1312 alone for an average of 28 months with tumors suspected of recurrence.  
1313 The tumors comprised: oligodendroglioma II (two); oligodendroglioma III  
1314 (one); anaplastic astrocytoma (two); malignant mixed glioma (one);  
1315 astrocytoma II (two); and glioblastoma multiforme (one). Choline spectra  
1316 derived from MRS (1.5 T Siemens) sequence voxels ranging from 1.3 ml to  
1317 3.8 ml were used as markers for recurrence and were compared with  
1318 radiological and SPECT results.

1319         The kappa (k) measure of agreement was calculated between MRS  
1320 and each of the other two tests. The results were: MRS vs. SPECT  
1321 (k=0.72), MRS vs. CT/MRI (k=0.57) and CT/MRI vs. SPECT (k=0.37).  
1322 There was no biopsy confirmation of tumor recurrence and therefore no  
1323 'reference standard'. In addition, the sample size was small, and no tests of  
1324 statistical significance or confidence intervals were reported.

1325         Lichy et al. (2002) examined the value of MRS, FDG-PET, and IMT-  
1326 SPECT in evaluating suspicious brain lesions detected by MRI follow-up of  
1327 24 patients with irradiated gliomas. Multivoxel 2D MRS (1.5 T; voxel size =  
1328 8.8 x 8.8 x15 mm<sup>3</sup>) was used to obtain relative signal intensity ratios of  
1329 Cho, Cr, and NAA. Eighty-six voxels from suspicious lesions and 147 from  
1330 'normal' areas were analyzed. Clinical and MRI/CT follow-up, not biopsy,  
1331 was used to classify lesions as neoplastic or non-neoplastic.

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This study reported that the true positive rate (it is assumed that surgery was the standard of comparison) for identifying neoplastic tissue was 88% for MRS, 73% for FDG-PET, and 100% for IMT-SPECT. The true positive rate for identifying non-neoplastic tissue was 89% for MRS, 100% for FDG-PET and 75% for IMT-SPECT. Cho and Cho/NAA were present in significantly higher levels in neoplastic tissue. Additional information about sensitivity and specificity were reported, but the performance outcomes being evaluated were unclear. In this study three diagnostic techniques were compared only to each other and not to either biopsy or surgical results. In addition, there was no independent verification of results, and no confidence intervals for diagnostic test performance were reported.

### **4.2.3 Abstracts Of Category-2 Studies Distinguishing Homogeneity, Proliferation, And Grade Of Lesions**

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Herminghaus et al. (2001a) prior to biopsy evaluated 29 consecutive patients with MRI results and history suggestive of neuroepithelial brain tumors. The purpose of the study was to evaluate MRI's ability to distinguish low from high-grade tumors. Single voxel MRS (1.5 T) was



1352 used to evaluate tumor tissues as well as normal appearing brain tissue in  
1353 the contralateral hemisphere. NAA, total creatine, Cho, Lip, and Lac were  
1354 analyzed. Tumor spectroscopic data were classified (“observer-  
1355 independently”) as grade I/II or III/IV according to the World Health  
1356 Organization system. Biopsies were performed and confirmed by following  
1357 patients for three years. Tumors showing at least 6 months of stability were  
1358 defined as low-grade; those tumors showing progression were classified as  
1359 high-grade.

1360 While the authors reported sensitivity (100%), specificity (86%), and  
1361 overall accuracy (96%), it is not clear what the reference standard was.  
1362 Since the authors also report sensitivity (95%), specificity (86%), and  
1363 overall accuracy (93%) for biopsy, it may be inferred that biopsy was not  
1364 the reference standard. It is possible that surgery was the reference  
1365 standard, but the study does not mention whether or how frequently  
1366 surgery was performed. This ambiguity makes it difficult to assess the  
1367 meaning of these findings. In addition, there was no independent  
1368 verification of results. (This study might also be classified as Category 3).

1369

1370           **4.3.1 Abstracts of Category-3: Studies Conducted to Evaluate**  
1371           **Diagnostic Thinking Impact**

1372           Mao et al., (2002) evaluated the utility of single voxel MRS (1.5 T  
1373 Phillips NT scanner) to guide selection of biopsy target areas in eight  
1374 patients with a previous biopsy yielding equivocal results. This study might  
1375 be considered as providing information for thinking about diagnostic impact.  
1376 Areas of decreased NAA and elevated Cho and Lac were identified so that  
1377 NAA and Cho maps could be used to target these areas as potential biopsy  
1378 sites. The maps were superimposed on the stereotactic anatomical image  
1379 to develop coordinates for the sites. Biopsies were then performed,  
1380 followed by either CT or MRI.

1381           MRS results showed abnormal metabolite maps for all eight patients,  
1382 with seven showing decreased NAA and increased CHO. Biopsy sites were  
1383 chosen from areas showing the most elevated CHO levels, and the  
1384 biopsies were positive for seven of the eight patients. Tumor types  
1385 included: two anaplastic astrocytomas (III); glioblastoma multiforme (IV);  
1386 two infiltrative astrocytomas (II); oligodendroglioma (II).

1387  
1388           While the study described in this abstract shows the technical  
1389 feasibility of using MRI to help select the site of biopsy, the sample size of

1390 eight was small, with no statistical analysis (it mentions a 'significant'  
1391 decrease in NAA and increased CHO, but no quantitative data to support  
1392 this is presented in the abstract). In addition, there was no comparison  
1393 group of patients with non-MRS guided biopsy and there was no  
1394 independent verification of the results.

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1397 **5. SUMMARY**

1398                   Ninety-six articles met our inclusion criteria for evaluation, with

1399 11 providing information beyond the level of technical feasibility. Eight

1400 articles evaluated the test performance of MRS in various settings. Three

1401 articles addressed the impact of MRS on diagnostic thinking and

1402 therapeutic decision making. No article was found that addressed

1403 improvement of patient outcome.

1404

1405                   **5.1 For what metabolite profiles does MRS provide equivalent,**  
1406                   **complementary, or more accurate diagnostic information?**

1407                   The following table summarizes the peak intensities and ratios of

1408 metabolites evaluated in Category-2 and higher studies.

1409

1410 Category 2 and higher studies that reported metabolite profiles

Study	Category	Qualitative interpretation	Quantitative measurements															
			Individual metabolites								Ratios							
			Cho	Cr	NAA	Lac	Lip	GI or MI	MGG	Cho/Cr	NAA/Cr	Cho/NAA	NAA/Cho	Lac/Cr	Lip/Cr	Cho/(Lip or Lac)	GI/Cr or MI/Cr	MGG/Cr
Rand	2	x																
Butzen	2	x	x	x	x	x	x					x						
Shukla-Dave	2	x																
Kimura	2		x	x	x	x	x			x	x			x	x	x		
Moller-Hartmann	2		x	x	x	x	x			x	x							
Tedeschi	2		x	x	x	x				x	x		x					
Roser	2		x	x	x		x	x	x	x	x				x		x	x
Lin (1999)	3,4		x	x	x	x	x	x		x	x						x	

1411

1412 These profiles represent a very heterogeneous mix of signals and  
 1413 ratios, study populations, study purpose, and results. Some of the signals  
 1414 and ratios were unique for a particular study. For example, Butzen et al.  
 1415 used a Cho/NAA ratio of greater than 1.0 to classify lesions as tumors for  
 1416 initial diagnosis and reported a sensitivity of 79% and specificity of 77%. No  
 1417 other study used this metabolite ratio; therefore their results could not be

1418 verified. The most common ratios evaluated were Cho/Cr and NAA/Cr,  
1419 which were reported in five studies. With so little data and many questions,  
1420 the above question could be answered only to a very limited extent.

1421           Cho/Cr is the only metabolite ratio that has been found to be useful  
1422 in differentiating neoplasm and non-neoplasm and supported by several  
1423 studies. Among all the full articles examined in this technology assessment,  
1424 Moller-Hartmann et al. provided the most complete reporting of the  
1425 metabolite signal intensities and ratios for each type of tumor found in their  
1426 study population. However, no single metabolite or ratio, other than  
1427 perhaps a very high Cho/Cr ratio to diagnose PNET, by itself could  
1428 differentiate among different neoplasms, among different tumor grades, or  
1429 between neoplastic and non-neoplastic lesions. A moderately high Cho/Cr  
1430 ratio of approximately four was observed for astrocytoma grade IV and  
1431 metastases, compared to a value of approximately 1.5 for cerebral  
1432 infarctions and abscesses. Kimura et al. also reported that a Cho/Cr ratio of  
1433 2.48 minimized the rate of misdiagnosis of neoplasm and non-neoplasm.  
1434 Lin et al. reported that the Cho/Cr ratio was the single most accurate  
1435 spectral measurement for differentiating neoplastic from non-neoplastic  
1436 lesions. Unfortunately, the results were presented only as a bar graph.

1437 In the only study that addressed the incremental diagnostic yield,  
1438 Moller-Hartmann et al. demonstrated that MRS added to conventional MRI  
1439 improved the number of correct diagnoses and reduced the number of  
1440 incorrect or equivocal diagnoses.

1441  
1442 **5.2 Does The Use Of MRS Lead To An Improved Net Health**  
1443 **Outcome?**

1444  
1445 Three studies addressed the potential impact of MRS results on  
1446 diagnostic thinking or therapeutic decision making. Conclusions that can be  
1447 drawn from these studies are severely limited due to the fact that the two  
1448 prospective studies had only 15 and 17 patients, respectively, and the only  
1449 large study was a retrospective analysis of medical records to identify  
1450 potential opportunities for MRS to influence diagnostic thinking.

1451  
1452 **5.3 Are Voxel Positions And Operator Error Important Factors In**  
1453 **Obtaining Diagnostic Images? If So, How Do They Impact MRS**  
1454 **Accuracy?**

1455 No study explicitly evaluated the impact of voxel position on the  
1456 accuracy of MRS. The retrospective study by Kimura et al. came closest to  
1457 this objective. This study evaluated the differences of measurements  
1458 between the whole lesion and the inner region of the same tumor.

1459 Significant differences between the inner region and the whole lesion were  
1460 found for various types of lesions. Although not specifically reported, the  
1461 voxel sizes of the inner regions obviously were smaller than those of the  
1462 whole lesions.

1463 No study commented on the potential impact of operator error in  
1464 placement of the voxel.

1465

#### 1466 **5.4 Strengths And Weaknesses Of The Studies**

1467 Most of the studies on Proton MRS were Category- 1 studies that  
1468 addressed technical feasibility. The stated purpose of some of the studies  
1469 classified as technical feasibility studies was to examine the impact of MRS  
1470 on practice, but limitations of these studies' designs kept them from  
1471 meeting the criteria necessary to achieve that level. Most of the studies we  
1472 evaluated in categories 2 to 4 concluded that MRS has value for the  
1473 indications studied. One study (Rand et al. 1997), which measured the  
1474 accuracy of single-voxel, image-guided proton MRS in distinguishing  
1475 normal from abnormal brain tissue and neoplastic from non-neoplastic  
1476 brain disease, was an excellent example in some respects of the type of  
1477 study needed to assess diagnostic efficacy. The use of multiple blinded  
1478 readers and ROC analyses should be encouraged. Detailed presentation of



1479 quantified spectra intensities and ratios similar to those reported in the  
1480 article by Moller-Hartmann et al. would help the interpretation of results  
1481 across studies.

1482         Sample size is also an important limitation. Sample sizes that might  
1483 be adequate for investigating one type of tumor are not necessarily  
1484 adequate for investigating multiple types of tumors in the same study. This  
1485 applies to tumor grades as well.

1486         In summary, while there are a large number of studies that confirm  
1487 MRS' technical feasibility, there are very few published studies to evaluate  
1488 the diagnostic accuracy and whether it can positively affect diagnostic  
1489 thinking and therapeutic choice. Those studies that do address these areas  
1490 often have significant design flaws including inadequate sample size,  
1491 retrospective design and other limitations that could bias the results.

1492

## 1493         **5.5 Implications for future research**

1494         The relative rarity of brain tumors, the relatively low installed base of  
1495 MRS software and the constraints of clinical practice have precluded the  
1496 establishment of large, double-blinded controlled trials that would go  
1497 beyond exploring technical feasibility. Experience with MRS has only  
1498 become available to the general community of radiologists within the past

1499 five years. Prior to this time, commercial software for shimming and  
1500 analyzing spectra was not reliable, except in the hands of trained  
1501 specialists. The current commercial software is vastly improved and can be  
1502 mastered with a reasonable amount of additional training. Prior to about  
1503 1995, MRS was available at only a few research-oriented institutions.  
1504 Hence studies were typically single institution feasibility studies or small  
1505 case series. The recent change in the availability of MRS is only now  
1506 reaching enough centers to allow more advanced investigations using the  
1507 technique. MRS is still not available in many community hospitals, and  
1508 even some academic centers.

1509         The reason that the research is not more advanced may be that in  
1510 addition to the relatively recent availability of MRS, its use in brain tumor  
1511 evaluation evolved by using techniques that were not straightforward.  
1512 Initially, it was hoped that tumors would have a characteristic “signature”  
1513 that would allow rapid MRS diagnoses. Because the sensitivity of MRS  
1514 allows demonstration of only a limited set of chemical compounds in the  
1515 brain, such signatures have not been found. However, means of using the  
1516 chemical information that is provided by MRS for tumor evaluation has  
1517 progressed as new ideas have evolved for effective use of this information.

1518

## 6. CONCLUSION

Human studies conducted on the use of MRS for brain tumors demonstrate that this non-invasive method is technically feasible and suggest potential benefits for some of the proposed indications. There is a paucity of high quality direct evidence demonstrating the impact on diagnostic thinking and therapeutic decision making. In addition, the techniques of acquiring the MRS spectra and interpreting the results are not well standardized. The table below summarizes the current state of evidence.

CATEGORY	DESCRIPTION	EVIDENCE SUMMARY
1	Technical feasibility and optimization	Large amount of evidence
2	Diagnostic accuracy	
	Distinguish neoplasm from non-neoplasm	Limited evidence
	MRS added to MRI	Limited evidence
	Tumor grading	Limited evidence
	Differentiate intracranial cystic lesions	Limited evidence
3	Diagnostic thinking impact	Limited evidence
4	Therapeutic choice impact	Limited evidence
5	Patient outcome impact	No evidence
6	Societal impact	No evidence

1531  
1532

## APPENDIX A: ANALYTIC FRAMEWORK: POTENTIAL USES OF MRS

<i>Newly Diagnosed Space-Occupying Brain Mass* Identified By CT or MRI</i>	<i>Follow-Up Of Patients with Previously Diagnosed Brain Tumor Undergoing Treatment</i>
<b>Potential use of MRS in diagnostic evaluation and prognostication</b>	
<ul style="list-style-type: none"> <li>• Replacement of diagnostic biopsy by MRS               <ul style="list-style-type: none"> <li>◦ <i>Outcome measure: same or improved accuracy/less invasiveness</i></li> </ul> </li> <li>• Differentiating masses               <ul style="list-style-type: none"> <li>• Distinguishing malignant neoplasms from non-malignant neoplasms and vascular lesions (e.g. ring-enhancing primary tumors from abscesses)                   <ul style="list-style-type: none"> <li>• Distinguishing single metastatic lesions such as gliomas from primary tumors</li> <li>• Distinguishing among types of neoplasm (e.g. PNET from astrocytoma or neurofibroma bright spots from astroglial tumors)</li> </ul> </li> <li>• <i>Outcome measure: Higher sensitivity and specificity in differentiating masses</i></li> </ul> </li> <li>• MRS-guided biopsy to improve biopsy yield               <ul style="list-style-type: none"> <li>• <i>Outcome measure: Success rate of MRS-guided biopsies</i></li> </ul> </li> <li>• Tumor grading: degree of malignancy               <ul style="list-style-type: none"> <li>• <i>Outcome measure: % of inappropriate biopsies avoided; biopsy yield</i></li> </ul> </li> </ul>	<ul style="list-style-type: none"> <li>• Determining whether tumor has recurred</li> <li>• Differentiate recurrence from radiation injury (necrosis)</li> <li>• <i>Outcome measure: Higher sensitivity and specificity in differentiating masses</i></li> <li>• MRS-guided biopsy to improve biopsy yield</li> <li>• <i>Outcome measure: Success rate of MRS-guided biopsies</i></li> </ul>
<b>Potential use of MRS in patient management</b>	
<ul style="list-style-type: none"> <li>• Planning treatment               <ul style="list-style-type: none"> <li>◦ Choosing among therapies</li> <li>◦ Identifying tumor margin and volume for radiosurgery planning/surgical resection</li> <li>◦ Identifying tumor margin and volume for radiotherapy (gamma knife therapy) planning</li> <li>◦ Identifying target volume (isolating most active portions of tumor) for radiosurgery</li> </ul> </li> </ul>	<ul style="list-style-type: none"> <li>• Re-initiating radiosurgery when recurrence differentiated from necrosis</li> <li>• Rapidly assessing treatment effectiveness to optimize treatment               <ul style="list-style-type: none"> <li>◦ Monitor response to treatment</li> </ul> </li> <li>• <i>Outcome measures: survival, quality of life</i></li> </ul>

<i>Newly Diagnosed Space-Occupying Brain Mass* Identified By CT or MRI</i>	<i>Follow-Up Of Patients with Previously Diagnosed Brain Tumor Undergoing Treatment</i>
<ul style="list-style-type: none"> <li>planning <ul style="list-style-type: none"> <li>○ Tumor grading: timing interventions</li> </ul> </li> <li>• <i>Outcome measures: survival, quality of life</i></li> </ul>	
<b>Factors potentially affecting MRS performance</b>	
<ul style="list-style-type: none"> <li>• Lesion location (e.g. proximity to bone and sinuses) and voxel positions</li> <li>• Concurrent disease (suspicion of known Ca elsewhere, e.g. lung, breast); suspicion of HIV</li> <li>• Operator error</li> <li>• Machine used/software and equation version</li> </ul>	<ul style="list-style-type: none"> <li>• Lesion location (e.g. proximity to bone and sinuses) and voxel positions</li> <li>• Concurrent disease (suspicion of known Ca elsewhere, e.g. lung, breast); suspicion of HIV</li> <li>• Operator error</li> <li>• Machine used/software and equation version</li> </ul>

1533

## APPENDIX B: Glossary

1534

1535 **Cho** – choline

1536 **cm<sup>3</sup>** – cubic centimeter

1537 **Cr** – creatine and phosphocreatine

1538 **CT** – computed tomography

1539 **GI** – glycine

1540 **Lac** – lactate

1541 **Lip** – lipid

1542 **MGG** – macromolecules, glutamine, and glutamate

1543 **MI** – myo-inositol

1544 **MR** – magnetic resonance

1545 **MRI** – magnetic resonance imaging

1546 **MRS** – magnetic resonance spectroscopy

1547 **NAA** – N-acetyl-aspartate

1548 **ODV** – orthonormal discriminant vector

1549 **PET** – positron emission tomography

1550 **PNET** – peripheral neuroectodermal tumor

1551 **ROC** – receiver operating characteristic

1552 **VOI** – volume of interest

1553 **Tesla** – unit of magnetic flux

## References

Adams, E. Evaluating diagnostic tests: a guide to the literature. Technology Assessment Program, Management Decision and Research Center, Veterans Administration Health Services Research and Development Service December, (4) 1997.

Adamson AJ, Rand SD, Prost RW, Kim TA, Schultz C, Haughton VM. Focal brain lesions: effect of single-voxel proton MR spectroscopic findings on treatment decisions. *Radiology* 1998; 209(1):73-78.

Alger JR, Frank JA, Bizzi A, Fulham MJ, DeSouza BX, Duhaney MO et al. Metabolism of human gliomas: assessment with H-1 MR spectroscopy and F-18 fluorodeoxyglucose PET. *Radiology* 1990; 177(3):633-641.

Barba I, Moreno A, Martinez-Perez I, Tate AR, Cabanas ME, Baquero M et al. Magnetic resonance spectroscopy of brain hemangiopericytomas: high myoinositol concentrations and discrimination from meningiomas. *Journal of Neurosurgery* 2001; 94(1):55-60.

Barbarella G, Ricci R, Pirini G, Tugnoli V, Tosi MR, Bertoluzza A et al. In vivo single voxel 1H MRS of glial brain tumors: correlation with tissue histology and in vitro MRS. *International Journal of Oncology* 1998; 12(2):461-468.

Bruhn H, Frahm J, Gyngell ML, Merboldt KD, Hanicke W, Sauter R et al. Noninvasive differentiation of tumors with use of localized H-1 MR spectroscopy in vivo: initial experience in patients with cerebral tumors. *Radiology* 1989; 172(2):541-548.

Burtscher IM, Skagerberg G, Geijer B, Englund E, Stahlberg F, Holtas S. Proton MR spectroscopy and preoperative diagnostic accuracy: an evaluation of intracranial mass lesions characterized by stereotactic biopsy findings. *AJNR: American Journal of Neuroradiology* 2000; 21(1):84-93.

Butzen J, Prost R, Chetty V, Donahue K, Neppi R, Bowen W et al. Discrimination between neoplastic and nonneoplastic brain lesions by use of proton MR spectroscopy: the limits of accuracy with a logistic regression model. *AJNR: American Journal of Neuroradiology* 2000; 21(7):1213-1219.

Castillo M, Smith JK, Kwock L. Correlation of myo-inositol levels and grading of cerebral astrocytomas. *AJNR: American Journal of Neuroradiology* 2000; 21(9):1645-1649.

Chang KH, Song IC, Kim SH, Han MH, Kim HD, Seong SO et al. In vivo single-voxel proton MR spectroscopy in intracranial cystic masses. *AJNR: American Journal of Neuroradiology* 1998; 19(3):401-405.

Chumas P, Condon B, Oluoch-Olunya D, Griffiths S, Hadley D, Teasdale G. Early changes in peritumorous oedema and contralateral white matter after dexamethasone: a study using proton magnetic resonance spectroscopy. *Journal of Neurology, Neurosurgery & Psychiatry* 1997; 62(6):590-595.

Croteau D, Scarpace L, Hearshen D, Gutierrez J, Fisher JL, Rock JP et al. Correlation between magnetic resonance spectroscopy imaging and image-guided biopsies: semiquantitative and qualitative histopathological analyses of patients with untreated glioma. *Neurosurgery* 2001; 49(4):823-829.

Demaerel P, Johannik K, Van Hecke P, Van Ongeval C, Verellen S, Marchal G et al. Localized <sup>1</sup>H NMR spectroscopy in fifty cases of newly diagnosed intracranial tumors. *Journal of Computer Assisted Tomography* 1991; 15(1):67-76.

Domingo Z, Rowe G, Blamire AM, Cadoux-Hudson TA. Role of ischaemia in the genesis of oedema surrounding meningiomas assessed using magnetic resonance imaging and spectroscopy. *British Journal of Neurosurgery* 1998; 12(5):414-418.

Dowling C, Bollen AW, Noworolski SM, McDermott MW, Barbaro NM, Day MR et al. Preoperative proton MR spectroscopic imaging of brain



tumors: correlation with histopathologic analysis of resection specimens. *AJNR: American Journal of Neuroradiology* 2001; 22(4):604-612.

Esteve F, Rubin C, Grand S, Kolodie H, Le Bas JF. Transient metabolic changes observed with proton MR spectroscopy in normal human brain after radiation therapy. *International Journal of Radiation Oncology, Biology, Physics* 1998; 40(2):279-286.

Falini A, Calabrese G, Origgi D, Lipari S, Triulzi F, Losa M et al. Proton magnetic resonance spectroscopy and intracranial tumours: clinical perspectives. *Journal of Neurology* 1996; 243(10):706-714.

Fineberg HV, Bauman R, Sosman M. Computerized cranial tomography. Effect on diagnostic and therapeutic plans. *JAMA* 1977 Jul 18;238(3):224-7.

Fryback DG, Thornbury JR. The efficacy of diagnostic imaging. *Med Decis Making* 1991 Apr-Jun;11(2):88-94.

Fountas KN, Kapsalaki EZ, Gotsis SD, Kapsalakis JZ, Smisson HF, III, Johnston KW et al. In vivo proton magnetic resonance spectroscopy of brain tumors. *Stereotactic & Functional Neurosurgery* 2000; 74(2):83-94.

Frahm J, Bruhn H, Hanicke W, Merboldt KD, Mursch K, Markakis E. Localized proton NMR spectroscopy of brain tumors using short-echo time STEAM sequences. *Journal of Computer Assisted Tomography* 1991; 15(6):915-922.

Fulham MJ, Bizzi A, Dietz MJ, Shih HH, Raman R, Sobering GS et al. Mapping of brain tumor metabolites with proton MR spectroscopic imaging: clinical relevance. *Radiology* 1992; 185(3):675-686.

Furuya S, Naruse S, Ide M, Morishita H, Kizu O, Ueda S et al. Evaluation of metabolic heterogeneity in brain tumors using <sup>1</sup>H-chemical shift imaging method. *NMR in Biomedicine* 1997; 10(1):25-30.

Galanaud D, Chinot O, Nicoli F, Confort-Gouny S, Le Fur Y, Barrie-Attarian M et al. Use of proton magnetic resonance spectroscopy of the brain to differentiate gliomatosis cerebri from low-grade glioma. *Journal of Neurosurgery* 2003; 98(2):269-276.

Go KG, Kamman RL, Mooyaart EL, Heesters MA, Pruijm J, Vaalburg W et al. Localised proton spectroscopy and spectroscopic imaging in cerebral gliomas, with comparison to positron emission tomography. *Neuroradiology* 1995; 37(3):198-206.

Go KG, Krikke AP, Kamman RL, Heesters MA. The origin of lactate in peritumoral edema as measured by proton-magnetic resonance spectroscopic imaging. *Acta Neurochirurgica - Supplementum* 1997; 70:173-175.

Gotsis ED, Fountas K, Kapsalaki E, Toulas P, Peristeris G, Papadakis N. In vivo proton MR spectroscopy: the diagnostic possibilities of lipid resonances in brain tumors. *Anticancer Research* 1996; 16(3B):1565-1567.

Graves EE, Nelson SJ, Vigneron DB, Chin C, Verhey L, McDermott M et al. A preliminary study of the prognostic value of proton magnetic resonance spectroscopic imaging in gamma knife radiosurgery of recurrent malignant gliomas. *Neurosurgery* 2000; 46(2):319-326.

Graves EE, Nelson SJ, Vigneron DB, Verhey L, McDermott M, Larson D et al. Serial proton MR spectroscopic imaging of recurrent malignant gliomas after gamma knife radiosurgery. *AJNR: American Journal of Neuroradiology* 2001; 22(4):613-624.

Gupta RK, Cloughesy TF, Sinha U, Garakian J, Lazareff J, Rubino G et al. Relationships between choline magnetic resonance spectroscopy, apparent diffusion coefficient and quantitative histopathology in human glioma. *Journal of Neuro-Oncology* 2000; 50(3):215-226.

Gupta RK, Sinha U, Cloughesy TF, Alger JR. Inverse correlation between choline magnetic resonance spectroscopy signal intensity

and the apparent diffusion coefficient in human glioma. *Magnetic Resonance in Medicine* 1999; 41(1):2-7.

Hagberg G, Burlina AP, Mader I, Roser W, Radue EW, Seelig J. In vivo proton MR spectroscopy of human gliomas: definition of metabolic coordinates for multi-dimensional classification. *Magnetic Resonance in Medicine* 1995; 34(2):242-252.

Hall WA, Liu H, Martin AJ, Truwit CL. Comparison of stereotactic brain biopsy to interventional magnetic-resonance-imaging-guided brain biopsy. *Stereotactic & Functional Neurosurgery* 1999; 73(1-4):148-153.

Hall WA, Martin A, Liu H, Truwit CL. Improving diagnostic yield in brain biopsy: coupling spectroscopic targeting with real-time needle placement. *Journal of Magnetic Resonance Imaging* 2001; 13(1):12-15.

Harada M, Tanouchi M, Nishitani H, Miyoshi H, Bandou K, Kannuki S. Non-invasive characterization of brain tumor by in-vivo proton magnetic resonance spectroscopy. *Japanese Journal of Cancer Research* 1995; 86(3):329-332.

Heesters MA, Go KG, Kamman RL, Mooyaart EL, Meertens H, Paans AM et al. <sup>11</sup>C-tyrosine position emission tomography and <sup>1</sup>H magnetic resonance spectroscopy of the response of brain gliomas to radiotherapy. *Neuroradiology* 1998; 40(2):103-108.

Heesters MA, Kamman RL, Mooyaart EL, Go KG. Localized proton spectroscopy of inoperable brain gliomas. Response to radiation therapy. *Journal of Neuro-Oncology* 1993; 17(1):27-35.

Henriksen O, Wieslander S, Gjerris F, Jensen KM. In vivo <sup>1</sup>H-spectroscopy of human intracranial tumors at 1.5 tesla. Preliminary experience at a clinical installation. *Acta Radiologica* 1991; 32(2):95-99.

Herminghaus S, Dierks T, Pilatus U, Moller-Hartmann W, Wittsack J, Marquardt G et al. Determination of histopathological tumor grade in

neuroepithelial brain tumors by using spectral pattern analysis of in vivo spectroscopic data. *Journal of Neurosurgery* 2003; 98(1):74-81.

Houkin K, Kamada K, Sawamura Y, Iwasaki Y, Abe H, Kashiwaba T. Proton magnetic resonance spectroscopy (1H-MRS) for the evaluation of treatment of brain tumours. *Neuroradiology* 1995; 37(2):99-103.

Howe FA, Barton SJ, Cudlip SA, Stubbs M, Saunders DE, Murphy M et al. Metabolic profiles of human brain tumors using quantitative in vivo 1H magnetic resonance spectroscopy. *Magnetic Resonance in Medicine* 49(2):223-32, 2003.

Hubesch B, Marinier DS, Hetherington HP, Twieg DB, Weiner MW. Clinical MRS studies of the brain. *Investigative Radiology* 1989; 24(12):1039-1042.

Ikehira H, Miyamoto T, Yasukawa T, Obata T, Katoh H, Koga M et al. Differences in metabolic and morphological reactions after radiation therapy: proton NMR spectroscopy and imaging of patients with intracranial tumors. *Radiation Medicine* 1995; 13(5):199-204.

Ishimaru H, Morikawa M, Iwanaga S, Kaminogo M, Ochi M, Hayashi K. Differentiation between high-grade glioma and metastatic brain tumor using single-voxel proton MR spectroscopy. *European Radiology* 2001; 11(9):1784-1791.

Isobe T, Matsumura A, Anno I, Yoshizawa T, Nagatomo Y, Itai Y et al. Quantification of cerebral metabolites in glioma patients with proton MR spectroscopy using T2 relaxation time correction. *Magnetic Resonance Imaging* 2002; 20(4):343-349.

Kadota O, Kohno K, Ohue S, Kumon Y, Sakaki S, Kikuchi K et al. Discrimination of brain abscess and cystic tumor by in vivo proton magnetic resonance spectroscopy. *Neurologia Medico-Chirurgica* 2001; 41(3):121-126.

Kamada K, Houkin K, Abe H, Sawamura Y, Kashiwaba T. Differentiation of cerebral radiation necrosis from tumor recurrence by

proton magnetic resonance spectroscopy. *Neurologia Medico-Chirurgica* 1997; 37(3):250-256.

Kamada K, Moller M, Saguer M, Ganslandt O, Kaltenhauser M, Kober H et al. A combined study of tumor-related brain lesions using MEG and proton MR spectroscopic imaging. *Journal of the Neurological Sciences* 2001; 186(1-2):13-21.

Kaminogo M, Ishimaru H, Morikawa M, Ochi M, Ushijima R, Tani M et al. Diagnostic potential of short echo time MR spectroscopy of gliomas with single-voxel and point-resolved spatially localised proton spectroscopy of brain. *Neuroradiology* 2001; 43(5):353-363.

Kauppinen RA, Niskanen T, Hakumaki J, Williams SR 1993 Quantitative analysis of  $^1\text{H}$  NMR spectra of human brain. *Magnetic Resonance Medicine* 32:140-150.

Kim SH, Chang KH, Song IC, Han MH, Kim HC, Kang HS et al. Brain abscess and brain tumor: discrimination with in vivo H-1 MR spectroscopy. *Radiology* 1997; 204(1):239-245.

Kimura T, Sako K, Gotoh T, Tanaka K, Tanaka T. In vivo single-voxel proton MR spectroscopy in brain lesions with ring-like enhancement. *NMR in Biomedicine* 2001; 14(6):339-349.

Kinoshita K, Tada E, Matsumoto K, Asari S, Ohmoto T, Itoh T. Proton MR spectroscopy of delayed cerebral radiation in monkeys and humans after brachytherapy. *AJNR: American Journal of Neuroradiology* 1997; 18(9):1753-1761.

Kizu O, Naruse S, Furuya S, Morishita H, Ide M, Maeda T et al. Application of proton chemical shift imaging in monitoring of gamma knife radiosurgery on brain tumors. *Magnetic Resonance Imaging* 1998; 16(2):197-204.

Kugel H, Heindel W, Ernestus RI, Bunke J, du MR, Friedmann G. Human brain tumors: spectral patterns detected with localized H-1 MR spectroscopy. *Radiology* 1992; 183(3):701-709.

Langkowski JH, Wieland J, Bomsdorf H, Leibfritz D, Westphal M, Offermann W et al. Pre-operative localized in vivo proton spectroscopy in cerebral tumors at 4.0 Tesla--first results. *Magnetic Resonance Imaging* 1989; 7(5):547-555.

Law M, Cha S, Knopp EA, Johnson G, Arnett J, Litt AW. High-grade gliomas and solitary metastases: differentiation by using perfusion and proton spectroscopic MR imaging. *Radiology* 2002; 222(3):715-721.

Lin A, Bluml S, Mamelak AN. Efficacy of proton magnetic resonance spectroscopy in clinical decision making for patients with suspected malignant brain tumors. *Journal of Neuro-Oncology* 1999; 45(1):69-81.

Lin AP, Ross BD. Short-echo time proton MR spectroscopy in the presence of gadolinium. *Journal of Computer Assisted Tomography* 2001; 25(5):705-712.

Luan W, Zhang J. In vivo hydrogen-1 magnetic resonance spectroscopy study of human intracranial tumors. *Chinese Medical Journal* 1998; 111(1):56-58.

Mader I, Roser W, Hagberg G, Schneider M, Sauter R, Seelig J et al. Proton chemical shift imaging, metabolic maps, and single voxel spectroscopy of glial brain tumors. *Magma* 1996; 4(2):139-150.

Majos C, Alonso J, Aguilera C, Serrallonga M, Perez-Martin J, Acebes JJ et al. Proton magnetic resonance spectroscopy ( $^1\text{H}$  MRS) of human brain tumours: assessment of differences between tumour types and its applicability in brain tumour categorization. *European Radiology* 13(3):582-91, 2003.

Manton DJ, Lowry M, Rowland-Hill C, Crooks D, Mathew B, Turnbull LW. Combined proton MR spectroscopy and dynamic contrast enhanced MR imaging of human intracranial tumours in vivo. *NMR in Biomedicine* 2000; 13(8):449-459.

Maris JM, Evans AE, McLaughlin AC, D'Angio GJ, Bolinger L, Manos H, Chance B. 31P nuclear magnetic resonance spectroscopic investigation of human neuroblastoma in situ. *N Engl J Med* 1985 Jun 6;312(23):1500-5.

McBride DQ, Miller BL, Nikas DL, Buchthal S, Chang L, Chiang F et al. Analysis of brain tumors using 1H magnetic resonance spectroscopy. *Surgical Neurology* 1995; 44(2):137-144.

McKnight TR, Noworolski SM, Vigneron DB, Nelson SJ. An automated technique for the quantitative assessment of 3D-MRSI data from patients with glioma. *Journal of Magnetic Resonance Imaging* 2001; 13(2):167-177.

McKnight TR, dem Bussche MH, Vigneron DB, Lu Y, Berger MS, McDermott MW et al. Histopathological validation of a three-dimensional magnetic resonance spectroscopy index as a predictor of tumor presence. *Journal of Neurosurgery* 2002; 97(4):794-802.

Meyerand ME, Pipas JM, Mamourian A, Tosteson TD, Dunn JF. Classification of biopsy-confirmed brain tumors using single-voxel MR spectroscopy. *AJNR: American Journal of Neuroradiology* 1999; 20(1):117-123.

Moller-Hartmann W, Herminghaus S, Krings T, Marquardt G, Lanfermann H, Pilatus U et al. Clinical application of proton magnetic resonance spectroscopy in the diagnosis of intracranial mass lesions. *Neuroradiology* 2002; 44(5):371-381.

Murphy PS, Dzik-Jurasz AS, Leach MO, Rowland IJ. The effect of Gd-DTPA on T(1)-weighted choline signal in human brain tumours. *Magnetic Resonance Imaging* 2002; 20(1):127-130.

Negendank WG, Sauter R, Brown TR, Evelhoch JL, Falini A, Gotsis ED et al. Proton magnetic resonance spectroscopy in patients with glial tumors: a multicenter study. *Journal of Neurosurgery* 1996; 84(3):449-458.

Ng SH, Ko SF, Chen WC, Tang LM, Chang CN, Wai YY et al. Proton magnetic resonance spectroscopy of cerebral glioma after irradiation. *Chang Gung Medical Journal* 2001; 24(11):708-716.

Pirzkall A, McKnight TR, Graves EE, Carol MP, Sneed PK, Wara WW et al. MR-spectroscopy guided target delineation for high-grade gliomas. *International Journal of Radiation Oncology, Biology, Physics* 2001; 50(4):915-928.

Pirzkall A, Nelson SJ, McKnight TR, Takahashi MM, Li X, Graves EE et al. Metabolic imaging of low-grade gliomas with three-dimensional magnetic resonance spectroscopy. *International Journal of Radiation Oncology, Biology, Physics* 2002; 53(5):1254-1264.

Poptani H, Gupta RK, Jain VK, Roy R, Pandey R. Cystic intracranial mass lesions: possible role of in vivo MR spectroscopy in its differential diagnosis. *Magnetic Resonance Imaging* 1995; 13(7):1019-1029.

Poptani H, Gupta RK, Roy R, Pandey R, Jain VK, Chhabra DK. Characterization of intracranial mass lesions with in vivo proton MR spectroscopy. *AJNR: American Journal of Neuroradiology* 1995; 16(8):1593-1603.

Preul MC, Caramanos Z, Collins DL, Villemure JG, LeBlanc R, Olivier A et al. Accurate, noninvasive diagnosis of human brain tumors by using proton magnetic resonance spectroscopy. *Nature Medicine* 1996; 2(3):323-325.

Preul MC, Caramanos Z, Villemure JG, Shenouda G, LeBlanc R, Langleben A et al. Using proton magnetic resonance spectroscopic imaging to predict in vivo the response of recurrent malignant gliomas to tamoxifen chemotherapy. *Neurosurgery* 2000; 46(2):306-318.

Prost R, Haughton V, Li SJ. Brain tumors: localized H-1 MR spectroscopy at 0.5 T. *Radiology* 1997; 204(1):235-238.

Rabinov JD, Lee PL, Barker FG, Louis DN, Harsh GR, Cosgrove GR et al. In vivo 3-T MR spectroscopy in the distinction of recurrent



glioma versus radiation effects: initial experience. *Radiology* 2002; 225(3):871-879.

Rand SD, Prost R, Haughton V, Mark L, Strainer J, Johansen J et al. Accuracy of single-voxel proton MR spectroscopy in distinguishing neoplastic from nonneoplastic brain lesions. *AJNR: American Journal of Neuroradiology* 1997; 18(9):1695-1704.

Ricci PE, Pitt A, Keller PJ, Coons SW, Heiserman JE. Effect of voxel position on single-voxel MR spectroscopy findings. *AJNR: American Journal of Neuroradiology* 2000; 21(2):367-374.

Rock JP, Hearshen D, Scarpace L, Croteau D, Gutierrez J, Fisher JL et al. Correlations between magnetic resonance spectroscopy and image-guided histopathology, with special attention to radiation necrosis. *Neurosurgery* 2002; 51(4):912-919.

Roser W, Hagberg G, Mader I, Dellas S, Seelig J, Radue EW et al. Assignment of glial brain tumors in humans by in vivo <sup>1</sup>H-magnetic resonance spectroscopy and multidimensional metabolic classification. *Magma* 1997; 5(3):179-183.

Schlemmer HP, Bachert P, Herfarth KK, Zuna I, Debus J, van Kaick G. Proton MR spectroscopic evaluation of suspicious brain lesions after stereotactic radiotherapy. *AJNR: American Journal of Neuroradiology* 2001; 22(7):1316-1324.

Segebarth CM, Baleriaux DF, Luyten PR, den Hollander JA. Detection of metabolic heterogeneity of human intracranial tumors in vivo by <sup>1</sup>H NMR spectroscopic imaging. *Magnetic Resonance in Medicine* 1990; 13(1):62-76.

Shimizu H, Kumabe T, Shirane R, Yoshimoto T. Correlation between choline level measured by proton MR spectroscopy and Ki-67 labeling index in gliomas. *AJNR: American Journal of Neuroradiology* 2000; 21(4):659-665.

Shimizu H, Kumabe T, Tominaga T, Kayama T, Hara K, Ono Y et al. Noninvasive evaluation of malignancy of brain tumors with proton MR

spectroscopy. *AJNR: American Journal of Neuroradiology* 1996; 17(4):737-747.

Shukla-Dave A, Gupta RK, Roy R, Husain N, Paul L, Venkatesh SK et al. Prospective evaluation of in vivo proton MR spectroscopy in differentiation of similar appearing intracranial cystic lesions. *Magnetic Resonance Imaging* 2001; 19(1):103-110.

Sijens PE, Knopp MV, Brunetti A, Wicklow K, Alfano B, Bachert P et al. <sup>1</sup>H MR spectroscopy in patients with metastatic brain tumors: a multicenter study. *Magnetic Resonance in Medicine* 1995; 33(6):818-826.

Sijens PE, van den Bent MJ, Nowak PJ, van Dijk P, Oudkerk M. <sup>1</sup>H chemical shift imaging reveals loss of brain tumor choline signal after administration of Gd-contrast. *Magnetic Resonance in Medicine* 1997; 37(2):222-225.

Sijens PE, Vecht CJ, Levendag PC, van Dijk P, Oudkerk M. Hydrogen magnetic resonance spectroscopy follow-up after radiation therapy of human brain cancer. Unexpected inverse correlation between the changes in tumor choline level and post-gadolinium magnetic resonance imaging contrast. *Investigative Radiology* 1995; 30(12):738-744.

Tamiya T, Kinoshita K, Ono Y, Matsumoto K, Furuta T, Ohmoto T. Proton magnetic resonance spectroscopy reflects cellular proliferative activity in astrocytomas. *Neuroradiology* 2000; 42(5):333-338.

Tarnawski R, Sokol M, Pieniazek P, Maciejewski B, Walecki J, Mischczyk L et al. <sup>1</sup>H-MRS in vivo predicts the early treatment outcome of postoperative radiotherapy for malignant gliomas. *International Journal of Radiation Oncology, Biology, Physics* 2002; 52(5):1271-1276.

Tedeschi G, Lundbom N, Raman R, Bonavita S, Duyn JH, Alger JR et al. Increased choline signal coinciding with malignant degeneration of cerebral gliomas: a serial proton magnetic resonance spectroscopy imaging study. *Journal of Neurosurgery* 1997; 87(4):516-524.

Thomsen C, Jensen KE, Achten E, Henriksen O. In vivo magnetic resonance imaging and <sup>31</sup>P spectroscopy of large human brain tumours at 1.5 tesla. *Acta Radiologica* 1988; 29(1):77-82.

Tien RD, Lai PH, Smith JS, Lazeyras F. Single-voxel proton brain spectroscopy exam (PROBE/SV) in patients with primary brain tumors. *AJR American Journal of Roentgenology* 1996; 167(1):201-209.

Tomoi M, Kimura H, Yoshida M, Itoh S, Kawamura Y, Hayashi N et al. Alterations of lactate (+lipid) concentration in brain tumors with in vivo hydrogen magnetic resonance spectroscopy during radiotherapy. *Investigative Radiology* 1997; 32(5):288-296.

Vigneron D, Bollen A, McDermott M, Wald L, Day M, Moyher-Noworolski S et al. Three-dimensional magnetic resonance spectroscopic imaging of histologically confirmed brain tumors. *Magnetic Resonance Imaging* 2001; 19(1):89-101.

Wald LL, Nelson SJ, Day MR, Noworolski SE, Henry RG, Huhn SL et al. Serial proton magnetic resonance spectroscopy imaging of glioblastoma multiforme after brachytherapy. *Journal of Neurosurgery* 1997; 87(4):525-534.

Walecki J, Sokol M, Pieniazek P, Maciejewski B, Tarnawski R, Krupska T et al. Role of short TE <sup>1</sup>H-MR spectroscopy in monitoring of post-operation irradiated patients. *European Journal of Radiology* 1999; 30(2):154-161.

## Abstract References

Antiniw AS, Lau A, Nelson SJ. <sup>1</sup>H magnetic resonance spectroscopic imaging as a tool for evaluating patients with recurrent gliomas being considered for treatment with gamma knife radiosurgery. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2002.

Ben Sira L, Miller E, Siegal T, Gomori JM. Can proton MR spectroscopy (1H MRS) differentiate between oligodendrogliomas and astrocytomas? Radiological Society of North America 2002.

Bizzi A, Danesi U, Broggi G, Pollo B, Castelli G, Savolardo M et al. H-MR spectroscopic imaging-guided surgery of brain tumors: diagnosis of infiltrative vs circumscribed lesions. Radiological Society of North America 2001.

Bizzi A, Danesi U, Pollo B, Franzini A, Broggi G, Savolardo M. H-MR spectroscopic imaging-guided surgery of brain tumors and correlation with neuropathology. American Society of Neuroradiology 2001.

Castillo M, Smith JK, Kwock L. Proton MR spectroscopy of brainstem lesions: preliminary experience. American Society of Neuroradiology 2001.

Catalaa I, Henry RG, Graves E, Lu Y, Vigneron D, Nelson SJ. Diffusion, perfusion and H1-spectroscopy in patients with newly diagnosed gliomas. Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001.

Cha S, Saindane AM, Law M, Knopp EA, Zagzag D. Proton MR spectroscopy of tumefactive demyelinating lesions. American Society of Neuroradiology 2002.

Cruz LH, Brandao LA, Martins G, Domingues RC, Provenzale JM, Domingues RC. Perfusion MR imaging and proton MR spectroscopy of neoplastic brain tumors. Radiological Society of North America 2001.

Fan G, Wu Z. Proton MR spectroscopy in the differentiation of high-grade glioma solitary metastases. Radiological Society of North America 2002.

Fatterpekar G, Delman B, Rosenthal H, Sacher M, Lidov M, Naidich T. Use of diffusion-weighted imaging and MR spectroscopy to distinguish brain abscess from intraparenchymal cystic/necrotic tumors. American Society of Neuroradiology 2002.

Fujiwara DT, de Castro CC, Rosemberg S, Rotta MJ, Piva RMV, Crri GG. In patients with brain tumors, can the contralateral brain hemisphere be used as control for single-voxel  $^1\text{H}$  spectroscopy? Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001.

Gomori JM, Levin N, Rubinstein R, Shoshan Y, Siegal T. Conventional and functional imaging techniques in patients with delayed radiation-induced brain injury (RIBI). Radiological Society of North America 2001.

Graves EE, Takahashi M, Pirzkall A, Larson D, Verhey LJ, Chang S et al. Serial  $^1\text{H}$  magnetic resonance spectroscopy imaging of gliomas after fractionated radiation therapy. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2002.

Hakyemez B, Parlak M, Tuncel E. Clinical impact of in vivo single-voxel proton MR spectroscopy in neoplastic and nonneoplastic brain disorders. American Society of Neuroradiology 2001.

Hearshen D, Scarpace L, Patel S, Rock JP, Peck D, Mikkelsen T. Multi-slice proton spectroscopic imaging of delayed radiation necrosis correlated with intraoperative histology. Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001.

Herminghaus S, Pilatus U, Lanfermann H, Setzer M, Lang J, Zanella FE. Clinical impact of single voxel in vivo proton MR spectroscopy ( $^1\text{H}$  MRS) in the diagnostic of focal brain lesions – an analysis of 293 cases using cluster and discriminant analysis. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2002a.

Herminghaus S, Pilatus U, Marquardt G, Möller-Hartmann W, Setzer M, Lanfermann H. Differentiation of low from high grade gliomas: proton MR spectroscopy vs stereotactic biopsy. American Society of Neuroradiology 2001a.

Herminghaus W, Pilatus U, Matthias S, Lang J, Lanfermann H, Volker S et al. Pathologic metabolism of neuroepithelial brain tumors: prognostic impact of total choline compounds and lipids as measured with in vivo proton MNR spectroscopy. Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001b.

Herminghaus W, Pilatus U, Raab P, Lanfermann H, Schlote W, Zanella FE. Impact of in vivo proton MR spectroscopy for the assessment of the proliferative activity in viable and partly necrotic brain tumor tissue. American Society of Neuroradiology 2001c.

Herminghaus W, Pilatus U, Setzer M, Lang J, Lanfermann H, Schlote W, Zanella FE. Proton MR spectroscopy: a reliable tool for differentiating different oncotypes? American Society of Neuroradiology 2002b.

Herminghaus W, Setzer M, Pilatus U, Lang J, Lanfermann H, Zanella FE. Pathologic metabolism of neuroepithelial brain tumors: prognostic impact of total choline compounds and lipids as measured with in vivo proton MNR spectroscopy. American Society of Neuroradiology 2001d.

Hiltunen Y, Pulkkinen J, Häkkinen AM, Lundbom N, Kauppinen RA. Automatic independent component analysis of  $^1\text{H}$  spectroscopic imaging data from human brain tumors. Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001.

Hiwatashi A, Moritani T, Kinoshita T, Zhong J, Wang HZ, Shrier DA et al. Multivoxel MR spectroscopy and echo-planar diffusion-weighted MR imaging in intracranial tumors. American Society of Neuroradiology 2002.

Howe FA, Murphy M, Wilkins P, Loosemore A, Bell BA, Griffiths JR. Correlation of the  $^1\text{H}$  MRS metabolic profile of human brain tumors

with patient survival. Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001.

Kovanlikaya I, Maya MM, Suri R, Moser FG, Tourje EJ, Pressman BD. Multivoxel MR spectroscopy of glial neoplasms: detection of tumor regrowth after treatment. Radiological Society of North America 2002.

Law M, Cha S, Knopp EA, Johnson G, Salibi N. Glioma grading with multi-voxel, multi-slice spectroscopy MRI and multi-slice perfusion MRI. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2002.

Leeds NE, Jackson E, Kumar A, Singh S, Mahankali S. MR spectroscopy in diagnosis and management of patients with gliomatosis cerebri. American Society of Neuroradiology 2002.

Lefkowitz D, Read K, Chin LS, Gullapalli RP. Accuracy of 1H MR spectroscopy in the assessment of malignant brain tumors. American Society of Neuroradiology 2002.

Lefkowitz D, Read K, Chin LS, Gullapalli RP. Treated malignant brain tumor assessment: accuracy of 1H-MR spectroscopy as an independent measure. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2001.

Li X, Lu Y, Nelson SJ. Analysis of spatial extent of the metabolic abnormality for newly diagnosed glioma patients. Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001.

Li X, Nelson SJ. Comparison of anatomic and metabolic abnormalities for newly diagnosed glioma patients prior to treatment with fractionated radiation therapy. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2002.

Lichy MP, Henze H, Sammet S, Maudsley AA, Bachert P, Debus J et al. Clinical decision making in irradiated gliomas: Value of proton MR spectroscopy compared to FDG-PET and IMT-SPECT. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2002.

Lim CCT, Chua VGE, Chai SP, Kong FH. Multi-voxel MR spectroscopy – distinguishing brain tumor from non-tumor. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2002.

Lim CCT, Chua VGE, Chai SP, Kong WL, Hui F. Multi-voxel MR spectroscopy: pitfalls and patterns in brain tumor assessment. American Society of Neuroradiology 2001.

Lin A, Ross B. How accurate is  $^1\text{H}$  MRS in the individual tumor patient? Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001.

Lin A, Shic F, Ross B. Differentiating diffuse brainstem neoplasms using proton magnetic resonance spectroscopy. Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001.

Londño A, Kwock L, Castillo M. Proton MR spectroscopy of meningiomas: alanine is lacking in most. American Society of Neuroradiology 2002.

Majos C, Alonso J, Arus C, Aguilera C, Serrallonga M, Lopez-Obarrio L. et al. Proton magnetic resonance spectroscopy ( $^1\text{H}$  MRS) of brain tumors at long echo time: assessment of differences between tumor types and their applicability in brain tumor categorization in adults. Radiological Society of North America 2001.

Majos C, Arus C, Aguilera C, Serrllonga, Alosó J, Gili J. Proton magnetic resonance spectroscopy ( $^1\text{H}$  MRS) of brain meningiomas at long echo time: utility in identification of meningiomas uncertain diagnosis. Radiological Society of North America 2002.

Mao H, Holder CA, Olson JJ, Brat D, Mukundan S.  $^1\text{H}$  MR spectroscopy imaging directed stereotactic biopsy of previously biopsied suspicious brain lesions with equivocal histologic results. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2002.



McKnight T, Vigneron D, Love T, Lamborn K, Chiu K, Berger M et al. Comparison of a Cho-NAA index with the MIB-1 proliferative index and cell density of tissue samples from grades II and III glioma. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2002.

McKnight TR, von dem Bussche MH, Vigneron DB, Berger MS, McDermontt MW, Dillon WP et al. Correlation of 3D MRS imaging tumor index with histology in patients with newly diagnosed gliomas. American Society of Neuroradiology 2001.

Peck DJ, Hearshen DO, Scarpance LM, Soltanian-Zadeh H, Mikkelsen T. Segmentation of brain tumor boundaries using pattern recognition of magnetic resonance spectroscopy. Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001.

Peck DJ, Hearshen DO, Soltanian-Zadeh H, Scarpance LM, Dodge C, Mikkelsen T. Segmentation of brain tumor boundaries using pattern recognition of magnetic resonance spectroscopy. Radiological Society of North America 2001.

Pilatus U, Reichel P, Herminghaus S, Raab P, Setzer M, Lanfermann H, Zanella FE. <sup>1</sup>H MRS of neutral lipids in low and high grade gliomas, recurrent gliomas, metastases, lymphomas, abscesses, and inflammation. Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001.

Pilatus U, Reichel P, Raab P, Herminghaus S, Setzer M, Lanfermann H, Zanella FE. MRS detectable lipids signal in low- and high-grade gliomas, recurrent gliomas, metastases, lymphomas, and abscesses. American Society of Neuroradiology 2001.

Scatliff JH, Kwock L, Varia MA, Walters BB. Brain MR imaging and MR proton spectroscopy in the assessment of cerebral metastases before and after radiosurgery. American Society of Neuroradiology 2001.

Shah T, Jayasundar R, Singh VP, Sarkar C. Correlation between in vivo and in vitro proton MRS and histology of brain tumors.

Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001.

Shah T, Jayasundar R, Singh VP, Sarkar C. Grading of gliomas – an in vivo proton MRS study. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2002.

Shah T, Jayasundar R, Singh VP, Sarkar C. Proton MRS in the differential diagnosis of intraventricular meningiomas and central neurocytomas. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2001.

Shah T, Jayasundar R, Singh VP, Bal CS, Gaikwad S, Sarkar C. Diagnostic potential of proton MRS in identifying tumor recurrence. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2002.

Smith JK, Kwock L, Londono A, Castillo M. Proton MR spectroscopy of brainstem lesions. Radiological Society of North America 2002.

Szabo De Edelenyi F, Estève F, Grand S, Segebarth C, Rubin C et al. Classification of brain tumors using  $^1\text{H}$  MRSI at an echo time of 272 msec in combination with linear discriminant analysis. Strategies to improve the correct classification rate. Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001.

Tate AR, Griffiths JR, Howe FA, Pujol J, Arus C. Differentiating types of human brain tumours by MRS. A Comparison of pre-processing methods and echo times. Proceedings of the International Society for Magnetic Resonance in Medicine 9; 2001.

Waldman AD, MacManus DG, Moore EA, Stevens J, Rees JH. Serial short-TE single-voxel MRS in low grade gliomas for early detection of malignant transformation. Proceedings of the International Society for Magnetic Resonance in Medicine 10; 2002.

Yin H, Gao YG, Cai Y, Ma L, Liang Y, Guo XG. Discrimination between brain space occupying lesions by 3D proton MR spectroscopy. Radiological Society of North America 2002.

Evidence Table 1. Summary of studies examining technical feasibility for magnetic resonance spectroscopy

Author	UI	Pub. Yr.	Country	Study characteristics					Technique		Study objectives						
				Study design (Case)	N (Crab)	Enrollment	Dr status	Mean Age, range	Mean volume (cm <sup>3</sup> )	S/M	Tumor diff	Tumor grading	Recr. vs Prim.	Met vs Primary	Neovasc	Other	
Alger	224962	1990	US	p	40	0	u	k	42, 18-81	27	s					x	
Barba	11147898	2001	England	p	27	0	u	k	ND	2x2x2	s					x	
Bachmann	8458376	1998	Italy	u	19	20	u	k	21-69	2x2x3	s				x		
Buhr	2748837	1989	Germany	p	9	0	u	k	53-61	3x3x3	s						x
Burtscher	10666230	2000	Sweden	p	26	0	u	k	62, 31-80	1.5x1.5x1.5-2.7/3x3x1.5-1.0x3x1.5	s/m	x					x
Castillo	11039343	2000	US	p	34	5	u	k	2-75	3-27	s	x					x
Chang	9541289	1998	Korea	p	39	0	u	k	43, 28-60	2x2x2	s				x		x
Chomas	8219244	1997	Scotland	p	9	0	u	k	54	21	s						x
Choussat	11564242	2001	US	p	31	0	u	k	>19	0.8	m	x					x
Demaeset	1846155	1991	Belgium	p	50	0	u	k	53.4, 16-79	8-84	s	x					x
Domingo	10070443	1998	UK	p	8	0	u	k	58, 41-78	1x1x1.5	s						x
Dowling	11290466	2001	US	p	29	0	u	k	15-68	1	m	x					
Estève	9457810	1998	France	p	11	0	u	k	30-63	1x0.9x2	s						
Falini	8923303	1998	Italy	p	70	0	u	M	ND	8	s	x					x
Fournias	11251398	2000	US/Greece	p	120	0	u	k	61.3, 29-76	8	s	x					x
Frahm	92042846	1991	Germany	p	19	-300 studies	u	k	ND	2-8	s	x					
Fulham	1438744	1992	US	r	50	0	u	k	43, 18-76	0.675-2.0	m	x			x		x
Furuwa	9251112	1997	Japan	r	17	0	u	k	ND	8 <sup>1</sup>	m	x					
Gallegher	12593610	2003	France	p	9	0, 8, 25	u	k	52, 35-69	ND / 2.0x2.0x1.5	s/m	x					
Go	7503095	1995	The Netherlands	u	32	0	u	k	ND	3x3x1	m						x
Go	9416313	1997	The Netherlands	u	18	0	u	u	ND	3x3x1, 1	m						x
Gotsis	8694527	1996	Greece	u	76	0	u	u	ND	2-8	s	x					x
Graves <sup>1</sup>	10690720	2000	US	p	36	0	u	k	45.5, 24-68	1	m						x
Graves <sup>2</sup>	11290487	2001	US	p	18	0	u	k	24-82	1	m				x		x
Guda	10929604	1999	US	r	20	0	na	k	27-68	1x1x1.2	m	x					x
Gupta	11263501	2001	US	p	18	0	u	M	29-82	1x1x1.2	m						x
Hagberg	7476984	1995	Switzerland	p	32	8	u	k	55	6-18	s	x					x
Hall	10853123	1999	US	u	6	0	u	k	ND	ND	u						x
Hara	95263377	1995	Japan	p	25	0	u	k	ND	15.6	s	x					x
Heesters	8120569	1993	The Netherlands	u	11	0	u	k	ND	27 cc / 9 cc / 1	s/m						x
Heesters	9541920	1998	The Netherlands	p	8	0	u	k	29-66	1	m						x
Henningshausen	12546355	2003	Germany	p	99	0	c	D	ND	4.2 - 12.7	s						x
Henriksen	2031809	1991	Denmark	p	17	0	u	k	49, 24-77	3x3x3	s	x					x
Hoskin	7781009	1995	Japan	u	11	0	u	k	ND	2x2x2 - 3x3x3	s						x
Hove	12541241	2003	UK	p	42	6	u	D	ND	4-8	s						x
Hubsch	2556986	1989	US	u	45	13	u	k	ND	18 - 40	s						x
Ikehira	8848553	1995	Japan	p	16	3	u	k	46.4, 14-71	5-27	s						x
Ishimaru	11511892	2001	Japan	p	56	0	u	k	65.6, 12-88	1.3x1.3x1.3 - 1.5x1.5x1.5	s						x
Isoke	12165353	2002	Japan	p	23	7	u	k	20-26	2.2 - 31.5	s	x					x
Kadota	11372554	2001	Japan	p	10	0	u	k	12-73	2x2x2 - 3x3x3	s	x					x
Kamada	9395925	1997	Japan	p	11	20	u	k	7-76	9-27	s						x
Kamada	11412866	2001	Germany	p	7	10	u	k	37-61	1.25x1.25x1.5	m						x
Kamino	11396738	2001	Japan	p	25	0	u	k	13-82	12x12x12 - 15x15x15	s	x					x
Kim	8205954	1998	Korea	p	14	0	c	k	26-70	2x2x2	s						x
Kirushita	9367328	1997	Japan	p	12	16	u	k	50, 43-62	1	s						x
Kizu	9508276	1998	Japan	r	6	0	n	k	50, 13-63	0.38-0.47	m						x
Kugel	11584024	1993	Germany	p	36	27	u	k	27-81	8-18	s	x					x
Lankowski	2607903	1989	Germany	p	16	0	u	k	22-74	4-20	s						x
Law	11867790	2002	US	p	17	34	c	k	51.9, 15-80	1x1x1.5 - 1x1x2	m						x
Lin	11584229	2001	US	p	49	14	c	k	50	variable	s						x
Liu	10332655	1998	China	p	13	0	u	k	42, 13-68	2x2x2	s	x					x
Mader	87029389	1998	Switzerland	p	17	7	u	n	50.3, 20-74	8 / 3.4-4.5	s/m	x					x
Majst	12594562	2003	Spain	p	25	0	c	u	ND	1.5 - 2	s	x					x
Manson	11252030	2001	UK	p	23	0	u	k	ND	variable	s	x					x
McBride	7602803	1995	US	p	23	16	u	k	ND	27	s	x					x
McKnight	11169821	2001	US	p	30	14	u	k	42	1	m	x					x

Types of tu

**Evidence Table 1. Summary of studies examining technical feasibility for magnetic resonance spectroscopy (Continued)**

Author	UI	Pub Yr	Country	Study characteristics					Technique			Study objective(s)					
				Study design	N (cases)	N (ctrls)	Enrollment	Dx status	Mean Age, range	Voxel volume (cm <sup>3</sup> )	S / M	Tumor diff	Tumor grading	Recur vs Prim.	Met vs Primary	Necrosis	Other
Meyerand	9974066	1999	US	p	27	0	u	k	43, 19-72	1 - 6.2	s	x	x				
Murphy	11973038	2002	UK	p	19	0	c	k	ND	8 - 16	s		x				
Negendank	8609557	1996	US/Europe/Japan	p	86	0	u	k	41, 3-75	8	s	x	x				
Ng	11820651	2001	Taiwan	p	58	0	u	k	ND	2 - 20	s	x				x	x
Pirzkall	11429219	2001	US/Germany	p	34	0	c	k	ND	1	m						x
Pirzkall	12128127	2002	US	p	20	0	u	k	39, 23-57	1	m						x
Poptani	7502961	1995	India	p	120	40	u	n	1-65	4.09 - 8	s	x	x				
Poptani	8583866	1995	India	p	34	30	u	n	1-65	4.09 - 8	s	x	x				
Preul	8612232	1996	Canada	u	91	14	u	u	ND	0.1	m	x					
Preul	10690729	2000	Canada	p	16	0	n	M	48.2, 24-70	0.7 - 1.2	m						x
Prost	9205253	1997	US	p	18	8	u	n	16-73	1.0 - 11.47	s						x
Rabinov	12461273	2002	US	p	14	0	u	k	40.4, 28-51	1.25	m						x
Ricci	10696025	2000	US	r	19	0	c	k	55, 42-70	4 - 8	s						x
Rock	12234397	2002	US	p	27	31	u	M	>18	0.9	m	x				x	
Schlemmer	11498420	2001	US/Germany	p	56	0	u	k	42.5	1.5 - 2x2x3	s	x					x
Segebarth	2319936	1990	Europe	p	10	12	u	k	ND	30 / 9-30	m						x
Shimizu	10782774	2000	Japan	p	26	0	c	n	46, 24-79	1.2x1.2x1.6 - 2x2x2	s		x				
Shimizu	8730195	1996	Japan	p	25	17	u	k	ND	1.3x1.3x1.5 - 2x2x2	s		x				
Sijens	9001146	1997	The Netherlands	u	17	0	u	k	ND	1x1x2 cm	m						
Sijens	7651119	1995	US/Europe	u	40	151	u	k	24-73	8	s	x					
Sijens	8748188	1995	The Netherlands	u	13	0	u	k	ND	3.4-64 / 10.2-13.6	s/m						x
Tamiya	10872152	2000	Japan	p	23	14	n	M	42.5, 15-68	1	s	x	x				
Tarnawski	11955739	2002	Poland	p	51	30	c	k	47, 20-68	1.5x1.5x1.5	s		x				x
Thomsen	2831923	1988	Europe	u	8	8	u	n	14-66	ND	ND	x	x				
Tien	8659372	1996	US	p	46	10	n	k	46, 17-78	6-8	s		x				
Tomoi	9140749	1997	Japan	u	8	0	u	k	62.5, 32-83	1.5x1.5x1.5	s						x
Vigneron	11295350	2001	US	p	31	8	u	n	ND	0.24 - 0.54, 1 - 2	m	x	x				
Wald	9322843	1997	US	p	12	0	u	k	ND	0.34 - 2	m						x
Walecki	10401596	1999	Poland	p	10	30	u	k	28-51	8	s						x

<sup>1</sup> Voxel size data unclear or incomplete

<sup>2</sup> Possible overlapping patient population

Abbreviations: c, consecutive; k, known; M, mixed; m, multiple; n, nonconsecutive; n, no histological diagnosis; ND, no data; p, prospective; r, retrospective; s, single; u, unknown

**Evidence Table 2. Summary of abstracts examining technical feasibility for magnetic resonance spectroscopy**

Author	Proceedings	Pub Yr	Country	Study characteristics					Technique		Study objective(s)						
				Study design	N (cases)	N (ctris)	Enrollment	Dx status	Mean Age, range	Voxel volume (cm <sup>3</sup> )	S / M	Tumor diff	Tumor grading	Recur vs Prim.	Met vs Primary	Necrosis	Other
Antiniw	ISMRM	2002	US	p	22	0	u	k	22-84	ND	m						x
Ben Sira	RSNA	2002	Israel	r	35	0	c	k	ND	ND	s	x					
Bizzi <sup>1</sup>	RSNA	2001	Italy	u	22	0	u	u	44	ND	m		x				
Bizzi <sup>1</sup>	ASNR	2001	Italy	u	20	0	u	u	40	ND	m						
Castillo	ASNR	2001	US	r	17	0	u	k	ND	ND	s	x					
Catalaa	ISMRM	2001	US	u	67	0	u	u	23-78	1	m		x				
Cha	ASNR	2002	US	r	10 gliomas	0	u	k	ND	ND	u	x					
Cruz	RSNA	2001	Brazil	r	15	0	u	k	ND	ND	s	x	x				
Fan	RSNA	2002	China	p	22	0	u	u	36.7mdn, 8-62	ND	u	x					
Fatterpekar	ASNR	2001	US	r	14 studies	0	u	u	ND	ND	u	x					
Fujiwara	ISMRM	2001	Brazil	u	22	5	u	u	ND	8	s						x
Gomori	RSNA	2001	Israel	u	10	12	u	k	ND	ND	u						x
Graves	ISMRM	2002	US	u	10	0	u	u	ND	ND	m						x
Hakyemez	ASNR	2001	Turkey	u	23	0	u	u	ND	2x2x2	s	x					
Hearshen <sup>2</sup>	ISMRM	2001	US	u	35	0	u	k	ND	.9x.9x1.5	m						
Herminghaus	ASNR	2002	Germany	u	174 lesions		u	u	ND	ND	s	x					
Herminghaus <sup>3</sup>	ASNR	2001	Germany	u	83	0	c	M	ND	ND	s						x
Herminghaus <sup>3</sup>	ASNR ISMRM	2001	Germany	u	31	0	u	u	52.8, 11-75	ND	s						x
Hiltunen	ISMRM	2001	Finland	u	8	2	u	k	ND		m		x				
Hiwatashi	ASNR	2002	US	u	24	0	u	u	ND	1	m						
Howe	ISMRM	2002	UK	u	25	8	u	k	ND	ND	u						x
Law	ISMRM	2002	US	u	20	10	u	k	ND	1x1x1.5 - 1x1x2	m		x				
Leeds	ASNR	2002	US	u	9	0	u	k	ND	ND	m		x				x
Li <sup>4</sup>	ISMRM	2001	US	u	18	0	u	M	ND	ND	s/m	x					
Li <sup>4</sup>	ISMRM	2002	US	u	19	0	u	k	ND	ND	m						x
Lim	ASNR	2001	Singapore	u	59	0	u	u	ND	ND	m						x
Lim	ISMRM	2002	Singapore	u	20	15	u	k	ND	1	m	x					
Lin	ISMRM	2001	US	p	7	15	u	u	43, 25-64 (cntrl)	4.5 (cntrl) 2-4.5 (case)	s						x
Lin	ISMRM	2001	US	u	50	50	c	k	ND	4-12.5	s						x
Londono	ASNR	2002	US	u	15 meningiomas		u	M	24-81	ND	s/m						x
Majos	RSNA	2002	Spain	u	130	0	u	u	ND	ND	s	x					
Majos	RSNA	2001	Spain	p	108	0	u	u	ND	ND	s						x
McKnight	ASNR	2001	US	u	58	0	u	u	ND	1	m	x	x				
McKnight	ISMRM	2002	US	u	20	0	u	u	ND	ND	m		x				
Peck	ISMRM RSNA	2001	US	u	10	0	u	k	ND	ND	u						x
Pilatus	ASNR ISMRM	2001	Germany	u	95	0	c	u	ND	ND	s						x
Scatliff	ASNR	2001	US	u	12	0	u	k	ND	1.5-2	s/m						x
Shah	ISMRM	2002	India	u	10	0	u	n	ND	3-6	s	x					
Shah <sup>5</sup>	ISMRM	2001	India	u	72	0	u	n	ND	1.7-8	s						x
Shah <sup>5</sup>	ISMRM	2002	India	u	52	0	u	n	ND	2.2 - 8	s		x				
Smith	RSNA	2003	US	u	25	5	u	u	ND	ND	s/m						
Szabo De Edelenyi	ISMRM	2001	France	u	56	7	u	n	ND	ND	m		x				
Tate	ISMRM	2001	UK/Spain	u	51	0	u	u	ND	ND	s	x					
Waldman	ISMRM	2002	UK	p	28	0	u	n	ND	1-8	s						x

<sup>1, 3, 4, 5</sup> Potential overlap of patient population

<sup>2</sup> Potential overlap of patient population with Rock, Hearshen, Scarpace et al., 2002

Abbreviations: ASNR, American Society of Neuroradiology; c, consecutive; k, known; M, mixed; m, multiple; mdn, median; n, nonconsecutive; N, no histological diagnosis; ISMRM, International Society for Magnetic Resonance in Medicine; NA, not applicable; ND, no data; p, prospective; r, retrospective; RIBI, radiation-induced brain injury; RSNA, Radiological Society of North America; s, single; u, unknown.